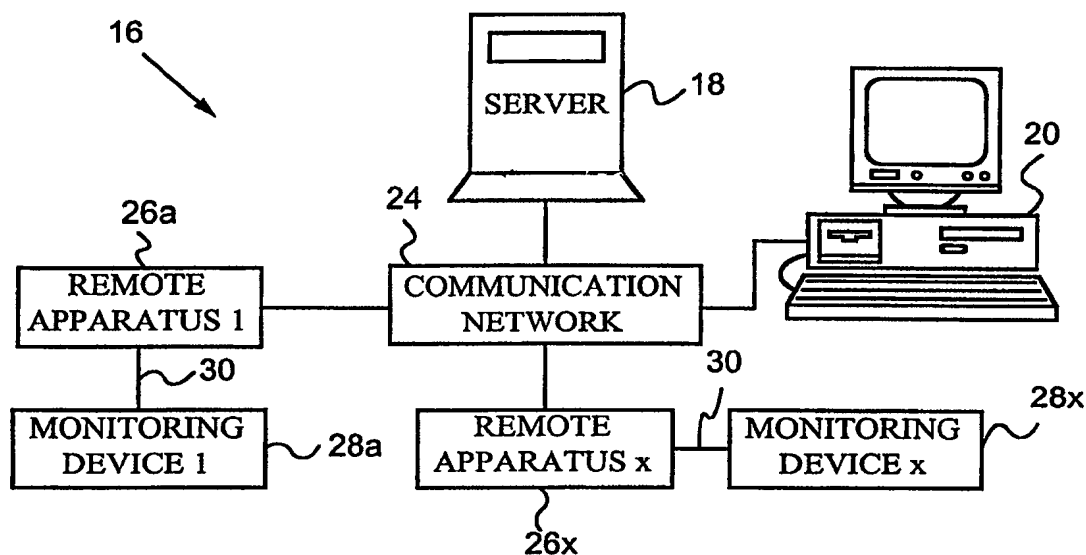




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(54) Title: NETWORKED SYSTEM FOR INTERACTIVE COMMUNICATION AND REMOTE MONITORING OF DRUG DELIVERY



(57) Abstract

This invention is a networked system (16) for communicating information to a patient, and for remotely monitoring the patient.

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5 **NETWORKED SYSTEM FOR INTERACTIVE COMMUNICATION AND
REMOTE MONITORING OF DRUG DELIVERY**

RELATED U.S. APPLICATION DATA

10 This application is a continuation-in-part of application Ser. No. 08/946,341, filed
October 7, 1997, which is a continuation-in-part of application Ser. No. 08/847,009 filed
April 30, 1997. The parent application claims priority from provisional application Ser.
No. 60/041,746 filed March 28, 1997 and from provisional application Ser. No.
60/041,751 filed March 28, 1997. All of the above named applications are incorporated
15 by reference herein.

FIELD OF THE INVENTION

20 The present invention relates generally to communication systems for remote monitoring
of patients, and in particular to a networked system for remotely monitoring patients and
for communicating information to the patients through the use of script programs. The
invention further relates to a patient monitoring and drug delivery measurement system
for measuring and electronically recording measurements of drug dose(s) administered to
a patient. The invention also relates to injection syringes adapted for use with a dose
25 measurement apparatus for electronically recording drug delivery measurements.

BACKGROUND OF THE INVENTION

Remote communication and monitoring systems

5 In the United States alone, over 100 million people have chronic health conditions, accounting for an estimated \$700 billion in annual medical costs. In an effort to control these medical costs, many healthcare providers have initiated outpatient or home healthcare programs for their patients. The potential benefits of these programs are particularly great for chronically ill patients who must treat their diseases on a daily basis.
10 However, the success of these programs is dependent upon the ability of the healthcare providers to monitor the patients remotely to avert medical problems before they become complicated and costly. Unfortunately, no convenient and cost effective monitoring system exists for those patients who have the greatest need for monitoring - the poor and the elderly.

15 Prior attempts to monitor patients remotely have included the use of personal computers and modems to establish communication between patients and healthcare providers. However, computers are too expensive to give away and the patients who already own computers are only a small fraction of the total population. Further, the patients who own
20 computers are typically young, well educated, and have good healthcare coverage. Thus, these patients do not have the greatest unmet medical needs. The patients who have the greatest unmet medical needs are the poor and elderly who do not own computers or who are unfamiliar with their use.

25 Similar attempts to establish communication between patients and healthcare providers have included the use of the Internet and internet terminals. Although internet terminals are somewhat less costly than personal computers, they are still too expensive to give away to patients. Moreover, monthly on-line access charges are prohibitive for poor patients.

30 Other attempts to monitor patients remotely have included the use of medical monitoring devices with built-in modems. Examples of such monitoring devices include blood glucose meters, respiratory flow meters, and heart rate monitors. Unfortunately, these

monitoring devices are only designed to collect physiological data from the patients. They do not allow flexible and dynamic querying of the patients for other information, such as quality of life measures or psycho-social variables of illness. Nor do they allow for remote monitoring or recording of drug dose(s) administered to, or self-administered by, a patient.

Prior attempts to monitor patients remotely have also included the use of interactive telephone or video response systems. Such interactive systems are disclosed in U.S. Patents 5,390,238 issued to Kirk et al. on February 14, 1995, 5,434,611 issued to Tamura on July 18, 1995, and 5,441,047 issued to David et al. on August 15, 1995. One disadvantage of these systems is that they either require a patient to call in to a central facility to be monitored or require the central facility to call the patient according to a rigid monitoring schedule.

If the patients are required to call the central facility, only the compliant patients will actually call regularly to be monitored. Non-compliant patients will typically wait until an emergency situation develops before contacting their healthcare provider, thus defeating the purpose of the monitoring system. If the central facility calls each patient according to a monitoring schedule, it is intrusive to the patient's life, and resistance to the monitoring program grows over time.

Another disadvantage of these conventional interactive response systems is that they are prohibitively expensive for poor patients. Further, it is difficult to identify each patient uniquely using these systems. Moreover, these systems are generally incapable of collecting medical data from monitoring devices, such as blood glucose meters, respiratory flow meters, or heart rate monitors.

Remote monitoring of drug delivery

In recent years, the value of keeping electronic medical records in place of paper records has been widely recognized in the health care industry. The use of electronic medical records allows health care providers and patients to store, retrieve, and share medical information with considerably more ease and accuracy. The sharing of medical

information is particularly important in treatment programs involving the injection of insulin, human growth hormone, or other medications.

Typically, these injections are performed using disposable syringes. Unfortunately, no adequate apparatus exists that measures and electronically records dose information from a disposable syringe. As a result, the patient or health care worker performing the injection is burdened with the task of injecting the dose and then manually recording the dose amount in a logbook.

Because of the frequency of such injections, often several times a day for diabetics, it becomes difficult for a patient to keep accurate records. Indeed, studies have shown that a patient's own records and recollections are often incomplete and inaccurate.

Additionally, a patient may intentionally cheat while making self-recorded entries in an attempt to create a logbook that will please his or her doctor. In the long-term this makes patient monitoring extremely difficult and jeopardizes the treatment program, possibly even endangering the patient's life.

Attempts have been made to develop electronic management systems for assisting patients in self-administered drug programs. For example, U.S. Patent 5,019,974 issued to Beckers describes a hand-held, microprocessor-based recorder that interfaces with a master computer. The patient enters therapy information into the recorder via a keyboard. The recorder includes a display for displaying treatment therapy guidelines to the patient. The recorder also has a blood glucose meter for recording the patient's blood glucose levels.

The recorder described by Beckers does not automatically measure and record dose information from a disposable syringe. After injecting a dose, the patient must manually enter the dose information into the recorder using switches or keys. Although this is an improvement over keeping written records on paper, the effectiveness of the drug program is still limited by the patient's recollections and recordings, which are unreliable.

Attempts have also been made to develop devices that deliver a predetermined dose of medication and record the dose amount. For example, U.S. Patent 5,176,502 issued to Sanderson et al. on January 5, 1993 describes a syringe pump for expelling a preset dose of medication from a syringe. The syringe pump includes a syringe retainer for holding the syringe and a driver for engaging the plunger of the syringe. An electric motor pushes the driver and plunger into the syringe barrel to expel the medication.

The syringe pump further includes a monitoring circuit for monitoring the motion of the driver during the delivery of the medication. The monitoring circuit includes a linear potentiometer having an electrically conductive strip of resistive material. The resistive material is positioned such that it engages an electrical contact of the driver. The position of the electrical contact on the resistive strip varies the voltage of the monitoring circuit, thus indicating the position of the plunger inside the barrel. A microprocessor receives voltage signals from the monitoring circuit and compares the voltage signals to preprogrammed signals to determine if the plunger displacement corresponds to correct displacement for delivering the preset dose. A control mechanism connected to the microprocessor regulates the driver's movement to ensure the preset dose of medication is delivered.

Although the syringe pump described by Sanderson does allow electronic recording of dose information, it is only designed to deliver medication directly into an intravenous line. It is not designed to inject a patient directly nor can it measure and record a dose from a syringe unless the syringe pump pushes the plunger. Consequently, the syringe pump is of little use to a health care worker who must inject a patient directly, or to an outpatient who must follow a self-injection treatment program.

Another device for injecting a preset dose of medication and for recording the injected dose is disclosed in U.S. Patent 4,950,246 issued to Muller on August 21, 1990. Muller describes a battery-operated injection pen having a pump rod driven by an electric motor. The electric motor is controlled by an electronic control unit that includes a

microprocessor with a memory for storing dose information. The injection pen further includes a sensor connected to the control unit for electrically determining the position of the pump rod, and thus the amount of medication injected.

- 5 Although the injection pen described by Muller measures and electronically records dose information, it has several disadvantages that have precluded its widespread use. The injection pen is an expensive device requiring complicated electronic equipment to deliver and record doses. Moreover, because the injection pen integrates a syringe and electronic recorder into one device, it is not disposable. The patient must use it
- 10 repeatedly for each injection, even after the injection pen has been contaminated with blood. Consequently, the injection pen does not provide an inexpensive, convenient, or hygienic solution to patients wishing to measure and electronically record injected dose information.
- 15 U.S. Pat. 4,853,521 to Claeys presents a programmable, intelligent reader unit, which receives and records drug data using hand-held or fixed scanners. The scanners read bar codes in place on syringes, ampoules, flow meters, etc. In addition, this intelligent reader allows the user to weigh a syringe before and after injection to determine and record the administered amount of medicine. Dosage data logged in this manner can be displayed
- 20 or printed out in the form of a record.

Operating the device described by Claeys requires many complicated steps of weighing syringes, scanning in bar codes, etc. The complexity of the required procedures, as well as the high cost of the apparatus, have precluded its widespread use. Additionally, the

25 device cannot be easily carried by the user for recording doses while away from the health care facility or home. Thus, no inexpensive apparatus exists for determining and electronically recording dose information from a disposable syringe. Further, no such apparatus exists that is both simple in operation and easily carried by a user.

The following U.S. patents are incorporated by reference herein: U.S. patent No. 5,569,212; U.S. patent No. 5,628,309; U.S. patent No. 5,704,902; U.S. patent No. 5,720,733; U.S. patent No. 5,782,814; and U.S. patent No. 5,792,117. The following patent applications are also incorporated by reference herein: Serial No. 08/972,670;
5 Serial No. 08/972,375; Serial No. 08/898,711; and Serial No. US97/12966.

OBJECTS AND ADVANTAGES OF THE INVENTION

In view of the above, it is an object of the present invention to provide a simple and inexpensive system for remotely monitoring patients and for communicating information
10 to the patients. It is another object of the invention to provide a system, which allows flexible and dynamic querying of the patients. It is a further object of the invention to provide a system, which combines querying of patients with medical device monitoring in the same monitoring session. Another object of the invention is to provide a monitoring system which incurs lower communications charges than those incurred by
15 conventional monitoring systems. A further object of the invention is to provide a monitoring system, which may be used at any time convenient for a patient.

It is a further object of the present invention to provide a system, which combines interactive communication between a healthcare provider and a patient at a remote
20 location, with measurement and paperless recordation of drug dose(s) administered to the patient. It is a further object of the invention to provide an apparatus for inductively, capacitively, or optically determining, and for electronically recording, an injection dose delivered to a patient from a disposable syringe. It is another object of the invention to provide a drug dose measurement and patient monitoring apparatus that may be easily
25 operated and carried by a user. A further object of the invention is to provide a patient monitoring and drug delivery measurement apparatus suited to diabetic patients, and to diabetes home care in particular. It is yet another object to provide an apparatus facilitating automated paperless data processing, from measurements performed by the patient to the recording at the clinic.

30 These and other objects and advantages will become more apparent after consideration of the ensuing description and the accompanying drawings.

SUMMARY OF THE INVENTION

The invention presents a networked system for remotely monitoring an individual, for
5 communicating information to the individual, and for recording patient related data
generated at a remote location. The system includes a server and a remote interface for
entering in the server a set of queries to be answered by the individual. The server is
preferably a worldwide web server and the remote interface is preferably a personal
computer or network terminal connected to the web server via the Internet. The system
10 also includes a remotely programmable apparatus for interacting with the individual. The
remotely programmable apparatus is connected to the server via a communication
network, preferably the Internet. The apparatus interacts with the individual in
accordance with a script program received from the server. The server may also receive
patient-related data from the remotely programmable apparatus via the communication
15 network.

The server includes a script generator for generating the script program from the queries
entered through the remote interface. The script program is executable by the remotely
programmable apparatus to communicate the queries to the individual, to receive
20 responses to the queries, and to transmit the responses from the remotely programmable
apparatus to the server. The server also includes a database connected to the script
generator for storing the script program and the responses to the queries.

The remotely programmable apparatus has a communication device, such as a modem,
25 for receiving the script program from the server and for transmitting the responses and/or
patient related data to the server. The remotely programmable apparatus also has a user
interface for communicating the queries to the individual and for receiving the responses
to the queries from the individual. In a preferred embodiment, the user interface includes
a display for displaying the queries and user input buttons for entering the responses to
30 the queries. In an alternative embodiment, the user interface includes a speech
synthesizer for audibly communicating the queries and a speech recognizer for receiving
spoken responses to the queries.

The remotely programmable apparatus also includes a memory for storing the script program and the responses to the queries. The remotely programmable apparatus further includes a microprocessor connected to the communication device, the user interface, and the memory. The microprocessor executes the script program to communicate the queries to the individual, to receive the responses to the queries, and to transmit the responses to the server through the communication network.

In one embodiment, the system also includes at least one monitoring device for producing measurements of a physiological condition of the individual and for transmitting the measurements to the apparatus.

According to another embodiment, a communication and monitoring system includes a patient monitoring and drug delivery measurement apparatus, in communication with the remotely programmable apparatus for providing measurements of drug dose(s) administered to, or self-administered by, a patient, wherein the communication and monitoring system includes: a server, a communications network, and a remotely programmable apparatus; and wherein the patient monitoring and drug delivery measurement apparatus includes; a dose measurement unit or element, a measuring device, a calibration memory, and a recording device.

A patient monitoring system of the invention may further include a device interface connected to the microprocessor for receiving physiological condition and/or drug delivery measurements from the drug delivery measurement apparatus. The measurements are stored in the memory and transmitted to the server with the responses to the queries. The server also preferably includes a report generator connected to the database for generating a report of the measurements and responses. The report is displayed on the remote interface.

According to one embodiment, the invention provides a system for non-invasively measuring and electronically recording a dose of a drug or medication delivered to a patient from a syringe. A currently preferred patient monitoring and drug delivery measurement system comprises apparatus for measuring and electronically recording a

dose of a drug administered to a patient from a syringe, wherein the dose delivered from the syringe may be measured inductively, capacitively, or optically. There now follows a summary description of three different embodiments of a drug dose measurement apparatus, each for use in conjunction with a patient monitoring system of the invention.

5

i) Optical dose measurement

In one embodiment of the invention, there is provided an apparatus for optically measuring a dose of a drug delivered to a patient, the apparatus including: a holding means for receiving and holding the syringe, a light source in optical communication with
10 the syringe, an optical detector in optical communication with the syringe, and a recording means in electrical communication with the optical detector. An alignment means aligns the syringe barrel to the optical detector and/or the light source, when the syringe is in a measurement position.

15 The light source generates light incident on the syringe. An optical response of the syringe to the incident light is indicative of the liquid quantity within the syringe, and implicitly of the dose administered (or to be administered) from the syringe. The optical detector detects the optical response. The recording means records a dose datum indicative of the optical response and the dose. The dose can be computed from the
20 optical response in conjunction with calibration or syringe parameter data, as will be described in detail herein below.

The incident light preferably includes wavelengths that are suitable for measuring typical plunger displacements (resolution on the order of 0.1 mm to 1 mm) and/or liquid
25 quantities within the syringe (resolution on the order of 0.1 cm³), and that interact minimally with elements of the syringe (e.g. the barrel) which do not vary with the quantity of liquid within the syringe. Such wavelengths are preferably, but generally need not be, in the visible or near-visible (infrared/ultraviolet) ranges. Preferably, the detector is suitable for detecting light within a range of wavelengths emitted by the light

source. Generally, the wavelength range emitted by the light source need not be identical to the wavelength range detected by the detector. In fact, the wavelength ranges need not even overlap, if the light detected by the detector results from absorption and re-emission by the syringe.

5

The light source and detector preferably comprise semiconductor emitting/detecting devices, but generally may include any device capable of emitting/detecting light of desired wavelengths. Such devices may include antennas or heat sensors. The recording means includes an electronic memory, preferably a digital memory unit.

10

The detector preferably includes a plurality of longitudinally spaced individual optical detecting elements coupled to the holding means and in optical communication with the syringe. The detecting elements detect an optical response pattern of the syringe, i.e. a spatial distribution of the syringe response. Dose data indicative of the optical response pattern is then recorded. The light source preferably includes plural longitudinally spaced light emitters. Each light emitter generates a light beam incident on the syringe. The optical response pattern is indicative of the interaction of the light beams with the syringe. Preferably, each of the light emitters is substantially aligned longitudinally with one of the detecting elements. If a control means in electrical communication with each of the light emitters is used to individually control each of the light emitters, a separate response pattern may be recorded for each emitter.

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In an embodiment, which does not require an internal light source, the holding means encloses the syringe only on one side. The holding means does not completely enclose the syringe on the side opposite the detector, so as to allow external light to be incident on the syringe. The response pattern detected by the detector is then dependent on the interaction between the external light and the syringe.

In one embodiment, the syringe includes a response-enhancing element comprising an optical marking. The optical response of the syringe depends on the interaction of

30

incident light with the marking, and on the position of the marking. The position of the marking is indicative of the dose. The response-enhancing element may comprise a longitudinal element mechanically coupled to (e.g. on the surface of, or within) the syringe plunger. The longitudinal element is longitudinally marked by the marking. The
5 marking may be a shape marking, or a color marking varying longitudinally in brightness and/or hue.

If the detector detects light transmitted or emitted by the syringe, the detector is situated opposite the light source relative to the syringe. If the detector detects light reflected by
10 the syringe, the detector is situated adjacent the light source relative to the syringe (on the same side of the syringe).

A port connected to the recording means allows downloading dose data histories from the recording means to a host computer (storage and communications device). A display connected to the detector and/or recording means displays dose data including current
15 doses and dose histories to the patient. Generally, the recording means may record any signal indicative of the optical response detected by the detector. For example, the recording means may record directly the optical response signal generated by the detector. Doses are then computed on a distinct computer after downloading of the recording means contents to the computer. Preferably, however, a computing means
20 computes the dose data recorded by the recording means from the optical response by the detector.

Preferably, a housing encloses the light source, detector, recording means, and monitoring means. The holding means is mechanically coupled with the housing, and is
25 preferably enclosed by the housing. The housing may be sufficiently compact to be hand-held and carried by a user, and may be battery-powered.

ii) Capacitance-based measurement

An apparatus for capacitively measuring and electronically recording a dose delivered from a syringe includes: a holder for receiving and holding a syringe in a measurement position; a capacitive element coupled to the holder and enclosing the syringe such that a
5 capacitive response of the capacitive element is indicative of the dose when the syringe is in the measurement position; a measuring device connected to the capacitive element for measuring capacitive responses of the capacitive element; and a recording device connected to the measuring device for recording a dose datum indicative of the capacitive response and thus indicative of the dose.

10 Preferably, the holder includes a well, the well laterally enclosing the syringe when the syringe is in the measurement position. The capacitive element is then coupled to the well such that at least one electrode of the capacitive element laterally encloses the syringe when the syringe is in the measurement position. In one embodiment, the
15 capacitive element is defined between the liquid held in the syringe and an external electrode situated outside the syringe. A needle contact coupled to the holder is then used to establish electrical communication between the measuring device and the liquid, through the syringe needle, when the syringe is in the measurement position. In another embodiment, the capacitive element is defined between first and second electrically
20 conducting longitudinal plates coupled to the holder, electrically insulated from each other, and situated opposite each other relative to the syringe.

In yet another embodiment, the capacitive element is situated entirely within the syringe. Two coaxial cylindrical electrodes, one near the inside surface of the syringe barrel and
25 the other near the outside surface of the syringe plunger, are connected to input and output terminals on the outside of the syringe barrel. The housing includes a contact field coupled to the outside of the housing. The contact field includes an input contact for contacting the input terminal, and an output contact for contacting the output terminal. The input and output contacts are connected to the measuring device.

A housing encloses the measuring and recording devices, and preferably encloses and magnetically shields the capacitive element. The holder is mechanically coupled to the housing. The housing is sufficiently compact to be hand-held and carried by a user. The
5 capacitive element preferably consists of a single capacitor, and the capacitive response preferably includes the capacitance of the capacitor. In an alternative embodiment, the capacitive element includes plural longitudinally-spaced capacitors, and the capacitive response includes a capacitive response pattern.

10 iii) Inductance-based dose measurement

An apparatus for inductively measuring and electronically recording a dose delivered using a syringe includes: a holder for receiving and holding a syringe in a measurement position; an inductive element coupled to the holder and enclosing the syringe such that
15 an inductive response of the inductive element is indicative of the dose when the syringe is in the measurement position; a measuring device connected to the inductive element for measuring inductive responses of the inductive element; and a recording device connected to the measuring device for recording a dose datum indicative of the inductive response and thus indicative of the dose.

20 Preferably, the holder includes a well laterally enclosing the syringe when the syringe is in the measurement position. The inductor is then coupled to the well such that the inductor laterally encloses the syringe when the syringe is in the measurement position. It is preferred that the syringe includes an inductance-enhancing element whose position relative to the syringe barrel is indicative of the dose, and whose position determines the
25 inductive response of the inductive element. The inductance-enhancing element preferably includes a ferromagnetic or ferromagnetic longitudinal plunger element embedded in a plastic shell to form the syringe plunger. The inductance-enhancing element preferably includes a ferrite strip, but may comprise a ferromagnetic core filling the plunger cross-section almost entirely, or a series of longitudinally spaced, stacked

disks arranged within the plunger. Alternatively, a conventional syringe having a plunger consisting essentially of a plastic rod may be used.

5 A housing encloses the measuring and recording devices, and preferably encloses and magnetically shields the inductive element. The holder is mechanically coupled to the housing. The housing is sufficiently compact to be hand-held and carried by a user. The inductive element preferably consists of a single inductor, and the inductive response preferably includes the inductance of the inductor. In an alternative embodiment, the inductive element includes plural longitudinally spaced inductors, and the inductive
10 response includes an inductive response pattern.

In one embodiment, the inductor is situated within the syringe barrel and is connected to input and output terminals on the outside of the syringe. The housing then includes a contact field coupled to the outside of the housing. The contact field includes an input
15 contact for contacting the input terminal, and an output contact for contacting the output terminal.

For both inductive and capacitive measurement embodiments of the monitoring system, a port connected to the recording device may be used to download data stored in the
20 recording device to an external storage or communication device, such as a host computer. Also connected to the recording device is a monitoring or testing device for testing a physical or physiological condition of the patient and for generating condition data representative of the physical or physiological condition. The recording device records the condition data. Preferably, the monitoring or testing device is a blood glucose
25 meter and the physical or physiological condition is the patient's blood glucose level. A display connected to the measuring device is used to display recorded doses and blood glucose levels to the patient.

A computing device is connected to the recording device. The computing device
30 computes dose data from dose measurement responses (capacitive, inductive, or optical)

and stored calibration data, for storage in the recording device. Dose data preferably includes administered doses. The calibration data, stored in a calibration memory device, is indicative of the correspondence between dose measurement responses and dose data for the particular syringe used by the patient. The calibration data is generated by measuring dose measurement responses for the entire range of potential liquid quantities in the syringe, and recording the correspondence between liquid quantities and dose measurement responses.

BRIEF DESCRIPTION OF THE DRAWINGS

Fig. 1 is a block diagram of a networked system according to one embodiment of the invention.

Fig. 2 is a block diagram illustrating the interaction of the components of the system of Fig. 1.

Fig. 3 is a perspective view of a remotely programmable apparatus of the system of Fig. 1.

Fig. 4 is a block diagram illustrating the components of the remotely programmable apparatus of Fig. 3.

Fig. 5 is a script entry screen according to a preferred embodiment of the invention.

Fig. 6A is a listing of a sample script program according to a preferred embodiment of the invention.

Fig. 6B is a continuation of the listing of Fig. 6A.

Fig. 7 is a script assignment screen according to a preferred embodiment of the invention.

Fig. 8 is a sample query appearing on a display of the apparatus of Fig. 3.

Fig. 9 is a sample prompt appearing on the display of the apparatus of Fig. 3.

Fig. 10 is a sample report displayed on a workstation of the system of Fig. 1.

Fig. 11A is a flow chart illustrating the steps included in a monitoring application executed by the server of Fig. 1 according to a preferred embodiment of the invention.

Fig. 11B is a continuation of the flow chart of

Fig. 11A.

Fig. 12A is a flow chart illustrating the steps included in the script program of Figs. 6A-6B.

Fig. 12B is a continuation of the flow chart of

5 Fig. 12A.

Fig. 13 is a perspective view of a remotely programmable apparatus according to a second embodiment of the invention.

Fig. 14 is a sample prompt appearing on a display of the apparatus of Fig. 13.

Fig. 15 is a block diagram illustrating the components of the apparatus of Fig. 13.

10 Fig. 16 is a schematic block diagram illustrating the interaction of the server of Fig. 1 with the apparatus of Fig. 3 according to a third embodiment of the invention.

Fig. 17 is a first sample message appearing on the display of the apparatus of Fig. 3.

15 Fig. 18 is a second sample message appearing on the display of the apparatus of Fig. 3.

Fig. 19 is a script entry screen according to the third embodiment of the invention.

Fig. 20A is a block diagram of a networked monitoring system including a remote patient monitoring and drug dose measurement apparatus, according to another embodiment of the invention.

20 Fig. 20B is a high-level schematic diagram illustrating a patient monitoring and drug delivery measurement apparatus of the system of Fig. 20A, according to the invention.

Fig. 21 is a perspective view of a drug delivery measurement apparatus according to another embodiment of the invention.

25 Fig. 22A is a longitudinal sectional view of a syringe situated in a measurement position within a holder of the apparatus of Fig. 21, according to one embodiment of the invention.

Fig. 22B is a transverse sectional view of the holder and syringe of Fig. 22A.

30 Fig. 23A is a longitudinal sectional view of a syringe, holder, and capacitor arrangement, according to another embodiment of the invention.

Fig. 23B is a transverse sectional view of the holder and syringe of Fig. 23A.

Fig. 24A is a perspective view of an apparatus suitable for use with a syringe, the apparatus comprising an internal capacitor, according to one embodiment of the invention.

5 Fig. 24B is a longitudinal sectional view of a syringe capacitor geometry suitable for use with the apparatus of Fig. 24A.

Fig. 25 is a high-level schematic diagram illustrating a patient monitoring and drug delivery measurement apparatus according to another embodiment of the invention.

Fig. 26 is a perspective view of a drug delivery measurement apparatus according to another embodiment of the invention.

10 Fig. 27A is a longitudinal sectional view of a syringe suitable for use with the apparatus of Fig. 24A.

Fig. 27B is a transverse sectional view of the syringe of Fig. 27A.

Fig. 28 is a longitudinal sectional view of an inductance-enhanced syringe of the invention.

15 Fig. 29A is a longitudinal section view of a multi-inductor element according to the invention.

Fig. 29B is a longitudinal section view of another multi-inductor element according to the invention.

20 Fig. 30A illustrates qualitatively the dependence of inductance with plunger displacement for the geometry shown in Fig. 26.

Fig. 30B illustrates qualitatively the dependence of inductance with plunger displacement for each inductor in the geometry of Fig. 29A.

Fig. 31A is a high-level schematic diagram illustrating a patient monitoring and drug delivery measurement apparatus, according to another embodiment of the invention.

25 Fig. 31B illustrates broadly the principal detection step performed by the apparatus of Fig. 31A.

Fig. 32A is a perspective view of a drug delivery measurement apparatus according to another embodiment of the invention.

Fig. **32B** is a longitudinal sectional view of a syringe situated in a measurement position in a holder of the apparatus of Fig. **32A**, illustrating a preferred light source and detector arrangement.

Fig. **32C** shows a detail of Fig. **32B**, including the plunger-liquid interface within the syringe.

Fig. **32D** shows an alternative light source and detector arrangement in a view similar to that of Fig. **32C**, according to the invention.

Fig. **32E** shows another alternative light source and detector arrangement in a view similar to that of Fig. **32C**, according to the invention.

Fig. **33A** shows an apparatus, which does not require an internal light source, according to another embodiment of the invention.

Fig. **33B** shows a longitudinal sectional view of a syringe situated in a measurement position in a holder of the apparatus of Fig. **33A**.

Fig. **34** shows a perspective view of a drug delivery measurement apparatus and a syringe adapted for use with the apparatus, according to another embodiment of the invention.

DETAILED DESCRIPTION

The invention presents a system and method for remotely monitoring individuals, for communicating information to the individuals, and for receiving data from an individual at a remote location. In a preferred embodiment of the invention, the individuals are patients and the system is used to collect data relating to the health status or medical treatment of the patients. However, it is to be understood that the invention is not limited to remote monitoring of patients or patient-related activities. The system and method of the invention may be used for any type of remote monitoring application. The invention may also be implemented as an automated messaging system for communicating information to individuals, as will be discussed in an alternative embodiment below.

A system and method for remote interactive communication and remote monitoring of individuals will first be described with reference to Figs. **1-19**. Thereafter, a system for patient monitoring and drug delivery measurement, including a drug delivery

measurement apparatus for use in conjunction with the interactive communication and remote monitoring system, will be described with reference to Figs. **20A-34**.

A preferred embodiment of the invention is illustrated in Figs. **1-12**. Referring to Fig. **1**,
5 a networked system **16** includes a server **18** and a workstation **20** connected to server **18**
through a communication network **24**. Server **18** is preferably a worldwide web server
and communication network **24** is preferably the Internet. It will be apparent to one
skilled in the art that server **18** may comprise a single stand-alone computer or multiple
10 computers distributed throughout a network. Workstation **20** is preferably a personal
computer, remote terminal, or web TV unit connected to server **18** via the Internet.
Workstation **20** functions as a remote interface for entering in server **18** messages and
queries to be communicated to the patients.

System **16** also includes a plurality of remotely programmable apparatuses, schematically
15 represented in Fig. **1** as **26a** and **26x** for monitoring a corresponding plurality of patients.
Each remotely programmable apparatus **26a-x** is designed to interact with a patient in
accordance with script programs received from server **18**. Each remotely programmable
apparatus **26a-x** is in communication with server **18** through communication network **24**,
preferably the Internet. Alternatively, each apparatus, e.g., **26a**, may be placed in
20 communication with server **18** via wireless communication networks, cellular networks,
telephone networks, or any other network which allows each remotely programmable
apparatus **26a** to exchange data with server **18**. For clarity of illustration, only two
remotely programmable apparatus **26a**s are shown in Fig. **1**. However, it is to be
understood that system **16** may include any number of remotely programmable apparatus
25 **26a-x** for monitoring any number of patients.

Each patient to be monitored may be provided with a monitoring device **28a-x**, designed
to provide measurements of a physiological condition of the patient, to record the
physiological condition measurements, and to transmit the measurements to the patient's
30 remotely programmable apparatus **26a-x**, e.g., through a standard connection cable **30**.
Examples of suitable types of monitoring devices include blood glucose meters,
respiratory flow meters, blood pressure cuffs, electronic weight scales, and pulse rate
monitors. Such monitoring devices are well known in the art. The specific type of

monitoring device provided to each patient is dependent upon the patient's disease. For example, diabetes patients are provided with a blood glucose meters for measuring blood glucose concentrations, asthma patients are provided with respiratory flow meters for measuring peak flow rates, obesity patients are provided with weight scales, etc.

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Fig. 2 shows server 18, workstation 20, and remotely programmable apparatus 26a-x in greater detail. Server 18 includes a database 38 for storing script programs 40. The script programs are executed by each remotely programmable apparatus to communicate queries and messages to a patient, receive responses 42 to the queries, collect monitoring device measurements 44, and transmit responses 42 and measurements 44 to server 18. Database 38 is designed to store the responses 42 and measurements 44. Database 38 further includes a look-up table 46. Table 46 contains a list of the patients to be monitored, and for each patient, a unique patient identification code and a respective pointer to the script program assigned to the patient. Each remotely programmable apparatus 26a-x is designed to execute assigned script programs, which it receives from server 18.

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Figs. 3-4 show the structure of each remotely programmable apparatus according to a preferred embodiment. For clarity, only remotely programmable apparatus 26a is shown in Figs. 3-4, since each remotely programmable apparatus 26a-x has substantially the same structure as remotely programmable apparatus 26a. Referring to Fig. 3, remotely programmable apparatus 26a includes a housing 62. Housing 62 is sufficiently compact to enable apparatus 26a to be hand-held and carried by a patient. Remotely programmable apparatus 26a also includes a display 64 for displaying queries and prompts to the patient. In a preferred embodiment, display 64 is a liquid crystal display (LCD).

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Four user input buttons 70A, 70B, 70C, and 70D are located adjacent display 64. User input buttons 70A-C are for entering in remotely programmable apparatus 26a responses to the queries and prompts. In a preferred embodiment, user input buttons 70A-C are momentary contact push buttons. In alternative embodiments, user input buttons 70A-C may be replaced by switches, keys, a touch sensitive display screen, or any other data input device.

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Three monitoring device jacks **68A**, **68B**, and **68C** are located on a surface of housing **62**. The device jacks are for connecting remotely programmable apparatus **26a** to a number of monitoring devices, such as blood glucose meters, respiratory flow meters, or blood pressure cuffs, through respective connection cables (not shown). Apparatus **26a** also includes a modem jack **66** for connecting apparatus **26a** to a telephone jack through a standard connection cord (not shown). Apparatus **26a** further includes a visual indicator, such as a light emitting diode (LED) **74**. LED **74** is for visually notifying the patient that he or she has unanswered queries stored in remotely programmable apparatus **26a**.

Fig. **4** is a schematic block diagram illustrating the components of apparatus **26a** in greater detail. Apparatus **26a** includes a microprocessor **76** and a memory **80** connected to microprocessor **76**. Memory **80** is preferably a non-volatile memory, such as a serial EEPROM. Memory **80** stores script programs received from the server, measurements received from monitoring device **28**, responses to queries, and the patient's unique identification code. Microprocessor **76** also includes built-in read only memory (ROM) which stores firmware for controlling the operation of apparatus **26a**. The firmware includes a script interpreter used by microprocessor **76** to execute the script programs. The script interpreter interprets script commands, which are executed by microprocessor **76**. Specific techniques for interpreting and executing script commands in this manner are well known in the art.

Microprocessor **76** is preferably connected to memory **80** using a standard two-wire I²C interface. Microprocessor **76** is also connected to user input buttons **70**, LED **74**, a clock **84**, and a display driver **82**. Clock **84** indicates the current date and time to microprocessor **76**. For clarity of illustration, clock **84** is shown as a separate component, but is preferably built into microprocessor **76**. Display driver **82** operates under the control of microprocessor **76** to display information on display **64**. Microprocessor **76** is preferably a PIC 16C65 processor, which includes a universal asynchronous receiver transmitter (UART) **78**. UART **78** is for communicating with a modem **86** and a device interface **90**. A CMOS switch **88** under the control of microprocessor **76** alternately connects modem **86** and interface **90** to UART **78**.

Modem **86** is connected to a telephone jack **22** through modem jack **66**. Modem **86** is for exchanging data with server **18** through communication network **24**. The data includes script programs, which are received from server **18** as well as responses to queries, device measurements, script identification codes, and the patient's unique identification code
5 which modem **86** transmits to server **18**. Modem **86** is preferably a complete 28.8 K modem commercially available from Cermetek, although any suitable modem may be used.

Device interface **90** is connected to device jacks **68A**, **68B**, and **68C**. Device interface **90**
10 is for interfacing with a number of monitoring devices, such as blood glucose meters, respiratory flow meters, blood pressure cuffs, weight scales, or pulse rate monitors, through device jacks **68A-C**. Device interface **90** operates under the control of microprocessor **76** to collect measurements from the monitoring devices and to output the measurements to microprocessor **76** for storage in memory **80**. In a preferred
15 embodiment, interface **90** is a standard RS232 interface. For simplicity of illustration, only one device interface is shown in Fig. 4. However, in alternative embodiments, remotely programmable apparatus **26a** may include multiple device interfaces to accommodate monitoring devices, which have different connection standards.

Referring again to Fig. 2, server **18** includes a monitoring application **48**. Monitoring
20 application **48** is a controlling software application executed by server **18** to perform the various functions described below. Application **48** includes a script generator **50**, a script assignor **52**, and a report generator **54**. Script generator **50** is designed to generate script programs **40** from script information entered through workstation **20**. The script
25 information is entered through a script entry screen **56**. In a preferred embodiment, script entry screen **56** is implemented as a web page on server **18**. Workstation **20** includes a web browser for accessing the web page to enter the script information.

Fig. 5 illustrates script entry screen **56** as it appears on workstation **20**. Screen **56**
30 includes a script name field **92** for specifying the name of a script program to be generated. Screen **56** also includes entry fields **94** for entering a set of queries to be answered by a patient. Each entry field **94** has corresponding response choice fields **96** for entering response choices for the query. Screen **56** further includes check boxes **98**

for selecting a desired monitoring device from which to collect measurements, such as a blood glucose meter, respiratory flow meter, or blood pressure cuff.

Screen **56** additionally includes a connection time field **100** for specifying a prescribed connection time at which each remotely programmable apparatus **26a-x** executing the script is to establish a subsequent communication link to server **18**. The connection time is preferably selected to be the time at which communication rates are the lowest, such as 3:00 AM. Screen **56** also includes a CREATE SCRIPT button **102** for instructing the script generator to generate a script program from the information entered in screen **56**. Screen **56** further includes a CANCEL button **104** for canceling the information entered in screen **56**.

In a preferred embodiment, each script program created by the script generator conforms to the standard file format used on UNIX systems. In the standard file format, each command is listed in the upper case and followed by a colon. Every line in the script program is terminated by a linefeed character {LF}, and only one command is placed on each line. The last character in the script program is a UNIX end of file character {EOF}. Table 1 shows an exemplary listing of script commands used in a preferred embodiment of the invention.

TABLE 1 - SCRIPT COMMANDS

Command	Description
CLS: {LF}	Clear the display.
ZAP: {LF}	Erase from memory the last set of query responses recorded.
LED: b{LF}	Turn the LED on or off, where b is a binary digit of 0 or 1. An argument of 1 turns on the LED, and an argument of 0 turns off the LED.
DISPLAY: {chars} {LF}	Display the text following the DISPLAY command.

INPUT: mmmm{LF}	Record a button press. The m's represent a button mask pattern for each of the four input buttons. Each m contains an "X" for disallowed buttons or an "O" for allowed buttons. For example, INPUT: OXOX{LF} allows the user to press either button #1 or #3.
WAIT: {LF}	Wait for any one button to be pressed, then continue executing the script program.
COLLECT: device{LF}	Collect measurements from the monitoring device specified in the COLLECT command. The user is preferably prompted to connect the specified monitoring device to the apparatus and press a button to continue.
NUMBER: aaaa{LF}	Assign a script identification code to the script program. The script identification code from the most recently executed NUMBER statement is subsequently transmitted to the server along with the query responses and device measurements. The script identification code identifies to the server which script program was most recently executed by the remote apparatus.
DELAY: t {LF}	Wait until time t specified in the DELAY command, usually the prescribed connection time.
CONNECT: {LF}	Perform a connection routine to establish a communication link to the server, transmit the patient identification code, query responses, device measurements, and script identification code to the server, and receive and store a new script program. When the server instructs the apparatus to disconnect, the script interpreter is restarted, allowing the new script program to execute.

The script commands illustrated in Table 1 are representative of the preferred embodiment and are not intended to limit the scope of the invention. After consideration of the ensuing description, it will be apparent to one skilled in the art many other suitable scripting languages and sets of script commands may be used to implement the invention.

Script generator **50** preferably stores a script program template, which it uses to create each script program. To generate a script program, script generator **50** inserts into the

template the script information entered in screen **56**. For example, Figs. **6A-6B** illustrate a sample script program created by script generator **50** from the script information shown in Fig. **5**.

- 5 The script program includes display commands to display the queries and response choices entered in fields **94** and **96**, respectively. The script program also includes input commands to receive responses to the queries. The script program further includes a collect command to collect device measurements from the monitoring device **28a-x** specified in check boxes **98**. The script program also includes commands to establish a
10 subsequent communication link to server **18** at the connection time specified in field **100**. The steps included in the script program are also shown in the flow chart of Figs. **12A-12B** and will be discussed in the operation section below.

- Referring again to Fig. **2**, script assignor **52** is for assigning script programs **40** to the
15 patients. Script programs **40** are assigned in accordance with script assignment information entered through workstation **20**. The script assignment information is entered through a script assignment screen **57**, which is preferably implemented as a web page on server **18**.

- 20 Fig. **7** illustrates a sample script assignment screen **57** as it appears on workstation **20**. Screen **57** includes check boxes **106** for selecting a script program to be assigned and check boxes **108** for selecting the patients to whom the script program is to be assigned. Screen **57** also includes an ASSIGN SCRIPT button **112** for entering the assignments. When button **112** is activated, the script assignor creates and stores for each patient
25 selected in check boxes **108** a respective pointer to the script program selected in check boxes **106**. Each pointer is stored in the patient look-up table of the database. Screen **57** further includes an ADD SCRIPT button **110** for accessing the script entry screen and a DELETE SCRIPT button **114** for deleting a script program.

- 30 Referring again to Fig. **2**, report generator **54** is designed to generate a patient report **58** from the responses and device measurements received in server **18**. Patient report **58** is displayed on workstation **20**. Fig. **10** shows a sample patient report **58** produced by report generator **54** for a selected patient. Patient report **58** includes a graph **116** of the

device measurements received from the patient, as well as a listing of responses 42 received from the patient. Specific techniques for writing a report generator program to display data in this manner are well known in the art.

5 The operation of a preferred embodiment is illustrated in Figs. 1-12. Fig. 11A is a flow chart illustrating steps included in the monitoring application executed by server 18. Fig. 11B is a continuation of the flow chart of Fig. 11A. In step 202, server 18 determines if new script information has been entered through script entry screen 56. If new script information has not been entered, server 18 proceeds to step 206. If new script
10 information has been entered, server 18 proceeds to step 204.

As shown in Fig. 5, the script information includes a set of queries, and for each of the queries, corresponding response choices. The script information also includes a selected monitoring device type from which to collect device measurements. The script
15 information further includes a prescribed connection time for each remotely programmable apparatus 26a to establish a subsequent communication link to server 18. The script information is generally entered in server 18 by a healthcare provider, such as the patients' physician or case manager. Of course, any person desiring to communicate with the patients may also be granted access to server 18 to create and assign script
20 programs. Further, it is to be understood that system 16 may include any number of remote interfaces for entering script generation and script assignment information in server 18.

In step 204, script generator 50 generates a script program from the information entered
25 in screen 56. The script program is stored in database 38. Steps 202 and 204 are preferably repeated to generate multiple script programs, e.g. a script program for diabetes patients, a script program for asthma patients, etc. Each script program corresponds to a respective one of the sets of queries entered through script entry screen 56. Following step 204, server 18 proceeds to step 206.

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In step 206, server 18 determines if new script assignment information has been entered through assignment screen 57. If new script assignment information has not been entered, server 18 proceeds to step 210. If new script assignment information has been

entered, server **18** proceeds to step **208**. As shown in Fig. 7, the script programs are assigned to each patient by selecting a script program through check boxes **106**, selecting the patients to whom the selected script program is to be assigned through check boxes **108**, and pressing the ASSIGN SCRIPT button **112**. When button **112** is pressed, script assignor **52** creates for each patient selected in check boxes **108** a respective pointer to the script program selected in check boxes **106**. In step **208**, each pointer is stored in look-up table **46** of database **38**. Following step **208**, server **18** proceeds to step **210**.

In step **210**, server **18** determines if any of the remotely programmable apparatus **26a**s are remotely connected to server **18**. Each patient to be monitored is preferably provided with his or her own remotely programmable apparatus **26a-x** which has the patient's unique identification code stored therein. Each patient is thus uniquely associated with a respective one of apparatus **26a-x**. If none of remotely programmable apparatus **26a-x** is connected, server **18** proceeds to step **220**.

If an apparatus **26a-x** is connected, server **18** receives from that remotely programmable apparatus the patient's unique identification code in step **212**. In step **214**, server **18** receives from the remotely programmable apparatus **26a** the query responses **42**, device measurements **44**, and script identification code recorded during execution of a previously assigned script program. The script identification code identifies to server **18** which script program was executed by the apparatus **26a-x** to record the query responses and device measurements. The responses, device measurements, and script identification code are stored in database **38**.

In step **216**, server **18** uses the patient identification code to retrieve from table **46** the pointer to the script program assigned to the patient. Server **18** then retrieves the assigned script program from database **38**. In step **218**, server **18** transmits the assigned script program to the patient's remotely programmable apparatus **26a-x** through communication network **24**. Following step **218**, server **18** proceeds to step **220**.

In step **220**, server **18** determines if a patient report request has been received from workstation **20**. If no report request has been received, server **18** returns to step **202**. If a report request has been received for a selected patient, server **18** retrieves from database

38 the measurements and query responses last received from the patient, step 222. In step 224, server 18 generates and displays patient report 58 on workstation 20. As shown in Fig. 10, report 58 includes the device measurements and query responses last received from the patient. Following step 224, server 18 returns to step 202.

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Figs. 12A-12B illustrate the steps included in the script program executed by remotely programmable apparatus, e.g., 26a. Before the script program is received, remotely programmable apparatus 26a is initially programmed with the patient's unique identification code and the script interpreter used by microprocessor 76 to execute the script program. The initial programming may be achieved during manufacture of apparatus 26a or during an initial connection to server 18. Following initial programming, remotely programmable apparatus 26a receives from server 18 the script program assigned to the patient associated with remotely programmable apparatus 26a. The script program is received by modem 86 through a first communication link and stored in memory 80.

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In step 302, microprocessor 76 assigns a script identification code to the script program and stores the script identification code in memory 80. The script identification code is subsequently transmitted to server 18 along with the query responses and device measurements to identify to server 18 which script program was most recently executed by apparatus 26a. In step 304, microprocessor 76 lights LED 74 to notify the patient that he or she has unanswered queries stored in remotely programmable apparatus 26a. LED 74 preferably remains lit until the queries are answered by the patient. In step 306, microprocessor 76 erases from memory 80 the last set of query responses recorded.

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In step 308, microprocessor 76 prompts the patient by displaying on display 64 "ANSWER QUERIES NOW? PRESS ANY BUTTON TO START". In step 310, microprocessor 76 waits until a reply to the prompt is received from the patient. When a reply is received, microprocessor 76 proceeds to step 312. In step 312, microprocessor 76 executes successive display and input commands to display the queries and response choices on display 64 and to receive responses to the queries.

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Fig. 8 illustrates a sample query and its corresponding response choices as they appear on display 64. The response choices are positioned on display 64 such that each response choice is located proximate a respective one of the input buttons 70A-D. In the preferred embodiment, each response choice is displayed immediately above a respective input button 70A-D. The patient presses the button (70A-D) corresponding to his or her response. Microprocessor 76 stores each response in memory 80.

In steps 314 - 318, microprocessor 76 executes commands to collect device measurements from a selected monitoring device 28a-x. The script program specifies the selected monitoring device 28a-x from which to collect the measurements. In step 314, microprocessor 76 prompts the patient to connect a selected monitoring device 28a-x, for example a blood glucose meter, to one of device jacks 68A-C. A sample prompt is shown in Fig. 9. In step 316, microprocessor 76 waits until a reply to the prompt is received from the patient. When a reply is received, microprocessor 76 proceeds to step 318. Microprocessor 76 also connects UART 78 to interface 90 through switch 88. In step 318, microprocessor 76 collects the device measurements from monitoring device 28a-x through interface 90. The measurements are stored in memory 80.

In step 320, microprocessor 76 prompts the patient to connect remotely programmable apparatus 26a to telephone jack 22 so that remotely programmable apparatus 26a may connect to server 18 at the prescribed connection time. In step 322, microprocessor 76 waits until a reply to the prompt is received from the patient. When a reply is received, microprocessor 76 turns off LED 74 in step 324. In step 326, microprocessor 76 waits until it is time to connect to server 18. Microprocessor 76 compares the connection time specified in the script program to the current time output by clock 84. When it is time to connect, microprocessor 76 connects UART 78 to modem 86 through switch 88.

In step 328, microprocessor 76 establishes a subsequent communication link between apparatus 26a and server 18 through modem 86 and communication network 24. If the connection fails for any reason, microprocessor 76 repeats step 328 to get a successful connection. In step 330, microprocessor 76 transmits the device measurements, query responses, script identification code, and patient identification code stored in memory 80 to server 18 through the subsequent communication link. In step 332, microprocessor 76

receives through modem **86** a new script program from server **18**. The new script program is stored in memory **80** for subsequent execution by microprocessor **76**. Following step **332**, the script program ends.

5 One advantage of the monitoring system **16** of the present invention is that it allows each patient to select a convenient time to respond to the queries, so that the monitoring system is not intrusive to the patient's schedule. A second advantage of monitoring system **16** is that it incurs very low communications charges because each remote apparatus **26a-x** connects to server **18** at times when communication rates are lowest.
10 Moreover, the cost to manufacture each remote apparatus **26a-x** is very low compared to personal computers or internet terminals.

A third advantage of the monitoring system is that it allows each apparatus **26a-x** to be programmed remotely through script programs. Patient surveys, connection times,
15 display prompts, selected monitoring devices, patient customization, and other operational details of each remotely programmable apparatus **26a-x** may be easily changed by transmitting a new script program to the apparatus **26a-x**. Moreover, each script program may be easily created and assigned by remotely accessing server **18** through the Internet. Thus, the invention provides a powerful, convenient, and
20 inexpensive system for remotely monitoring a large number of patients.

Figs. **13-15** illustrate a second embodiment of the invention in which each remotely programmable apparatus has speech recognition and speech synthesis functionality. Fig. **13** shows a perspective view of a remotely programmable apparatus **27** according to the
25 second embodiment. Apparatus **27** includes a speaker **72** for audibly communicating queries and prompts to the patient. Apparatus **27** also includes a microphone **118** for receiving spoken responses to the queries and prompts. Apparatus **27** may optionally include a display **64** for displaying prompts to the patient, as shown in Fig. **14**.

30 Fig. **15** is a schematic block diagram illustrating the components of remotely programmable apparatus **27** in greater detail. Apparatus **27** is similar in design to remotely programmable apparatus **26a** of the preferred embodiment, except that remotely

programmable apparatus 27 includes an audio processor chip 120 in place of microprocessor 76. Audio processor chip 120 is can be an RSC-164 chip, such as is commercially available from Sensory Circuits Inc., San Jose, CA.

5 Audio processor chip 120 has a microcontroller 122 for executing script programs received from server 18. A memory 80 is connected to microcontroller 122. Memory 80 stores the script programs and a script interpreter used by microcontroller 122 to execute the script programs. Memory 80 also stores measurements received from monitoring device 28, responses to the queries, script identification codes, and the patient's unique
10 identification code.

Audio processor chip 120 also has built in speech synthesis functionality for synthesizing queries and prompts to a patient through speaker 72. For speech synthesis, chip 120 includes a digital to analog converter (DAC) 142 and an amplifier 144. DAC 142 and
15 amplifier 144 drive speaker 72 under the control of microcontroller 122.

Audio processor chip 120 further has built in speech recognition functionality for recognizing responses spoken into microphone 118. Audio signals received through microphone 118 are converted to electrical signals and sent to a preamp and gain control circuit 128. Preamp and gain control circuit 128 is controlled by an automatic gain control circuit 136, which is in turn controlled by microcontroller 122. After being
20 amplified by preamp 128, the electrical signals enter chip 120 and pass through a multiplexer 130 and an analog to digital converter (ADC) 132. The resulting digital signals pass through a digital logic circuit 134 and enter microcontroller 122 for speech
25 recognition.

Audio processor chip 120 also includes a RAM 138 for short term memory storage and a ROM 140 which stores programs executed by microcontroller 122 to perform speech recognition and speech synthesis. Chip 120 operates at a clock speed determined by a
30 crystal 126. Chip 120 also includes a clock 84, which provides the current date and time to microcontroller 122. As in a preferred embodiment, apparatus 27 includes an LED 74, display driver 82, modem 86, and device interface 90, all of which are connected to microcontroller 122.

The operation of the second embodiment is similar to the operation of the preferred embodiment except that queries, response choices, and prompts are audibly communicated to the patient through speaker **72** rather than being displayed to the patient on display **64**. The operation of the second embodiment also differs from the operation of the preferred embodiment in that responses to the queries and prompts are received through microphone **118** rather than through user input buttons **76A-D**.

The script programs of the second embodiment are similar to the script program shown in Figs. **6A-6B**, except that each display command is replaced by a speech synthesis command and each input command is replaced by a speech recognition command. The speech synthesis commands are executed by microcontroller **122** to synthesize the queries, response choices, and prompts through speaker **72**. The speech recognition commands are executed by microcontroller **122** to recognize responses spoken into microphone **118**.

For example, to ask the patient how he or she feels and record a response, microcontroller **122** first executes a speech synthesis command to synthesize through speaker **72** "How do you feel? Please answer with one of the following responses: very bad, bad, good, or very good." Next, microcontroller **118** executes a speech recognition command to recognize the response spoken into microphone **118**. The recognized response is stored in memory **80** and subsequently transmitted to server **18**. Other than the differences described, the operation and advantages of the second embodiment are the same as the operation and advantages of the preferred embodiment described above.

Although the first and second embodiments focus on querying individuals and collecting responses to the queries, the system of the invention is not limited to querying applications. The system may also be used simply to communicate messages to the individuals. Figs. **16-19** illustrate a third embodiment in which the system is used to perform this automated messaging function. In the third embodiment, each script program contains a set of statements to be communicated to an individual rather than a set of queries to be answered by the individual. Of course, it will be apparent to one

skilled in the art that the script programs may optionally include both queries and statements.

5 The third embodiment also shows how the queries and statements may be customized to each individual by merging personal data with the script programs, much like a standard mail merge application. Referring to Fig. 16, personal data relating to each individual is preferably stored in look-up table 46 of database 38. By way of example, the data may include each individual's name, the name of each individual's physician, test results, appointment dates, or any other desired data. As in the preferred embodiment, database
10 38 also stores generic script programs 40 created by script generator 50.

Server 18 includes a data merge program 55 for merging the data stored in table 46 with generic script programs 40. Data merge program 55 is designed to retrieve selected data from table 46 and to insert the data into statements in generic script programs 40, thus
15 creating custom script programs 41. Each custom script program 41 contains statements, which are customized to an individual. For example, the statements may be customized with the individual's name, test results, etc. Examples of such customized statements are shown in Figs. 17-18.

20 The operation of the third embodiment is similar to the operation of the preferred embodiment except that the script programs are used to communicate messages to the individuals rather than to query the individuals. Each message is preferably a set of statements. Referring to Fig. 19, the statements may be entered in server 18 through script entry screen 56, just like the queries of the preferred embodiment.

25 Each statement preferably includes one or more insert commands specifying data from table 46 to be inserted into the statement. The insert commands instruct data merge program 55 to retrieve the specified data from database 38 and to insert the data into the statement. For example, the insert commands shown in Fig. 19 instruct the data merge
30 program to insert a physician name, an appointment date, a patient name, and a test result into the statements. As in the preferred embodiment, each statement may also include one or more response choices, which are entered in fields 96.

Following entry of the statements and response choices, CREATE SCRIPT button **102** is pressed. When button **102** is pressed, script generator **50** generates a generic script program from the information entered in screen **56**. The generic script program is similar to the script program shown in Figs. **6A-6B**, except that the display commands specify statements to be displayed rather than queries. Further, the statements include insert commands specifying data to be inserted into the script program. As in the preferred embodiment, multiple script programs are preferably generated, e.g. a generic script program for diabetes patients, a generic script program for asthma patients, etc. The generic script programs are stored in database **38**.

Following generation of the generic script programs, server **18** receives script assignment information entered through script assignment screen **57**. As shown in Fig. **7**, the script programs are assigned by first selecting one of the generic script programs through check boxes **106**, selecting individuals through check boxes **108**, and pressing the ASSIGN SCRIPT button **112**. When button **112** is pressed, data merge program **55** creates a custom script program for each individual selected in check boxes **108**.

Each custom script program is preferably created by using the selected generic script program as a template. For each individual selected, data merge program **55** retrieves from database **38** the data specified in the insert commands. Next, data merge program **55** inserts the data into the appropriate statements in the generic script program to create a custom script program for the individual. Each custom script program is stored in database **38**.

As each custom script program is generated for an individual, script assignor **52** assigns the script program to the individual. This is preferably accomplished by creating a pointer to the custom script program and storing the pointer with the individual's unique identification code in table **46**. When the individual's remote apparatus **26a-x** connects to server **18**, server **18** receives from apparatus **26a-x** the individual's unique identification code. Server **18** uses the unique identification code to retrieve from table **46** the pointer to the custom script program assigned to the individual. Next, server **18** retrieves the assigned script program from database **38** and transmits the script program to the

individual's remotely programmable apparatus **26a-x** through communication network **24**.

Remotely programmable apparatus **26a-x** receives and executes the script program. The
5 execution of the script program is similar to the execution described in the preferred
embodiment, except that statements are displayed to the individual rather than queries.
Figs. **17-18** illustrate two sample statements as they appear on display **64**. Each
statement includes a response choice, preferably an acknowledgment such as "OK".
After reading a statement, the individual presses the button corresponding to the response
10 choice to proceed to the next statement. Alternatively, the script program may specify a
period of time that each statement is to be displayed before proceeding to the next
statement. The remaining operation of the third embodiment is analogous to the
operation of the preferred embodiment described above.

15 Although it is presently preferred to generate a custom script program for each individual
as soon as script assignment information is received for the individual, it is also possible
to wait until the individual's apparatus connects to server **18** before generating the custom
script program. This is accomplished by creating and storing a pointer to the generic
script program assigned to the individual, as previously described in the preferred
20 embodiment. When the individual's remotely programmable apparatus **26a-x** connects to
server **18**, data merge program **55** creates a custom script program for the individual from
the generic script program assigned to the individual. The custom script program is then
sent to the individual's remotely programmable apparatus **26a-x** for execution.

25 Fig. **20A** is a block diagram of a networked monitoring system **16'**, according to a
currently preferred embodiment of the invention. System **16'** includes server **18**,
workstation **20** connected to server **18** through a communication network **24**, and at least
one remotely programmable apparatus
26a-x, essentially as described hereinabove with reference to Fig. 1. Each programmable
30 apparatus **26a-x** is in communication with server **18** through communication network **24**,
preferably the Internet. Alternatively, each patient's programmable apparatus, e.g., **26a**,
may be placed in communication with server **18** via wireless communication networks,

cellular networks, telephone networks, or any other network which allows each apparatus **26a-x** to exchange data with server **18**. It is to be understood that system **16'** may include any number of programmable apparatuses **26a-x** for monitoring any number of patients. For clarity, only two programmable apparatuses **26a-x** are shown in Fig. **20A**.

5 Workstation **20** may take the form of a health care provider or clinician's computer **426** (Fig. **20B**).

Each remotely programmable apparatus **26a-x** and its accompanying patient monitoring and drug delivery measurement apparatus **428/428'/428''a-x** is for monitoring a patient
10 and for recording a patient's activity. In particular, measurement apparatus **428/428'/428''** (Figs. **20B**, **25**, **31A**, respectively) is adapted to provide measurements of a physiological condition of the patient, to produce measurements of a patient's treatment, to record the measurements, and to transmit the measurements to the patient's programmable apparatus **26a-x**, e.g., through a standard connection cable **30**. Each
15 programmable apparatus **26a-x** is in communication with server **18** through communication network **24**, as described hereinabove, for transmitting measurement data from measurement apparatus, e.g., **428a-x**, to workstation **20**. Examples of suitable monitoring devices include blood glucose meters, respiratory flow meters, blood pressure cuffs, electronic weight scales, and pulse rate monitors. Examples of measurements of a
20 patient's treatment include measurements of drug dose administered or self-administered to the patient. According to a currently preferred embodiment, such measurements include dose(s) of a drug administered to the patient via a syringe.

Fig. **20B** is a high-level schematic diagram illustrating a dose administration or drug
25 delivery measurement apparatus **428** according to the invention. Apparatus **428** records data indicative of a dose of a drug or medication delivered to a patient from a syringe (e.g., syringe **580**, Fig. **21**). Apparatus **428** is capable of downloading the recorded data to a remotely programmable apparatus **26a-x** (Fig. **20A**).

According to one embodiment of the invention, remote apparatus **26a-x** may take the form of a patient's computer **424**, which in turn is capable of communicating with a clinician's computer **426** over a long-distance communication line such as a telephone line or the Internet,

5 as shown in Fig. **20B**. However, it is to be understood that apparatus **428** may be connected to other types of remote apparatus **26a-x**, and thence via a communications network to a remote interface, as described hereinabove with reference to Figs. **1-19** and elsewhere herein.

10 Apparatus **428** includes a dose measurement element, in the form of a capacitive element **422** enclosing at least part of a syringe (e.g., syringe **580**, Fig. **21**). According to other embodiments of the invention, a dose measurement element may take other, distinct forms. For example, a dose measurement element may be in the form of an inductive element (Figs. **25**, **29A**, **29B**). Capacitive element **422** includes one or more capacitors
15 arranged in a predetermined spatial relationship. A measuring device **432** is in electrical communication with capacitive element **422**, and detects a capacitive response of capacitive element **422** when the syringe is in a predetermined measurement position. Measuring device **432** preferably includes a LC circuit with a resonant frequency $\omega = 1/\sqrt{LC}$. Capacitance-measuring devices are well known in the art. The capacitive
20 response of capacitive element **422** is indicative of the quantity of liquid in the syringe, and consequently of the dose administered to the patient using the syringe. A control device **434** is in electrical communication with measuring device **432**, and temporally controls the operation of measuring device **432**. Control device **434** is capable of turning-on measuring device **432** when a syringe is in the measurement position, for
25 example before the administration of the dose to the patient. Control device **434** preferably includes a button, which the patient can press to trigger a measurement.

A computing device **436** is in electrical communication with measuring device **432** and with a calibration memory **438**. Computing device **436** preferably includes a

microprocessor. Computing device **436** is further in electrical communication with a recording device **440**. Recording device **440** preferably includes a memory chip. Computing device **436** generates dose data to be stored in recording device **440**. The dose data preferably includes a dose (e.g. an insulin dose) administered to the patient, but
5 may be in general any data which can be used to reconstruct (for example, within system **428**, at patient computer **24**, or at clinician computer **426**) the dose administered to the patient. In particular, computing device **436** calculates the quantity of liquid **592** within the syringe before injection of a dose, or the difference between the liquid quantities within the syringe before and after injection. Computing device **436** then sends
10 the result (the dose) to recording device **440** for storage.

According to the embodiment of Fig. **20B**, computing device **436** determines liquid quantities by comparing capacitive response data received from measuring device **432** with predetermined calibration data stored in calibration memory **438**. The calibration
15 data is indicative of the correspondence between capacitive responses and liquid quantities for the entire range of potential liquid quantities in the syringe. That is, calibration memory **438** stores the quantity of liquid **592** corresponding to a given capacitive response of capacitive element **422**, for all liquid quantities potentially present in the syringe.

20 A monitoring device **444** is electrically connected to recording device **440**. Monitoring device **444** tests a physical or physiological condition of the patient, and generates condition data representative of the physical or physiological condition. Preferably, the condition is diabetes, the monitoring device includes a blood glucose meter, and the
25 condition data includes a blood glucose level of the patient. Recording device **440** records the condition data generated by monitoring device **444**. A display **546** is electrically connected to recording device **440**, and displays dose data and condition data to the patient. Display **446** can be a liquid crystal display (LCD). A display such as display **446** may be directly connected to computing device **436** and monitoring device
30 **444**, rather than indirectly through recording device **440**. A digital clock **448** is

connected to recording device **440**. Upon prompting, clock **448** sends the current date and time to recording device **440** for recording in conjunction with dose and/or condition data.

5 Fig. **21** shows a perspective view of a measurement apparatus **528**, according to a preferred embodiment of the present invention. Apparatus **528** includes a housing **550** enclosing the various electronic components of apparatus **528**. Housing **550** preferably includes a metal layer for shielding internal components of apparatus **528** from external electric fields, and in particular the capacitive components of apparatus **528** (see below).
10 As is apparent to the skilled artisan, care should also be taken to minimize all stray capacitances. Housing **550** is sufficiently compact to allow apparatus **528** to be hand-held and carried by a user.

Display **446** is preferably recessed within housing **550**. A patient interface **558** (of
15 monitoring device **444**, Fig. **20B**) is also coupled to housing **550**. In a preferred embodiment, the patient places a finger on patient interface **558**, allowing monitoring device **444** to perform a blood glucose measurement for the patient. Blood glucose meters are well known in the art and will not be discussed here in detail. A dose measurement control **560** (of control means **434**, Fig. **20B**) is coupled to housing **550**,
20 and allows the patient to specify when dose measurements are to be performed by apparatus **528** (see below). A port **562** allows data transfer between recording device **440** and patient computer **424** (Fig. **20B**).

Housing **550** also encloses a holder **552** for receiving and snugly holding a syringe **580** in
25 the measurement position. A circular opening **553** within housing **550** provides access to holder **552**. Holder **552** has a well-like shape for laterally enclosing syringe **580**. Holder **552** defines an enclosed space **556** opposite opening **553**, for accommodating a needle **582** of syringe **580** when syringe **580** is in the measurement position. Syringe **580** can be a conventional syringe, such as a plastic syringe. Syringe **580** includes a
30 barrel **586** and a plunger **590**, defining a space for a liquid **592**. Liquid **592** preferably

includes insulin. Plunger **590** is capable of longitudinal motion relative to barrel **586**, for adjusting the volume available to liquid **592**. Holder **552** includes an alignment ledge **554** for aligning barrel **586** to holder **552** in the measurement position. A contact surface **584** of syringe **580** is in contact with alignment ledge **554** when syringe **580** is in the measurement position.

Fig. **22A** shows a longitudinal sectional view through syringe **580** and holder **552**, with syringe **580** in the measurement position. Fig. **22B** shows a transverse sectional view of the arrangement of Fig. **22A**. A capacitive element **600** consists of a single capacitor defined between an electrode **600a** and liquid **592**. Electrode **600a** is a cylindrical copper sheet embedded in a plastic side wall of holder **552**, and is electrically connected to measuring device **432** (Fig. **20B**). Electrode **600a** encloses syringe **580** externally and laterally. Liquid **592** is connected to measuring device **432** through needle **582** and a needle contact **583** coupled to holder **552**. Needle contact **583** is a corrosion-resistant metal block having a sloped (conical) side wall **585** for contacting needle **582** when syringe **580** is in the measurement position.

The dielectric constant within capacitive element **600** is relatively spatially invariant and does not change substantially with the quantity of liquid **592**. The dielectric constant within capacitive element **600** is determined by the materials and/or thicknesses of barrel **586**, the air between barrel **586** and the side wall of holder **552**, and the portion of the side wall of holder **552** between electrode **600a** and barrel **586**. Neglecting edge effects and effects stemming from the non-ideal conductivity of liquid **592**, the capacitance of capacitive element **600** is then primarily determined by its surface area, which is proportional to the longitudinal extent x of liquid enclosed by electrode **600a**.

To operate measurement apparatus **528**, a patient inserts the manufacturer-provided syringe **580** in holder **552** prior to administration of the dose. When syringe **580** is pressed against alignment ledge **554** and needle **582** contacts needle contact **583**, syringe **580** is in the measurement position. The patient presses dose measurement

control (e.g., button) **560** (Fig. **21**) to activate measuring device **432**. Measuring device **432** performs a measurement of the capacitance of capacitive element **600**. Computing device **436** then determines the quantity of liquid **592** within syringe **580**. Recording device **440** records the liquid quantity as the administered dose, in conjunction with the
5 current date and time obtained from clock **448**. Recording device **440** may also record condition data received from monitoring device **444**, and the associated date and time. Recording device **440** then contains the patient's blood glucose and insulin dose histories. The patient periodically (e.g. weekly) connects his or her measurement apparatus **528** to patient computer **424** and downloads the histories stored in recording device **440**. The
10 histories may then be periodically transmitted to clinician's computer **426**.

Fig. **23A** shows a longitudinal sectional view of an alternative capacitive element geometry of the present invention, while Fig. **23B** shows a transverse sectional view of the geometry of Fig. **23A**. A capacitive element **700** is coupled to holder **552**, and is
15 situated completely externally to syringe **580**. Capacitive element **700** includes a plurality of independent, longitudinally spaced, stacked capacitors **700a-e**. Each capacitor **700a-e** is independently connected to measuring device **432** (Fig. **20B**), and measuring device **432** determines the capacitive response of each capacitor **700a-e** independently. A capacitive response pattern of capacitive element **700** (the ensemble of
20 capacitive responses of capacitors **700a-e**) is indicative of the quantity of liquid **592** within syringe **580**. The use of plural stacked capacitors reduces the vulnerability of a system of the present invention to dosage determination errors caused by a constant capacitance offset.

25 Capacitor **700a** includes electrodes **700a'**, **700a''** embedded within the side wall of holder **552** on opposite sides of syringe **580**. Capacitors **700b-e** are similar to capacitor **700a** and are stacked above capacitor **700a**. The surface area of each capacitor **700a-e** is constant, and does not depend on the quantity of liquid **592**. The effective dielectric constant of each capacitor **700a-e** may depend, however, on the
30 quantity of liquid **592**. If liquid **592** is substantially conductive, it behaves like an

electrode inserted between electrodes **700a'** and **700a''**, thus creating two capacitors in series: one defined by electrode **700a'** and liquid **592**, the other defined by liquid **592** and electrode **700a''**. Preferably, the dielectric properties of barrel **586**, plunger **590** and liquid **592** are such that the capacitance response pattern of capacitive element **700** is
5 indicative of the position of plunger **590** relative to capacitive element **700** and/or of the quantity of liquid **592** within syringe **580**.

Fig. **24A** shows a perspective view of an alternative apparatus **820** of the present invention, suitable for measuring doses delivered by syringes using either capacitors or
10 inductors for dose measurement (Figs. **22A-23B** and **27A-28**, respectively). A circular placement field **870** is delineated on the outside of a housing **850** of apparatus **820**. Placement field **870** is bordered on four sides by a set of rigid positioning studs **872** forming a holder. Placement field **870** includes a circular input contact **874** positioned at the center of field **870**, and a ring-shaped output contact **876** positioned concentrically to
15 input contact **874**. Input contact **874** and output contact **876** are made of an electrically conductive material, preferably copper, and are connected to measuring device **432** (Fig. **20B**) or measuring device **432'** (Fig. **25**).

Fig. **24B** shows a longitudinal sectional view of a syringe **880** suitable for use with the
20 apparatus of Fig. **24A**. Syringe **880** includes a plunger **890** positioned within a barrel **886**. Plunger **890** includes a cylindrical cap **878** sized so as to fit on placement field **870** between studs **872** when syringe **880** is in a measurement position. Cap **878** includes an input terminal **812** and an output terminal **814** situated such that input terminal **812** and output terminal **814** are in electrical communication respectively with
25 input contact **874** and output contact **876** when syringe **880** is in the measurement position.

A metallic contact line **801** within plunger **890** establishes electrical communication between output terminal **814** and a cylindrical electrode **800a'** situated embedded within
30 the plastic body of plunger **890**, along the outside surface of plunger **890**. A second

cylindrical electrode **800a"** is encapsulated in the plastic body of barrel **886**, and is co-axial with electrode **800a'**. Electrode **800a"** is in electrical communication with input terminal **812** through metallic contact lines **802** and **804**. Line **802** is situated on the lateral (outside) surface of plunger **890**, while line **804** is situated within barrel **886**. A sliding electrical contact schematically illustrated as **803** is established between a fixed exposed point of line **804** and various points of line **802** as plunger **890** is moved within barrel **886**.

The following discussion is intended to illustrate a measurement apparatus of the invention, which utilizes a capacitive element, and should not be construed to limit the invention. Consider the geometry of Figs. **22A** and **22B**, for a typical syringe. Neglecting edge effects, the capacitance of capacitive element **600** is approximately

$$C \approx 2\pi\epsilon_{\text{bar}}x \ln\left(\frac{b}{a}\right) \quad [1]$$

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where **x** is the length of capacitor **600**, **a** and **b** are the radii of the cylinders defined respectively by liquid **592** and electrode **600a**, and ϵ_{bar} is the effective dielectric constant between liquid **592** and electrode **600a**. From eq. [1] it can be seen that dC/dx , the variation of the capacitance of capacitor **600** with displacement **x**, can be maximized for given radii **a** and **b** by increasing ϵ_{bar} . Thus, materials with high dielectric constants are preferred for the space between liquid **592** and electrode **600a**.

Fig. **25** is a high-level schematic diagram illustrating a dose administration or drug delivery measurement apparatus **428'** according to another embodiment of the instant invention. As for apparatus **428** described hereinabove with reference to Figure **20B**, apparatus **428** records data indicative of dose(s) delivered to a patient from a syringe (e.g., syringe **580'**). Apparatus **428'** is capable of downloading the recorded data to a remotely programmable apparatus (e.g., apparatus **26a-26x**, (Figs. 1, **20A**). According to the invention, a remotely programmable apparatus **26a-26x** may take the form of a

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patient computer **424** (Fig. **20B**), which in turn is capable of communicating with a clinician's computer **426** (Fig. **20B**) over a communication network or long-distance communication line, essentially as described hereinabove with reference to Figs. **1-20B**.

- 5 Apparatus **428'** includes an inductive element **423** enclosing at least part of the syringe. Inductive element **423** includes one or more inductors arranged in a predetermined spatial relationship. A measuring device **432'** is in electrical communication with inductive element **423**, and detects an inductive response of inductive element **423** when the syringe is in a predetermined measurement position. Measuring device **432'** preferably
- 10 includes a LC circuit with a resonant frequency $\omega = 1/\sqrt{LC}$. Inductance-measuring devices are well known in the art. The inductive response of inductive element **423** is indicative of the quantity of liquid in the syringe, and consequently of the dose administered to the patient using the syringe. Apparatus **428'** further includes a control device **434'** in electrical communication with a measuring device **432'**; a computing
- 15 device **436'** in electrical communication with measuring device **432'** and with a calibration memory **438'**; and a recording device **440'**, somewhat analogous to apparatus **428**, described hereinabove with reference to Fig. **20B**. Computing device **436'** is further in electrical communication with a recording device **440'**.
- 20 Computing device **436'** preferably includes a microprocessor. Recording device **440'** preferably includes a memory chip. Computing device **436'** generates dose data to be stored in recording device **440'**. The dose data preferably includes a dose (e.g. an insulin dose) administered to the patient, essentially as described hereinabove with reference to apparatus **428**. Computing device **436'** sends the result (the dose) to recording
- 25 device **440'** for storage.

Computing device **436'** determines liquid quantities by comparing inductive response data received from measuring device **432'** with predetermined calibration data stored in calibration memory **438'**. The calibration data is indicative of the correspondence

between inductive responses and liquid quantities for the entire range of potential liquid quantities in the syringe. That is, calibration memory 438' stores the liquid quantity corresponding to a given inductive response of inductive element 423, for all liquid quantities potentially present in the syringe.

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Apparatus 428' further includes a monitoring device 444' electrically connected to recording device 440', a display 446' also electrically connected to recording device 440', and a digital clock 448' connected to recording device 440', analogous to the corresponding components of apparatus 428 described hereinabove with reference to Fig. 20B. Upon prompting, clock 448' sends the current date and time to recording device 440' for recording in conjunction with dose or condition data related to the patient being monitored.

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Fig. 26 shows, in perspective view, an apparatus 528', according to one embodiment of the present invention. Apparatus 528' includes a housing 550' enclosing the various electronic components of apparatus 528'. Housing 550' preferably includes a metal layer for magnetically shielding internal components of apparatus 528', in particular inductive components of apparatus 528' (see below). Housing 550' is compact and has dimensions and weight characteristics similar to those described hereinabove with respect to housing 550 of Fig. 21.

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Housing 550' includes a (recessed) display 446' and a patient interface 558' (of monitoring device 444', Fig. 25) coupled to housing 550', similar to housing 550 of Fig. 21. In a preferred embodiment, the patient places a finger on patient interface 558', allowing monitoring device 444' to perform a blood glucose measurement for the patient. A dose measurement control 560' (of control device 434', Fig. 25) is coupled to housing 550', and allows the patient to specify when dose measurements are to be performed by apparatus 528' (see below). A port 562' allows data transfer between recording device 440' and a patient computer or remotely programmable apparatus (not shown).

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Housing 550' also encloses a holder 552' for receiving and holding a syringe 580' in the measurement position. Syringe 580' corresponds specifically to the calibration data stored in calibration memory 438'. A circular opening 553' within housing 550' provides
5 access to holder 552'. Holder 552' has a well-like shape for laterally enclosing syringe 580'. Holder 552' defines an enclosed space 556' opposite opening 553', for accommodating a needle 582' of syringe 580' when syringe 580' is in the measurement position. Enclosed space 556' is preferably closed off, so as to prevent accidental access to needle 582' while syringe 580' is in the measurement position.

10 Syringe 580' includes a barrel 586' and a plunger 590', defining a space for a liquid 592. Plunger 590' preferably includes a longitudinal strip 591' made of a ferromagnetic material such as ferrite, embedded in a plastic body 593'. Alternatively, a standard syringe with a plunger consisting of a plastic body can be used with a device of the
15 present invention. Plunger 590' is capable of longitudinal motion relative to barrel 586', for adjusting the volume available to liquid 592. Holding device 552' includes an alignment ledge 554' for aligning barrel 586' to holder 552' in the measurement position. A contact surface 584' of syringe 580' is in contact with alignment ledge 554' when syringe 580' is in the measurement position.

20 A cylindrical inductor 564 is mechanically coupled to holder 552', and encloses syringe 580' externally and laterally. Inductor 564 encloses syringe 580' along the entire longitudinal extent along which the position of plunger 590' and/or the quantity of liquid 592 may vary. The position of plunger 590' and/or the quantity of liquid 592
25 within syringe 580' determine the inductance of inductor 564. The magnetic permeabilities of plunger 590' and liquid 592 are substantially different, such that the inductance of inductor 564 is indicative of the position of plunger 590' relative to inductor 564 and of the quantity of liquid 592 within syringe 580'. In particular, the two permeabilities differ by at least a factor of two, preferably by a factor of ten or more.

The operation of apparatus 528' by a patient is similar to the operation of apparatus 528 as described hereinabove. Briefly, a patient inserts the manufacturer-provided syringe 580' in holder 552' prior to administration of the dose. When syringe 580' is pressed against alignment ledge 554', syringe 580' is in the measurement position. The patient presses dose measurement control (button) 560' to activate measuring device 432'. Measuring device 432' (Fig. 25) performs measurement of the inductance of inductor 564. Computing device 436' then determines the quantity of liquid 592 within syringe 580'. Recording device 440' records liquid quantity as the administered dose, in conjunction with current date and time from clock 448'. Recording device 440' may also record condition data received from monitoring means 444', and the associated date and time. The patient periodically connects apparatus 528' to a remotely programmable apparatus 26a-x or to a patient computer (not shown) and downloads the patient's blood glucose and insulin dose histories stored in recording device 440' for periodic transmission to, e.g., a clinician's computer (also not shown).

Fig. 27A shows a longitudinal sectional view of a syringe 980, according to one embodiment of the invention, while Fig. 27B shows a transverse sectional view of syringe 980. Syringe 980 is suitable for use with the apparatus of Fig. 24A, and includes a plunger 990 positioned within a barrel 986. Plunger 990 includes a cylindrical ferromagnetic core 991 encapsulated within a plastic shell 993. Plunger 990 also includes a cylindrical cap 978 sized so as to fit on placement field 470 (Fig. 24A) between studs 472 when syringe 980 is in a measurement position. Cap 978 includes an input terminal 912 and an output terminal 914 situated such that input terminal 912 and output terminal 914 are in electrical communication respectively with input contact 474 and output contact 476 when syringe 980 is in the measurement position. Barrel 986 includes an inductor 900 encapsulated within a plastic side wall. Metallic contact lines 903, 905 (located within plunger 990 and barrel 986) establish electrical communication between inductor 900 and input terminal 912 and output terminal 914, respectively. For taking a measurement, the patient places syringe 980 on placement field 470 and activates measuring device 432' to measure the inductance of inductor 900.

Fig. 28 shows a longitudinal sectional view of an alternative geometry for an inductance-enhanced syringe 1080 of the present invention. A plunger 1090 of syringe 1080 includes an inductance-enhancing element 1091 having a plurality of longitudinally spaced distinct segments 1095, embedded in a plastic shell 1093. Segments 1095 are thin ferromagnetic disks stacked along the longitudinal direction of plunger 1090. Segments 1095 have a magnetic permeability substantially higher than that of plastic shell 1093 or liquid 592.

Figs. 29A and 29B illustrate an alternative inductor geometry of the present invention. An inductive element 1100, coupled to and enclosing holder 552', is formed by a plurality of independent longitudinally-spaced, stacked inductors 1101a-c. Measuring device 432' is used to measure an inductive response pattern of inductors 1101a-c. The response pattern preferably consists of the inductance of each inductor 1101a-c. The longitudinal extent of each inductor 1101a-c is much greater than the desired resolution achievable with inductive element 1100. In the embodiment illustrated in Fig. 29B, the longitudinal extent of each inductor 1201a-p of an inductive element 1200 is of the same order of magnitude as the desired resolution to be achieved with inductive element 1200. The use of plural longitudinally stacked inductors 1201a-p reduces the vulnerability of a system of the present invention to dosage determination errors caused by a constant inductance offset.

Figs. 30A and 30B illustrate qualitatively the variation of inductance with plunger displacement for the inductive element geometries of Figs. 26 and 29A, respectively. In Figs. 30A and 30B, the plunger is taken to have a higher effective magnetic susceptibility than the liquid in the syringe. The inductance of inductor 564 increases with the extent of plunger 590' enclosed by inductor 564, as illustrated in Fig. 30A. The plunger displacement and delivered dose are computed from the measured inductance and stored calibration data. Likewise, the response pattern of inductive element 1100 changes as more of plunger 590' becomes enclosed by inductive element 1100. For a small dose to

be delivered (small plunger displacement), plunger **590'** is enclosed only by inductor **1101a** but not by inductors **1101b-c**. For a large dose to be delivered (large plunger displacement, or plunger pushed in close to the syringe needle), plunger **590'** is completely enclosed by inductors **1101a-b** and only partially enclosed by inductor **1101c**.

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The following discussion is intended to illustrate a measurement apparatus of the invention, which utilizes an inductive element, and should not be construed to limit the invention. Consider a geometry similar to those shown in Figs. **26** or **27A**, for a typical inductance-enhanced syringe. Consider a position of plunger **990** in which an inductor

10 encloses a length x of liquid and a length $D-x$ of plunger (see Fig. **27A**). From the inductance of an ideal long solenoid of length D , cross-sectional area A , and turn density (number of turns per unit length) n ,

$$L = \mu n^2 D A, \quad [2]$$

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one can obtain an order-of-magnitude estimate of the total inductance of the inductor as a function of x . Neglecting edge effects,

$$L_{\text{tot}} \approx L_{\text{liq}} + L_{\text{plg}} \approx n^2 A (\mu_{\text{liq}} x + \mu_{\text{plg}} (D - x)) = n^2 A (x(\mu_{\text{liq}} - \mu_{\text{plg}}) + \mu_{\text{plg}} D), \quad [3]$$

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where μ_{liq} and μ_{plg} are magnetic permeabilities, and L_{liq} and L_{plg} are inductances corresponding respectively to the liquid and the plunger. As illustrated by eq. [3], the sensitivity of L_{tot} to variations in x increases with the difference between the magnetic permeabilities of the plunger and the liquid.

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For a ferromagnetic-core plunger and corresponding solenoid, n is on the order of 10^5 m^{-1} , A is on the order of 10^{-5} m^2 , and μ_{liq} and μ_{plg} are, respectively, on the order of $10 \mu_0$ for water and $>10^3 \mu_0$ for a typical ferromagnetic or ferrimagnetic material. The above

values yield a sensitivity on the order of 10^2 mH per mm of plunger displacement. The inductor sensitivity may be lower for a ferrite-strip plunger or for a conventional plastic plunger. The inductor sensitivity may also be lower for other inductor geometries. The corresponding sensitivity of the inductance-measuring device may be adjusted according to the particular inductor geometry and plunger used; generally a more sensitive measuring device will be needed for measuring displacements of plungers having an effective permeability closer to that of the liquid.

Fig. 31A is a high-level schematic diagram illustrating a measurement apparatus 428'' according to another embodiment of the invention. Optical connections are indicated in Fig. 31A by dashed lines, while electrical connections are indicated by solid lines. Apparatus 428'' records data indicative of doses delivered to a patient using a syringe 580''. Apparatus 428'' is capable of downloading the recorded data to a remotely programmable apparatus 26a-x (Figs. 1, 20A), such as a patient computer 424 (Fig. 20B), which in turn is capable of communicating with workstation 20 (Figs. 1, 20A), or a clinician's computer 426 (Fig. 20B) over a communication network, telephone line, or the Internet.

Apparatus 428'' includes a light source 430 and an optical detector 450 for optical communication with syringe 580'' when the latter is in a measurement position. Light source 430 generates light incident on syringe 580''. Optical detector 450 detects an optical response of syringe 580'' to the light generated by light source 430. The optical response of syringe 580'' is indicative of the quantity of liquid in syringe 580'', and consequently of the dose administered to the patient using syringe 580''. A control means 434'', in electrical communication with light source 430 and optical detector 450, temporally controls the operation of light source 430 and optical detector 450. Control means 434'' turns on light source 430 and optical detector 450 when syringe 580'' is appropriately positioned for dose measurements, before and after the administration of the dose to the patient.

A computing means **436''** is in electrical communication with optical detector **450** and with a calibration memory **438''**. Computing means **436''** is further in electrical communication with a recording means **440''**. Computing means **436''** generates dose data to be stored in recording means **440''**. The dose data preferably includes a dose (e.g. an insulin dose) administered to the patient, but may be in general any data which can be used to reconstruct (for example within apparatus **428''**, at patient computer **424**, or at clinician computer **426**) the dose administered to the patient. In particular, computing means **436''** calculates quantities of liquid within syringe **580''** before and after injection of a dose. Computing means **436''** then calculates the difference between the two measured liquid quantities, and sends the result (the dose) to recording means **440''** for storage. Computing means **436''** determines liquid quantities by comparing optical response data received from optical detector **450** with predetermined calibration data stored in calibration memory **438''**. The calibration data is indicative of the correspondence between optical responses and liquid quantities for the entire range of potential liquid quantities in syringe **580''**. That is, calibration memory **438''** stores the liquid quantity corresponding to a given optical response of detector **450**, for all liquid quantities potentially present in syringe **580''**.

A monitoring or testing means **444''** is electrically connected to recording means **440''**. Monitoring means **444''** tests a physical or physiological condition of the patient, and generates condition data representative of the condition. The condition may be, for example, diabetes; the monitoring means may include a blood glucose meter; and the condition data may include a blood glucose level of the patient. Recording means **440''** records the condition data generated by monitoring means **444''**. A display **446''** is electrically connected to recording means **440''**, and displays dose data and condition data to the patient. Note that a display such as display **446''** may be directly connected to computing means **436''** and monitoring means **444''**, rather than indirectly through recording means **440''**.

Fig. 31B illustrates generally the principal detection step performed by measurement apparatus 428'' of the present invention. Light (electromagnetic radiation) is incident on syringe 580'' and interacts with syringe 580''. Light resulting from the interaction is then incident on detector 450 (Fig. 31A). The light incident on detector 450 may
5 generally be light transmitted, reflected, and/or emitted by syringe 580''. In general, two elements of syringe 580'' may vary with the quantity of liquid within syringe 580'' in a typical dose administration sequence: i) the position of the syringe plunger (relative to the syringe barrel), and ii) the quantity/position of the liquid within syringe 580''. Light
10 incident on syringe 580'' may interact with the plunger and/or liquid. The measured light interaction with the plunger is preferably substantially different from the interaction with the liquid, such that the interaction with syringe 580'' as a whole depends on at least one of the position of the plunger and the quantity of liquid.

Fig. 32A shows a perspective view of an apparatus 528'', according to a preferred
15 embodiment of the present invention. Apparatus 528'' includes a housing 550'' enclosing the various electronic and optical components of apparatus 528''.

Display 446'' is recessed within housing 550''. A patient interface 558'' (of monitoring means 444'', Fig. 31A) is also coupled to housing 550''. In a preferred embodiment, the patient places his or her finger on patient interface 558'', allowing monitoring
20 means 444'' to perform a blood glucose measurement for the patient. A dose measurement control 560'' of control means 434'' is coupled to housing 550'', and allows the patient to specify when dose measurements are to be performed by apparatus 528'' (see below).

25 Housing 550'' also encloses a holding means 552'' for receiving and holding a syringe 580'' in a measurement position. Syringe 580'' can be a conventional plastic syringe. Syringe 580'' includes a barrel 586'' and a plunger 590'', defining a space for a liquid 592. Plunger 590'' is capable of longitudinal motion relative to barrel 586'', for adjusting the volume available to liquid 592. Barrel 586'' has side walls transparent at a

wavelength of light emitted by light source **430** (Fig. **31A**), as well as a control portion **588''** opaque at a wavelength of light emitted by a control emitter (see below).

Holding means **552''** includes an alignment ledge **554''** for aligning barrel **586''** to holding means **552''** in a predetermined measurement position. A contact surface **584''** of syringe **580''** is in contact with alignment ledge **554''** when syringe **580''** is in the measurement position (see below). A space **556''** accommodates a needle **582''** of syringe **580''**, when the latter is in the measurement position.

Fig. **32B** shows a longitudinal sectional view through syringe **580''** and holding means **552''**, with syringe **580''** in a measurement position. A light source **1300** and an optical detector **1302** are mechanically coupled to holding means **552''**, and in optical communication with syringe **580''**. Optical detector **1302** is opposite light source **1300** relative to syringe **580''**, such that optical detector **1302** detects light transmitted through syringe **580''**. Light source **1300** generates light incident on both plunger **590''** and liquid **592**. A control light source **1304** and a control optical detector **1306** of control means **434''** (Fig. **31A**) are mechanically coupled to holding means **552''**, and are in optical communication with control portion **588''** (Fig. **32A**) when syringe **580''** is in the measurement position.

Fig. **32C** shows a detail of Fig. **32B**. Following a patient command entered by the patient pressing dose measurement control **560''** (Fig. **32A**), control light source **1304** emits a light beam **1309** which is blocked by control portion **588''** when syringe **580''** is in the measurement position. If light beam **1309** is blocked, control means **434''** operates light source **1300** and detector **1302** to take a first liquid quantity measurement, before the injection of liquid **592** by the patient. Light beam **1309** is then incident on control detector **1306** while syringe **580''** is out of holding means **552''**. When the patient inserts syringe **580''** into holding means **552''** after the injection of a dose of liquid **592**, light beam **1309** is again blocked, and control means **434''** operates light source **1300** and detector **1302** to take a second liquid quantity measurement. The difference between the

two liquid quantities is taken to be the dose injected by the patient, and is stored by recording means **440''**.

Light source **1300** includes a plurality of light emitters **1300a-f**, while detector **1302**
5 includes a plurality of detecting elements **1302a-f**. Light emitters **1300a-f** and detecting elements **1302a-f** are longitudinally spaced apart at regular intervals. Each light emitter **1300a-f** is longitudinally aligned to a corresponding detecting element **1302a-f**. Light emitters **1300a-f** are preferably narrow-angle light emitting diodes (LEDs), while detecting elements **1302a-f** are preferably photodiodes capable of detecting light of a
10 wavelength emitted by light emitters **1300a-f**.

For detecting the quantity of liquid **592** within syringe **580''**, light emitters **1300a-f** emit light beams **1308a-f** incident on plunger **590''** and liquid **592**. Detector elements **1302a-f** detect the resulting optical response pattern of syringe **580''**. Emitter **1300d**, situated
15 under the current position of plunger **590''**, emits a light beam **1308d** which passes through liquid **592** and is incident on detector **1302d**. Emitter **1300e**, situated above the current position of plunger **590''**, emits a light beam **1308e** which is incident on plunger **590''**. Plunger **590''** has a substantially different optical transmission property from liquid **592** at the wavelength(s) measured by detecting element **1302e**. Preferably,
20 plunger **590''** is opaque at those wavelengths. Plunger **590''** then substantially blocks beam **1308e**, such that beam **1308e** is not incident on detecting element **1302e**. An electrical signal indicative of the optical pattern detected by detector **1302** is sent to computing means **436''**.

25 Fig. **32D** illustrates an alternative geometry for a detector of the present invention. A detector **1352** includes detecting elements **202a-c**, each of which receives light emitted by plural emitters of light source **1300**. Fig. **32E** illustrates yet another geometry for a light source and detector of the present invention. A light source **1300'** and a detector **1352'** each comprise a single emitting or detecting element, extending
30 longitudinally over the range of potential plunger bottom positions. The total amount of

light detected by detector **1352'** is indicative of the plunger position – relatively little light is incident on detector **1352'** if the plunger occludes the light path between light source **1300'** and detector **1352'**. The single-element detecting scheme illustrated in Fig. **32E** can be less sensitive than a multiple-element detecting scheme using similar components, but is advantageous because of its simple design.

Fig. **33A** shows a perspective view of another embodiment of the present invention. An apparatus **1420** includes a holding means **1452** which encloses syringe **580''** only on one side when syringe **580''** is in a measurement position. Fig. **33B** shows a longitudinal side view of the holding means **1452** and syringe **580''** in the measurement position. A control ledge **1454** aligns barrel **586''** of syringe **580''** with a detector **1402** in the measurement position. Detector **1402** includes plural longitudinally spaced detecting elements **1402a-x**. To take measurements, the patient orients the measurement face of holding means **1452** toward an external source of spatially uniform light, preferably a parallel light beam. For example, the patient places apparatus **1452** close to a bright window or lamp. For the embodiment in Fig. **33A**, the computing means calculates quantities of liquid within syringe **580''** according to the distribution of signals received from the detecting elements of detector **1402**, rather than the absolute values of the signals.

Fig. **34** shows a perspective view of another embodiment of the present invention. An apparatus **1528** includes a holding means **1552** for holding the barrel of a syringe **1580** in a predetermined position relative to a measurement window **1503**. Syringe **1580** includes a plunger **1590** having a longitudinally varying marking **1591**. Marking **1591** is desirably a color marking, but generally may be a shape marking. A light source and detector (both not shown) are situated behind measurement window **1503**, for reading the part of marking **1591** in alignment with window **1503**. Light emitted by the light source is reflected by marking **1591** back into the detector. The reflected light (its intensity and/or spatial distribution) is indicative of the position of marking **1591** relative to window **1503**, which is in turn indicative of the quantity of liquid within syringe **1580**.

The quantity of liquid within syringe **1580** is in turn indicative of a dose delivered from syringe **1580**.

SUMMARY, RAMIFICATIONS, AND SCOPE

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Although the above description contains many specificities, these should not be construed as limitations on the scope of the invention but merely as illustrations of some of the presently preferred embodiments. Many other embodiments of the invention are possible. For example, the scripting language and script commands shown are
10 representative of the preferred embodiment. It will be apparent to one skilled in the art that many other scripting languages and specific script commands may be used to implement the invention.

Moreover, the invention is not limited to the specific applications described. The system
15 and method of the invention have many other applications both inside and outside the healthcare industry. For example, pharmaceutical manufacturers may apply the system in the clinical development and post marketing surveillance of new drugs, using the system as an interactive, on-line monitoring tool for collecting data on the efficacy, side effects, and quality of life impact of the drugs. Compared to the current use of labor intensive
20 patient interviews, the system provides a fast, flexible, and cost effective alternative for monitoring the use and effects of the drugs.

The system may also be used by home healthcare companies to enhance the service levels provided to customers, e.g. panic systems, sleep surveillance, specific monitoring of
25 disease conditions, etc. Alternatively, the system may be used to monitor and optimize the inventory of home stationed health supplies. As an example, the system may be connected to an appropriate measuring device to optimize timing of oxygen tank delivery to patients with chronic obstructive pulmonary disease (COPD).

30 It will be clear to one skilled in the art that the above embodiments may be altered in many ways without departing from the scope of the invention. Generally, the dose data may include, for example, quantities of liquid in the syringe before and/or after the

administration of the dose, or dose measurement (capacitive, inductive, or optical) response values before and/or after the administration of the dose. The patient's and/or the clinician's computers then determine the dose administered to the patient from the dose data stored in the recording device. In such an embodiment, calibration data may be
5 stored on the patient's or clinician's computer, and the measurement apparatus may lack a computing device. The patient computer need not be a conventional personal computer, but can be in general any data storage device or device allowing communication between the patient's measurement apparatus and the clinician's data storage device or server. A measurement apparatus of the present invention may connect directly to a clinician's
10 server, rather than indirectly through a patient computer. Various computation and storage devices used in the present invention may generally be implemented through software or dedicated hardware, or combinations thereof. For a multiple-delivery injection device such as an injection pen, liquid quantities before and after each injection are measured and the administered dose is taken to be the difference between the two
15 quantities. The dose measurement aspects of the present invention are not limited to diabetes care, and may be used for monitoring patient compliance with any injection-based treatment program.

Various capacitor geometries and placements may be suitable in a device of the present
20 invention. In particular, the capacitor need not laterally enclose the syringe completely or even partially, as long as the capacitive element is capacitively coupled to the syringe. The method does not require the presence of a plunger to determine capacitance. A method of the present invention may be used to capacitively measure liquid levels in plungerless syringes operated using air pressure, for example.

25 Similarly, various inductive element geometries and placements may be suitable in a device of the present invention. In particular, the inductive element need not laterally enclose the syringe completely or even partially, as long as the inductive element is inductively coupled to the syringe. The method does not require the presence of a plunger
30 to determine inductance; a method of the present invention may be used to inductively

measure liquid levels in plungerless injection devices operated using air pressure, for example.

With regard to optical based dose measurement embodiments of the invention, detecting
5 spatial distributions is useful for increasing sensitivity. The detector need not detect a
spatial distribution of light, however. The detector may detect a spatial sum of light
intensity over a whole area, as long as that spatial sum is indicative of the dose
administered with the syringe. For example, the detector may detect the total amount of
light passing through the syringe, or the total amount of light emitted by the syringe
10 following absorption of incident light (e.g. the total amount of heat emitted following
exposure to microwave radiation). Moreover, light emitting and detecting elements need
not be longitudinally spaced or aligned, and light beams need not be transverse to the
longitudinal axis of the syringe. Various light source and detector geometries and
placements may be suitable in a device of the present invention.

15 An optical method of dose measurement does not require the presence of a plunger to
transmit, reflect or absorb light. A method of the present invention may be used to
optically measure liquid levels in plungerless syringes operated using air pressure, for
example.

20 The optical dose measurement methods and devices described above may be extended to
non-optical wave energy forms such as sound (non-electromagnetic) waves. The
considerations discussed above for choosing frequency and detector parameters for
optical detectors largely apply to an apparatus using sound wave detection. For example,
25 suitable sound frequencies may include frequencies for which sound absorption by water
is significantly (e.g. at least by a factor of two) different from absorption by the syringe
plunger. Sound frequencies above the hearing range may be desirable so as to avoid
disturbing the user.

Therefore, the scope of the invention should be determined not by the examples given, but by the appended claims and their legal equivalents.

CLAIMS**What is claimed is:**

- 5 1. A system for remotely monitoring a dose of a drug administered to a patient, comprising:
 - a) a server;
 - b) a remote interface means connected to the server;
 - 10 c) a measurement apparatus for providing measurement data related to the patient; and
 - d) a remotely programmable apparatus, in communication with said measurement apparatus, for receiving measurement data from said measurement apparatus, said remotely programmable apparatus in communication with said server via a communication network; wherein said
15 measurement apparatus provides drug dose measurement data indicative of the dose.
- 20 2. The system of claim 1, wherein said measurement apparatus includes a recording device for recording the drug dose measurement data, said recording device in communication with said remotely programmable apparatus.
- 25 3. The system of claim 2, wherein said measurement apparatus further includes: a dose measurement element, and a measuring device in communication with said dose measurement element, said measurement apparatus for measuring a response of said dose measurement element, and wherein said measuring device is in communication with said recording device.
- 30 4. The system of claim 3, wherein said dose measurement element comprises a capacitive element or an inductive element.

5. The system of claim 2, wherein said measurement apparatus further includes a monitoring device for monitoring a physiological condition of the patient and for generating a condition datum representative of the physiological condition of the patient, said monitoring device in communication with said recording device such that said recording device records said condition datum.
6. The system of claim 5, wherein said monitoring device comprises a blood glucose meter and said condition datum comprises a blood glucose level of the patient.
7. The system of claim 2, wherein said recording device comprises a digital memory unit.
8. The system of claim 3, wherein said measurement apparatus further includes:
a display connected to said measuring device, said display for displaying the dose;
and
a computing device in communication with said recording device, said computing device for computing said drug dose measurement data from the response of said dose measurement element.
9. The system of claim 8, wherein said measurement apparatus further includes a calibration memory in communication with said computing device, said calibration memory for providing said computing device with calibration data indicative of a correspondence between the response of said dose measurement element and said drug dose measurement data.
10. The system of claim 3, wherein said measurement apparatus further includes a holder for receiving and holding a syringe in a measurement position.
11. The system of claim 10, further comprising a housing enclosing said measuring device and said recording device, wherein said holder is mechanically coupled to said housing.

12. The system of claim 11, wherein said housing further encloses said holder and said dose measurement element, said housing shielding said dose measurement element and the syringe from external electric fields.

5 13. The system of claim 10, wherein said holder comprises a well, said well laterally enclosing the syringe in the measurement position, and said dose measurement element is coupled to said well so as to laterally enclose the syringe in the measurement position.

10 14. The system of claim 10, wherein said dose measurement element comprises a capacitive element, said capacitive element being defined between a liquid held by the syringe and an electrode located external to the syringe, wherein said measurement apparatus further comprises a needle contact coupled to said holder, said needle contact for establishing electrical communication between said measuring device and a needle of the syringe when the syringe is in the measurement position, and said needle is in electrical contact
15 with the liquid.

15. The system of claim 10, wherein said dose measurement element comprises a capacitive element, said capacitive element including:

- 20 a) a first electrically conducting longitudinal plate coupled to said holder;
and
b) a second electrically conducting longitudinal plate coupled to said holder opposite said first longitudinal plate, and said second plate electrically insulated from said first plate.

25 16. The system of claim 10, wherein said inductive element is coupled to said holder such that an inductive response of said inductive element is indicative of the dose when the syringe is in the measurement position.

17. The system of claim 1, wherein the measurement apparatus further includes:

- 30 a) a syringe having a barrel and an inductance-enhancing element; and

- b) a holder for receiving and holding said syringe in a measurement position, wherein a position of said inductance-enhancing element relative to said barrel of said syringe is indicative of the dose, and wherein said inductive response is indicative of said position of said inductance-enhancing element.

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18. The system of claim 17, wherein said syringe includes a plunger, and said inductance-enhancing element comprises a ferromagnetic material, a longitudinal plunger element, a ferromagnetic plunger core, or a plurality of distinct sections arranged longitudinally within said plunger.

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19. The system of claim 1, wherein the measurement apparatus further includes:
- a) a holding means for receiving and holding a syringe in a measurement position;
- b) a light source coupled to said holding means and in optical communication with the syringe, for generating light incident on the syringe when said syringe is in the measurement position, wherein an optical response of the syringe to said light is indicative of said dose; and
- c) an optical detector coupled to said holding means and in optical communication with the syringe, for detecting the optical response; wherein said optical detector is in electrical communication with said recording device, said recording device for recording a dose datum indicative of said optical response, wherein said dose datum is indicative of the dose.

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20. The system of claim 1, wherein said server includes a script generating means for generating a script program executable by said remotely programmable apparatus to communicate a message to the patient.

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21. The system of claim 20, wherein the remotely programmable apparatus comprises:
- i) a communication means for transmitting the measurement data to said server;

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- ii) a memory means for storing the script program;
- iii) a user interface means for communicating the message to the patient; and
- iv) a processor means connected to said communication means, said user interface means, and said memory means for executing the script program.

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22. The system of claim 20, wherein said remotely programmable apparatus includes:

- i) communication means for receiving the script program from said server and for transmitting to said server responses to the queries;
- ii) user interface means for communicating queries to the patient and for receiving responses to the queries;
- iii) memory means for storing the script program and responses to the queries;
- iv) processor means connected to said communication means, said user interface means, and said memory means for executing the script program to communicate the queries to the patient, to receive the responses to the queries, and to transmit the responses to said server; and
- v) device interface means connected to said processor means for receiving the measurement data from said measurement apparatus; wherein said memory means includes means for storing the measurement data, and said communication means includes means for transmitting the measurement data to said server.

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23. A system for remotely monitoring a dose of a drug administered to a patient, comprising:

- a) a server;
- b) a remote interface means connected to the server;
- c) a measurement apparatus for providing measurement data related to the patient; and
- d) a remotely programmable apparatus for receiving measurement data from the measurement apparatus, the remotely programmable apparatus being

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networked to the server via a communication network; wherein the measurement apparatus includes:

- i) a syringe having a barrel, a plunger, and a response-enhancing element;
- ii) a holding means for receiving and holding said syringe in a measurement position;
- iii) a light source coupled to said holding means and in optical communication with said syringe, for generating light incident on said syringe, wherein an optical response of said syringe to said light is indicative of said dose; and
- iv) an optical detector coupled to said holding means and in optical communication with said syringe, for detecting the optical response;
- v) a recording device in electrical communication with said optical detector; and
- vi) an alignment means for aligning said barrel of said syringe to said optical detector, said recording device for recording a dose datum indicative of said optical response, wherein said dose datum is indicative of the dose.

24. The system of claim 23, wherein a position of a marking of said response-enhancing element is indicative of said dose; and said optical response depends on an interaction of the light with said marking in said position.

25. The system of claim 23, wherein said response-enhancing element comprises a longitudinal element mechanically coupled to said plunger, and said longitudinal element is longitudinally marked.

26. The system of claim 24, wherein said marking comprises a longitudinally-variable color marking which varies longitudinally in brightness or in hue.

27. The system of claim 23, wherein said optical detector is situated opposite said light source relative to said syringe, or adjacent said light source relative to said syringe.

28. A system for monitoring a patient, comprising:

- a) a server;
- b) a remote interface means connected to the server;

5 c) a remotely programmable apparatus for receiving measurement data from the measurement apparatus, the remotely programmable apparatus being networked to the server via a communication network; and

- d) an optical dose measurement apparatus, in communication with said server, for providing a dose datum of a drug delivered to the patient from a syringe;

10 wherein the optical dose measurement apparatus includes:

- i) a holding means for receiving and holding the syringe;
- ii) at least one optical detecting element coupled to said holding means and in optical communication with the syringe, for detecting an optical response pattern of the syringe, wherein said optical response pattern is indicative of the dose; and

15 iii) a recording means in electrical communication with said at least one optical detecting element, for recording a dose datum indicative of said optical response pattern, wherein said dose datum is indicative of the dose.

20 29. A method for remotely monitoring a patient, comprising the steps of:

- a) providing the patient with a remotely programmable apparatus and a measurement apparatus in communication with the remotely programmable apparatus, the measurement apparatus having:

- 25 i) a dose measurement element,
- ii) a measuring device in communication with the dose measurement element for measuring a response of the dose measurement element; and

- iii) a recording device in communication with the measuring device, wherein the measurement apparatus provides measurement data related to the patient;
- b) collecting the measurement data in the remotely programmable apparatus;
- 5 c) transmitting the measurement data from the remotely programmable apparatus to a server; and
- d) receiving and storing the measurement data in the server.

30. The method of claim 29, wherein the remotely programmable apparatus includes:

- 10 i) a communication means for exchanging data between the remotely programmable apparatus and the server through a communication network;
- ii) a memory means for storing the data exchangeable between the remotely programmable apparatus and the server; and
- 15 iii) a processor means connected to the communication means, and the memory means.

31. The method of claim 29, wherein the measurement data related to the patient comprises dose measurement data indicative of a dose of a drug delivered to the patient.

32. The method of claim 29, wherein the dose measurement element comprises a capacitive element or an inductive element.

33. The method of claim 33, wherein the measurement apparatus further includes a recording device and a monitoring device, wherein the monitoring device provides physiological condition measurements to the recording device, the physiological condition measurements indicative of a physiological condition of the patient; wherein the remotely programmable apparatus further includes a device interface connected to the processor means for receiving the physiological condition

measurements; and wherein said step b) comprises collecting the physiological condition measurements in the remotely programmable apparatus.

34. The method of claim 33, wherein the physiological condition comprises diabetes,
5 and the physiological condition measurements comprise a blood glucose level of the patient.

35. The method of claim 30, wherein the data exchangeable between the remotely
programmable apparatus and the server includes a script program, executable by
10 the remotely programmable apparatus, to communicate queries to the patient, to receive responses to the queries, and to transmit the responses to the server; and wherein the remotely programmable apparatus further includes a user interface means for communicating the queries to the patient and for receiving the responses to the queries.

36. The method of claim 35, wherein the server comprises a web server having a web
page for entry of the queries, and wherein the queries are entered by accessing the
web page through the Internet and entering the queries in the web page.

37. A method for communicating information to a patient, the method comprising the
steps of:

a) providing the patient with a measurement apparatus and a remotely
programmable apparatus in communication with the measurement apparatus,
the remotely programmable apparatus having:

i) a communication means for exchanging data with a server through a
communication network, wherein the exchangeable data includes a
script program executable by the remotely programmable apparatus to
communicate a message to the patient;

ii) a memory means for storing the script program;

iii) a user interface for communicating the message; and

- i) a processor means connected to the communication means, the memory means, and the user interface for executing the script program;

and the measurement apparatus having:

- vi) a measuring device;
- vii) and a recording device in communication with the measuring device and the remotely programmable apparatus;

- b) generating measurement data from the measurement apparatus related to the patient;

- c) transmitting the measurement data from the recording device to the remotely programmable apparatus via a standard cable; and

- d) transmitting the measurement data from the remotely programmable apparatus to the server through the communication network.

38. The method of claim 37, wherein the measurement apparatus further includes a dose measurement element, the measuring element for measuring a response of the dose measurement element.

39. The method of claim 38, wherein the measurement apparatus further includes a monitoring device for monitoring a physiological condition of the patient, and wherein the measurement data transmitted in said steps c) and d) includes physiological condition data and dose measurement data.

40. The method of claim 39, wherein the physiological condition data comprises a blood glucose level of a patient, and the dose measurement data comprises a dose of insulin administered to the patient.

41. The method of claim 39, wherein the dose measurement data comprises a dose of a drug administered to the patient from a syringe.

42. The method of claim 41, wherein the syringe includes a plunger, a barrel, and an inductance-enhancing element, wherein a position of the inductance-enhancing element relative to the barrel is indicative of the dose, and the inductance-enhancing element comprises a ferromagnetic material, a longitudinal plunger element, a
5 ferromagnetic plunger core, or a plurality of distinct sections arranged longitudinally within the plunger.

43. The method of claim 41, wherein the measurement apparatus further includes:

- 10 i) a holder for receiving and holding the syringe in a measurement position; and
- ii) a capacitive element coupled to the holder such that a capacitive response of the capacitive element is indicative of the dose when the syringe is in the measurement position; wherein the measuring device is in communication with the capacitive element for measuring the capacitive response; and
15 wherein the recording device is in communication with the measuring device for recording a dose datum indicative of the capacitive response, wherein the dose datum is indicative of the dose.

44. The method of claim 37, wherein the measurement apparatus further includes:

- 20 i) a holder for receiving and holding a syringe in a measurement position,
- ii) a light source in optical communication with the syringe when the syringe is in the measurement position; and
- iii) an optical detector in optical communication with the syringe when the syringe is in the measurement position, the optical detector for detecting an
25 optical response; and the syringe includes a response-enhancing element having a marking, wherein a position of the marking of the response-enhancing element is indicative of the dose.

45. The method of claim 37, further comprising the steps of:

- 30 e) entering in the server the message to be communicated to the patient;

- f) generating the script program in the server;
- g) transmitting the script program from the server to the remotely programmable apparatus through the communication network; and
- h) executing the script program in the apparatus to communicate the message to the patient.

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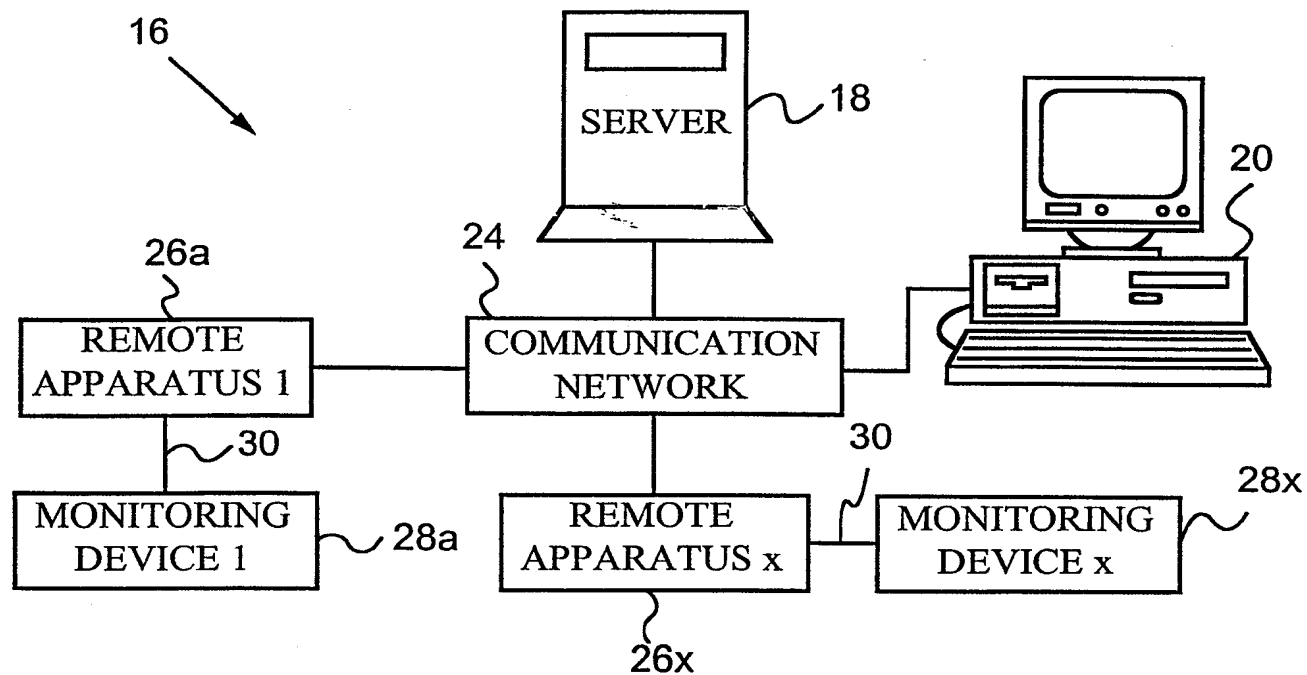


FIG. 1

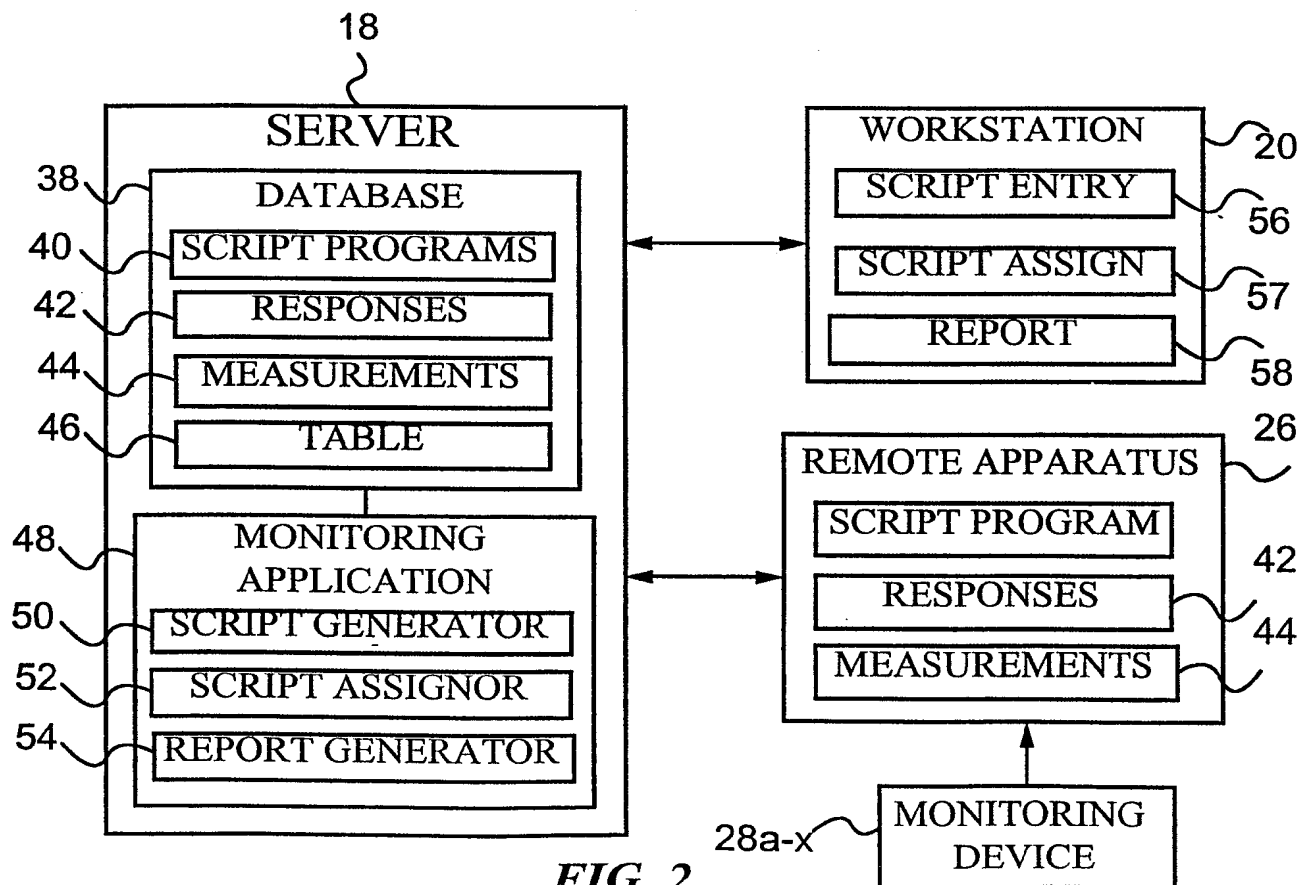


FIG. 2

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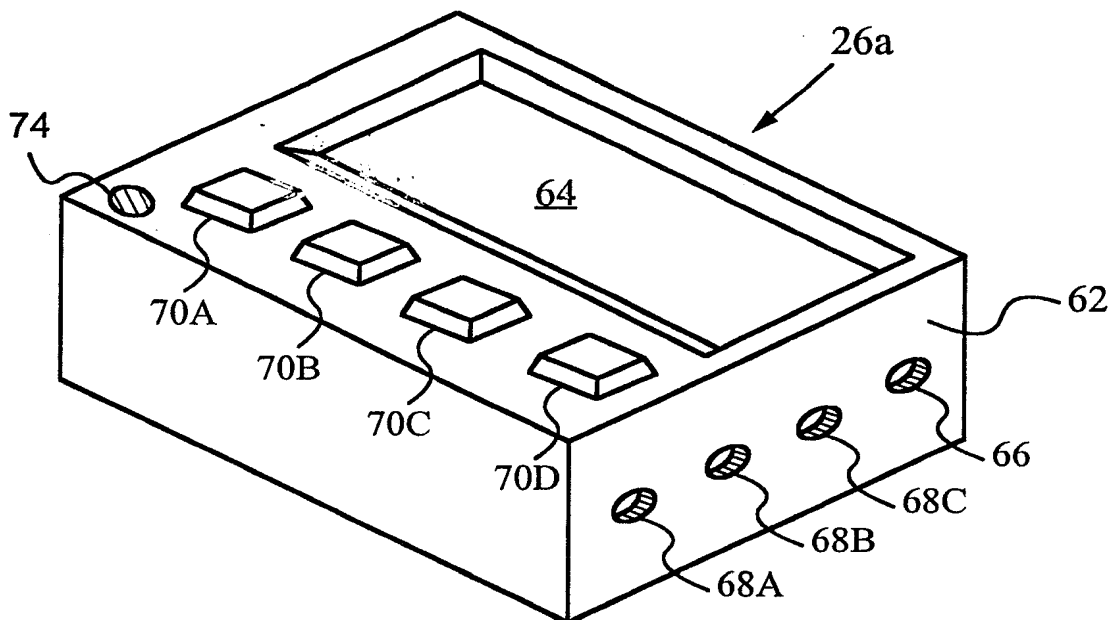


FIG. 3

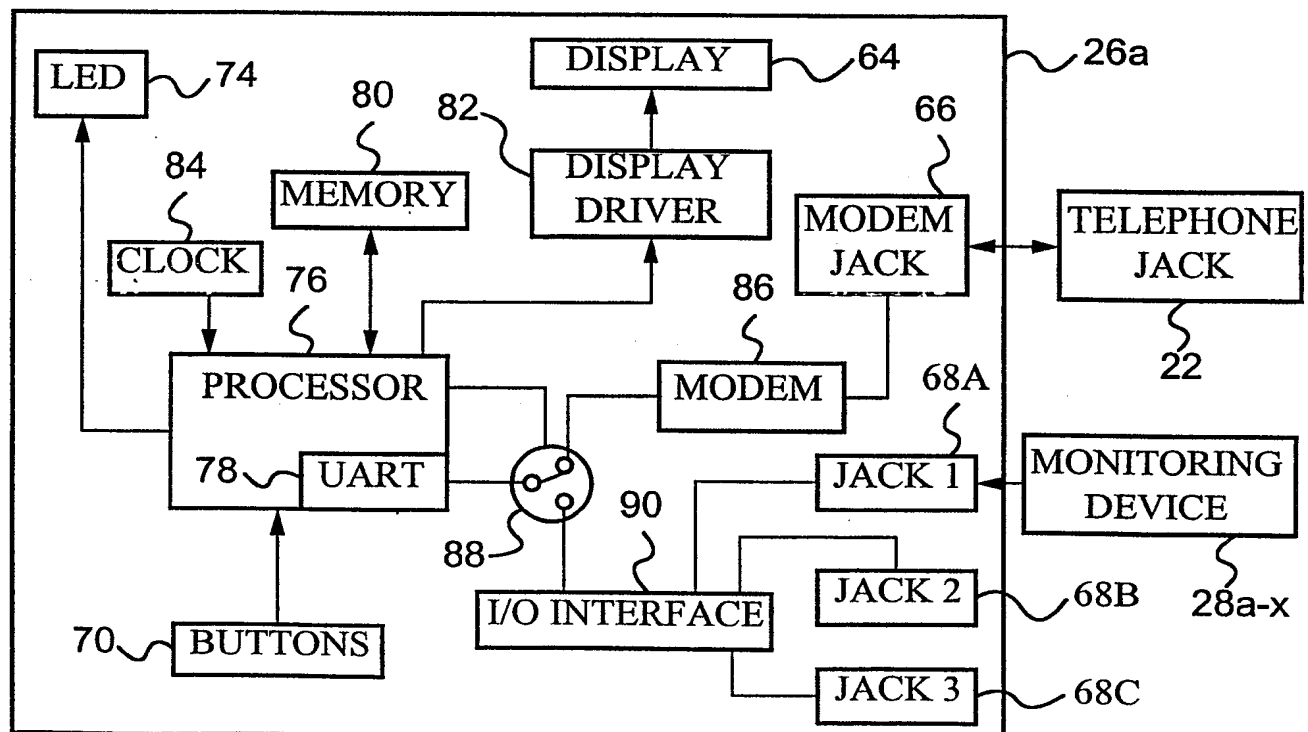


FIG. 4

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SCRIPT ENTRY SCREEN

SCRIPT NAME: DIABETES SCRIPT 1 92

QUERIES	CHOICE 1	CHOICE 2	CHOICE 3	CHOICE 4
HOW DO YOU FEEL?	VERY BAD	BAD	GOOD	VERY GOOD
HOW WELL ARE YOU MANAGING YOUR DISEASE?	VERY BADLY	BADLY	WELL	VERY WELL
HOW HARD IS IT FOR YOU TO FOLLOW YOUR TREATMENT PLAN?	VERY HARD	HARD	EASY	VERY EASY
HOW HARD IS IT FOR YOU TO CONTROL YOUR BLOOD SUGAR?	VERY HARD	HARD	EASY	VERY EASY

SELECT DEVICE TYPE(S)

98 ☒ GLUCOSE METER

INJECTION TIME: 03:00 ▽ 100

☐ RESPIRATORY FLOW METER

CREATE SCRIPT 102

☐ BP CUFF

CANCEL 104

FIG. 5

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NUMBER: 9001 {LF}

LED: 1 {LF}

ZAP: {LF}

CLS: {LF}

DISPLAY: ANSWER QUERIES NOW?

PRESS ANY BUTTON TO START {LF}

WAIT: {LF}

CLS: {LF}

DISPLAY: HOW DO YOU FEEL?

VERY

VERY

BAD BAD GOOD GOOD {LF}

INPUT: OOOO {LF}

CLS: {LF}

DISPLAY: HOW WELL ARE YOU

MANAGING YOUR DISEASE?

VERY

VERY

WELL BADLY WELL WELL {LF}

INPUT: OOOO {LF}

CLS: {LF}

DISPLAY: HOW HARD IS IT FOR YOU TO

FOLLOW YOUR TREATMENT PLAN?

VERY

VERY

HARD HARD EASY EASY {LF}

INPUT: OOOO {LF}

CLS: {LF}

DISPLAY: HOW HARD IS IT FOR YOU TO

CONTROL YOUR BLOOD SUGAR?

VERY

VERY

HARD HARD EASY EASY {LF}

FIG. 6A

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INPUT: OOOO {LF}
CLS: {LF}
DISPLAY: CONNECT GLUCOSE METER
AND PRESS ANY BUTTON
WHEN FINISHED {LF}
WAIT: {LF}
CLS: {LF}
DISPLAY: COLLECTING MEASUREMENTS {LF}
COLLECT: GLUCOSE_METER {LF}
CLS: {LF}
DISPLAY: CONNECT APPARATUS TO
TELEPHONE JACK AND
PRESS ANY BUTTON
WHEN FINISHED {LF}
WAIT: {LF}
LED: 0 {LF}
CLS: {LF}
DELAY: 03:00 {LF}
DISPLAY: CONNECTING TO SERVER {LF}
CONNECT: {LF}
{EOF}

FIG. 6B

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SCRIPT ASSIGNMENT SCREEN

AVAILABLE SCRIPTS:		PATIENTS:	
<input checked="" type="checkbox"/> 106	<u>DIABETES SCRIPT 1</u> 108	<input checked="" type="checkbox"/> 108	<u>DAN LINDSEY</u>
<input type="checkbox"/>	<u>DIABETES SCRIPT 2</u>	<input type="checkbox"/>	<u>MARK SMITH</u>
<input type="checkbox"/> 110	<u>ASTHMA SCRIPT 1</u> 112	<input type="checkbox"/>	<u>DEAN JONES</u>
<input type="button" value="ADD SCRIPT"/> 110		<input type="button" value="ASSIGN SCRIPT"/> 112	
		<input type="button" value="DELETE SCRIPT"/> 114	

FIG. 7

26a

HOW DO YOU FEEL?

VERY BAD	BAD	GOOD	VERY GOOD
<input type="checkbox"/> 70A	<input type="checkbox"/> 70B	<input type="checkbox"/> 70C	<input type="checkbox"/> 70D

64

FIG. 8

26a

**CONNECT GLUCOSE METER
AND PRESS ANY BUTTON
WHEN FINISHED**

<input type="checkbox"/> 70A	<input type="checkbox"/> 70B	<input type="checkbox"/> 70C	<input type="checkbox"/> 70D
------------------------------	------------------------------	------------------------------	------------------------------

64

FIG. 9

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PATIENT REPORT

PATIENT:

42

DATE OF MEASUREMENT:

116

QUERY RESPONSES

HOW DO YOU FEEL?

HOW WELL ARE YOU
MANAGING YOUR DISEASE?

HOW HARD IS IT FOR YOU TO
FOLLOW YOUR TREATMENT PLAN?

HOW HARD IS IT FOR YOU TO
CONTROL YOUR BLOOD SUGAR?

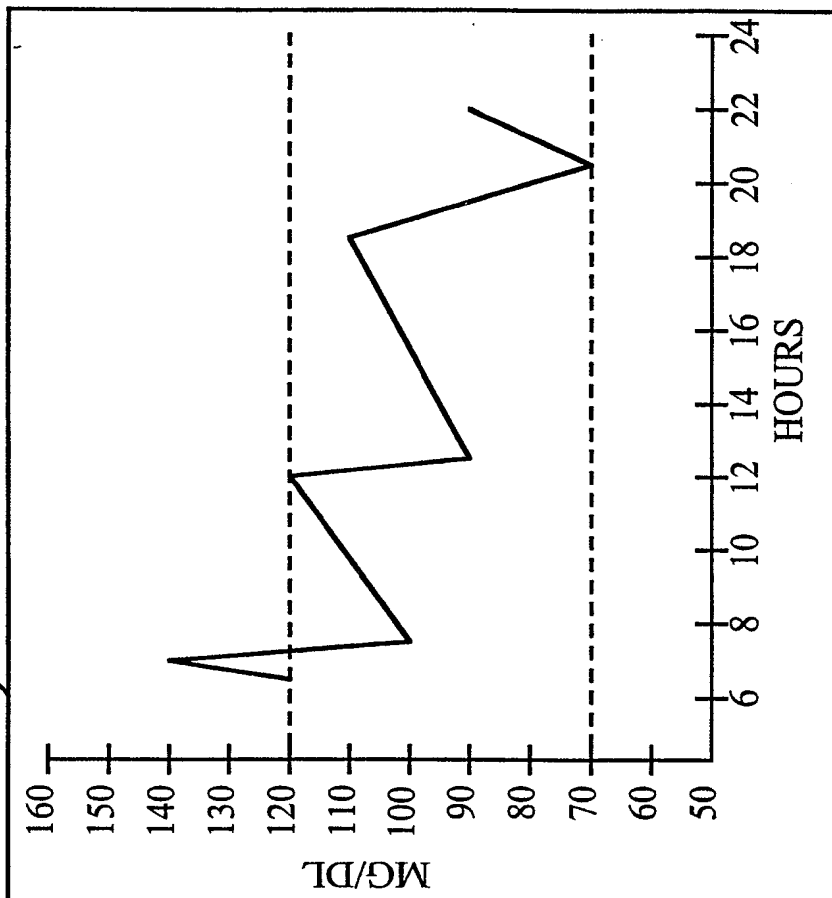


FIG. 10

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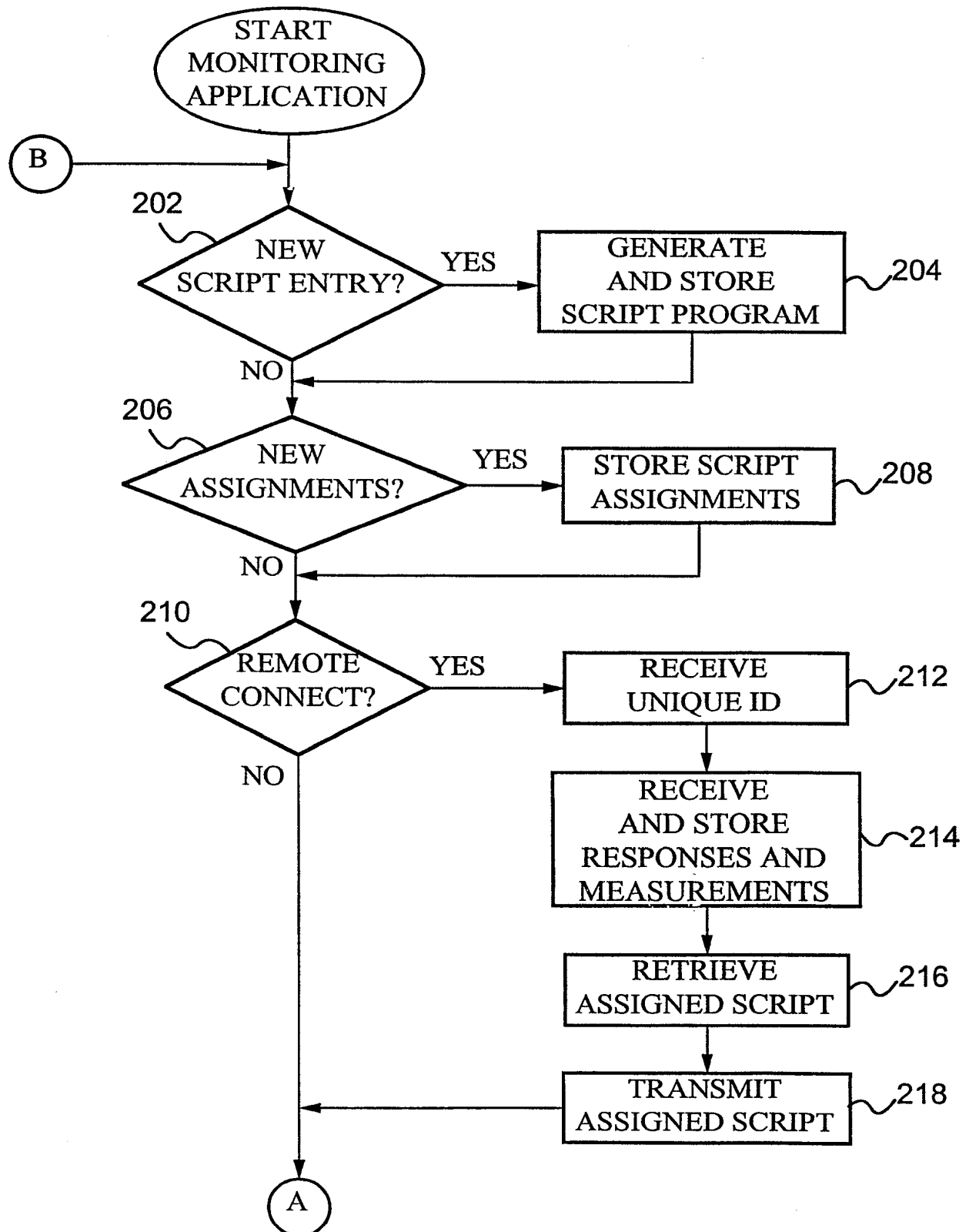
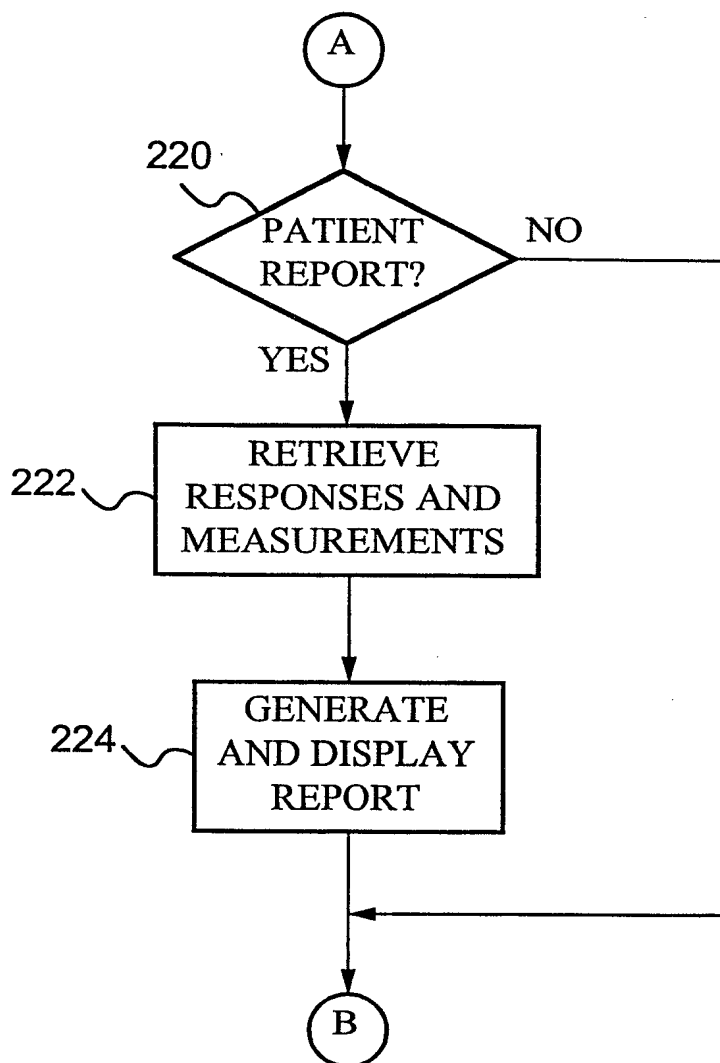
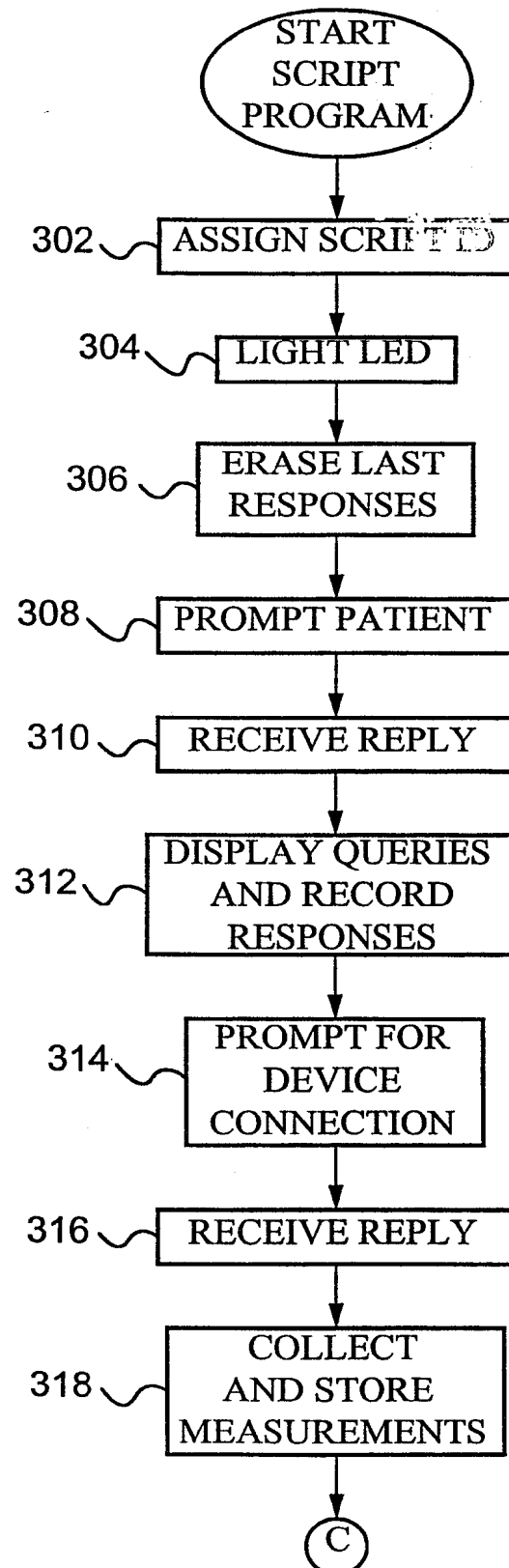
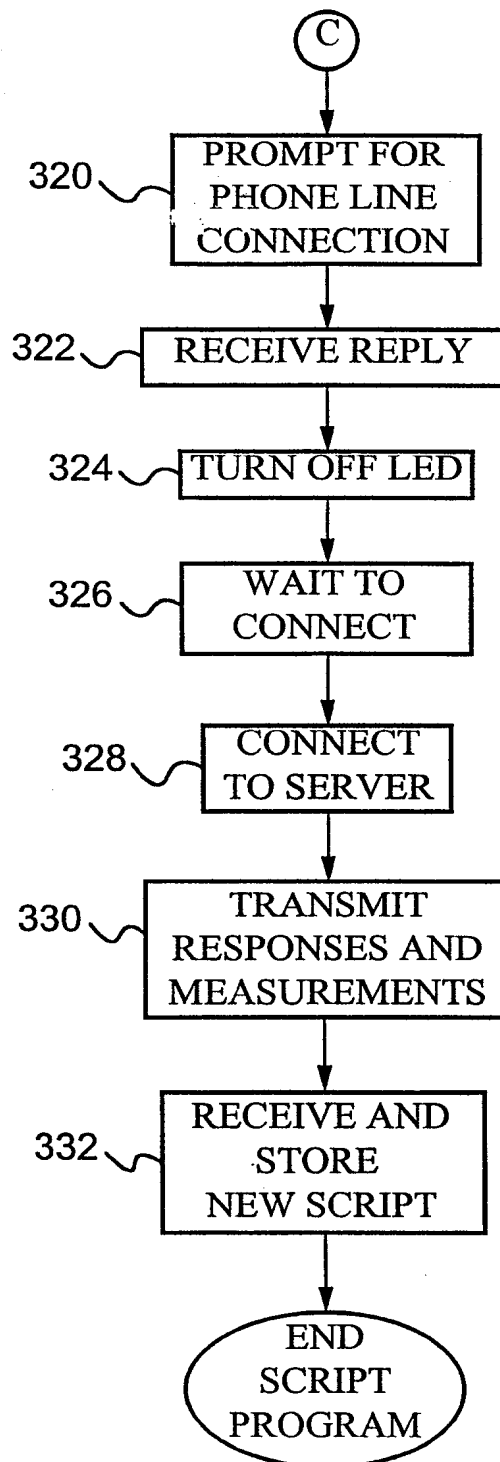


FIG. 11A

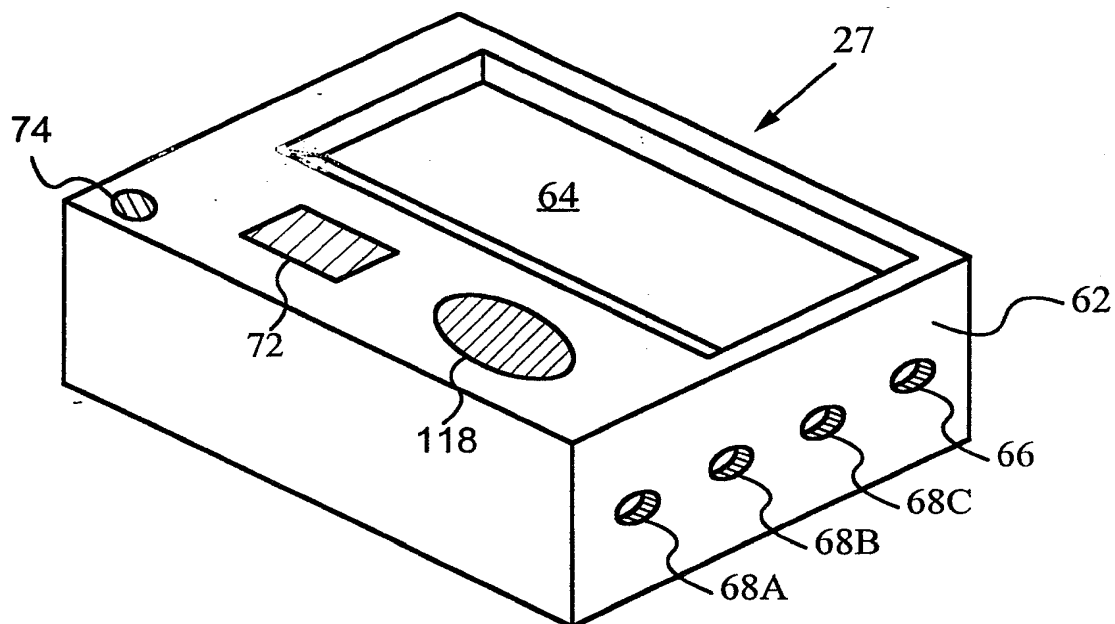
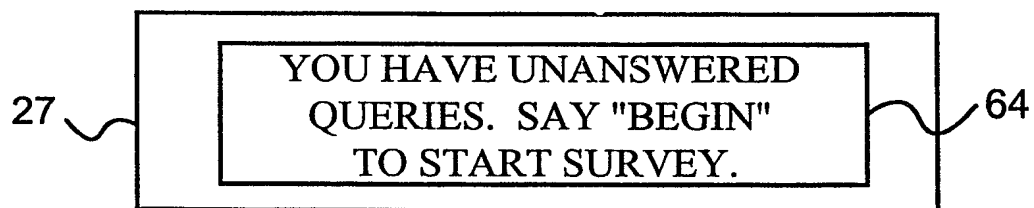
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**FIG. 11B**

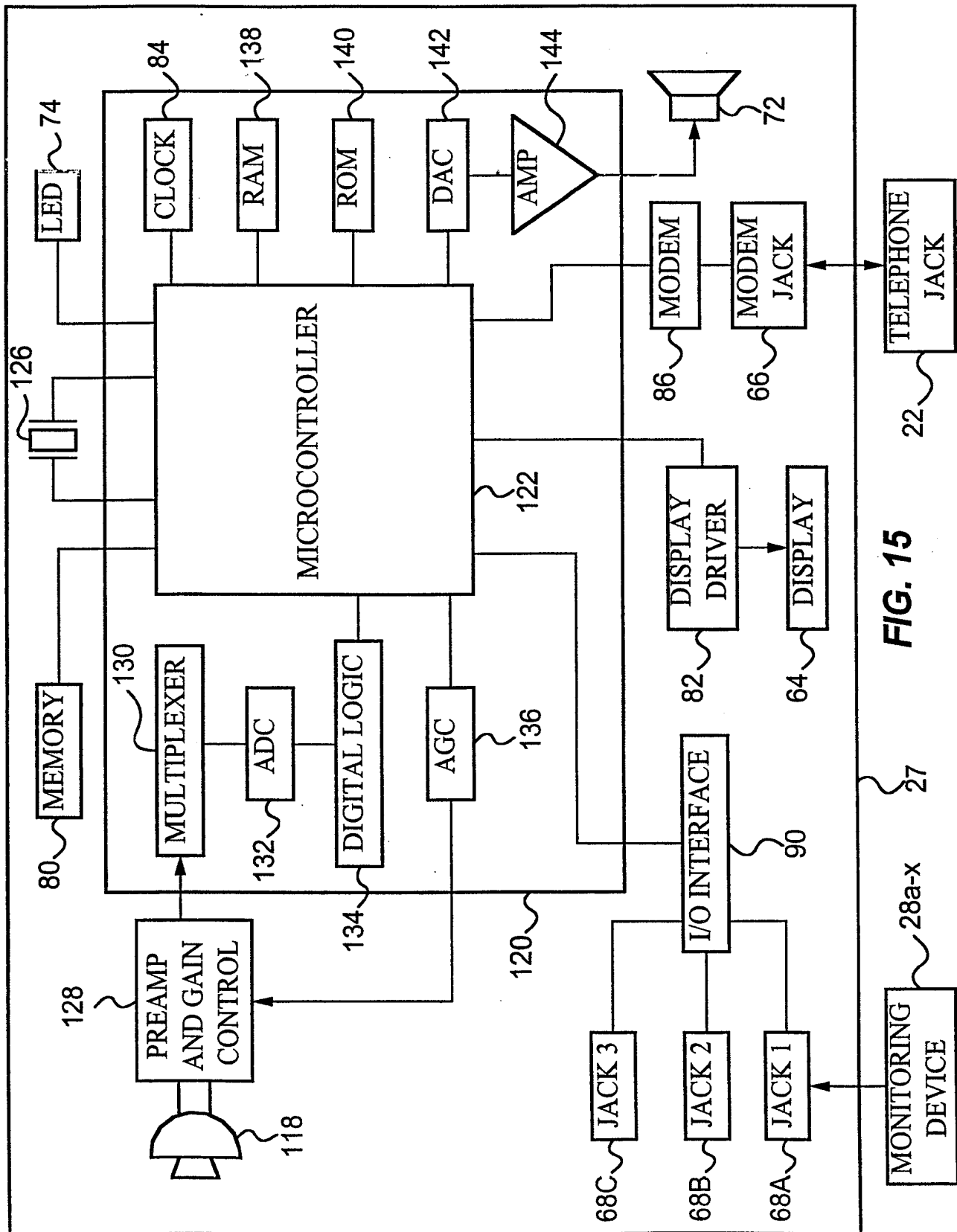
10/31**FIG. 12A**

11/31**FIG. 12B**

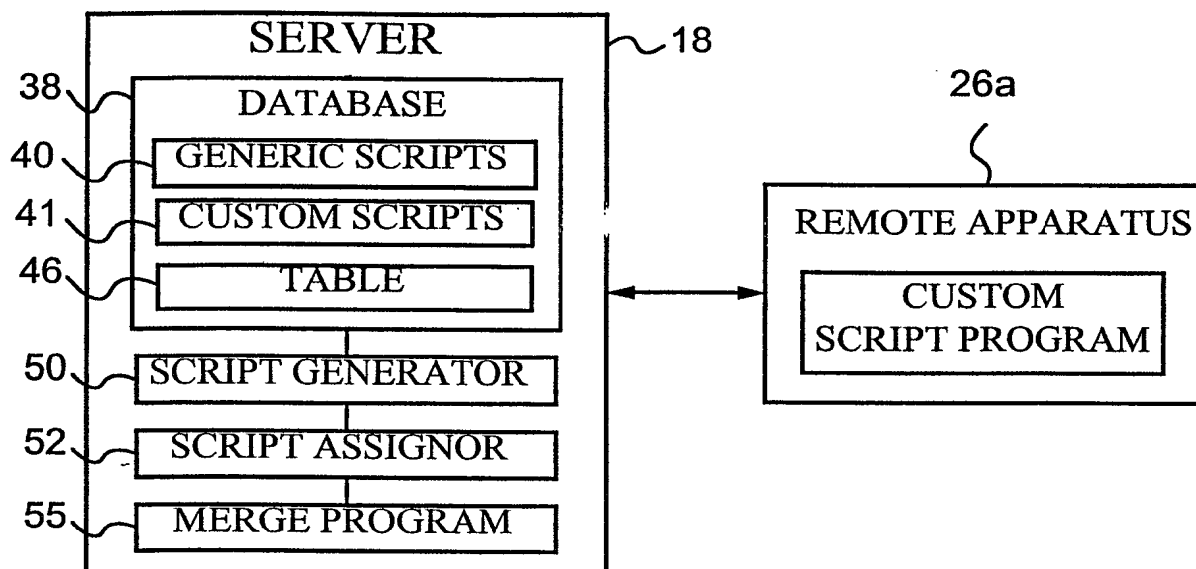
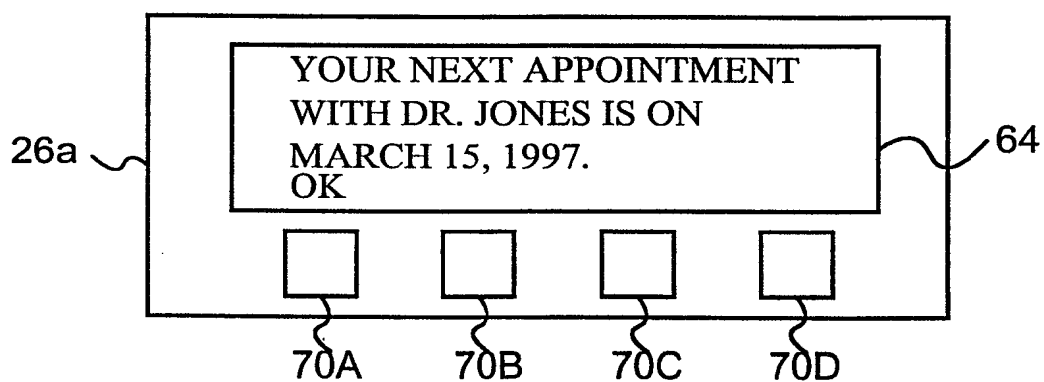
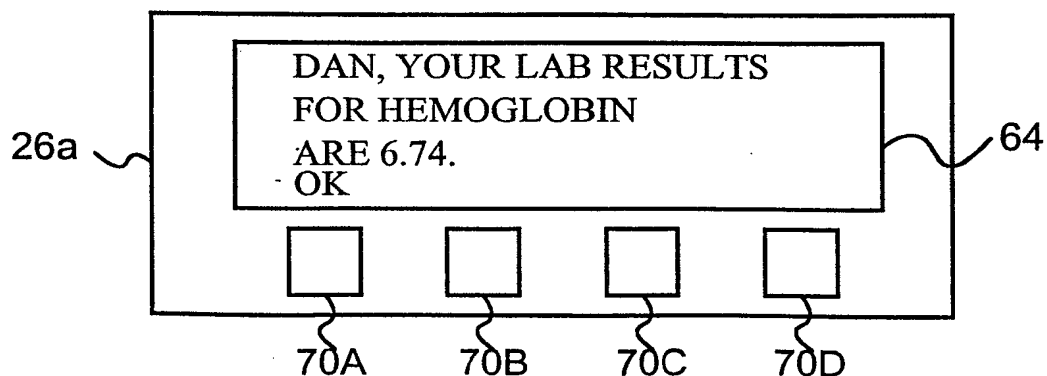
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**FIG. 13****FIG. 14**

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**FIG. 16****FIG. 17****FIG. 18**

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SCRIPT ENTRY SCREEN

SCRIPT NAME:

92

STATEMENTS	CHOICE 1	CHOICE 2	CHOICE 3	CHOICE 4
YOUR NEXT APPOINTMENT WITH <<INSERT PHYSICIAN_NAME>> IS ON <<INSERT APPOINTMENT_DATE>>	OK	<input type="text"/>	<input type="text"/>	<input type="text"/>
<<INSERT PATIENT_NAME>>, YOUR LAB RESULTS FOR HEMOGLOBIN ARE <<INSERT HbA1c_RESULT>>	OK	<input type="text"/>	<input type="text"/>	<input type="text"/>
<<INSERT PATIENT_NAME>>, REMEMBER TO EXERCISE CONSISTENTLY	OK	<input type="text"/>	<input type="text"/>	<input type="text"/>

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96

CONNECTION TIME:

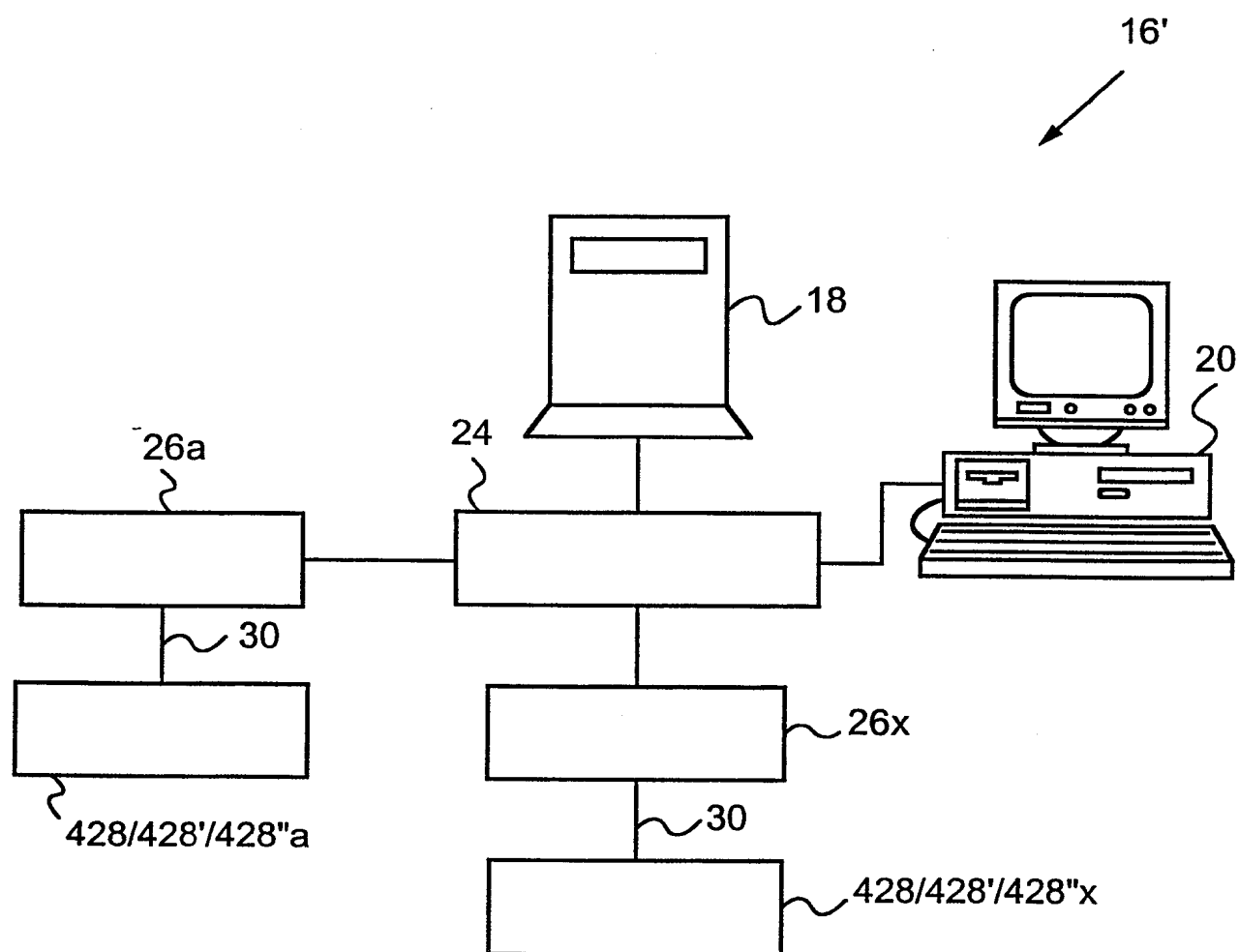
100

102

104

FIG. 19

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**FIG. 20A**

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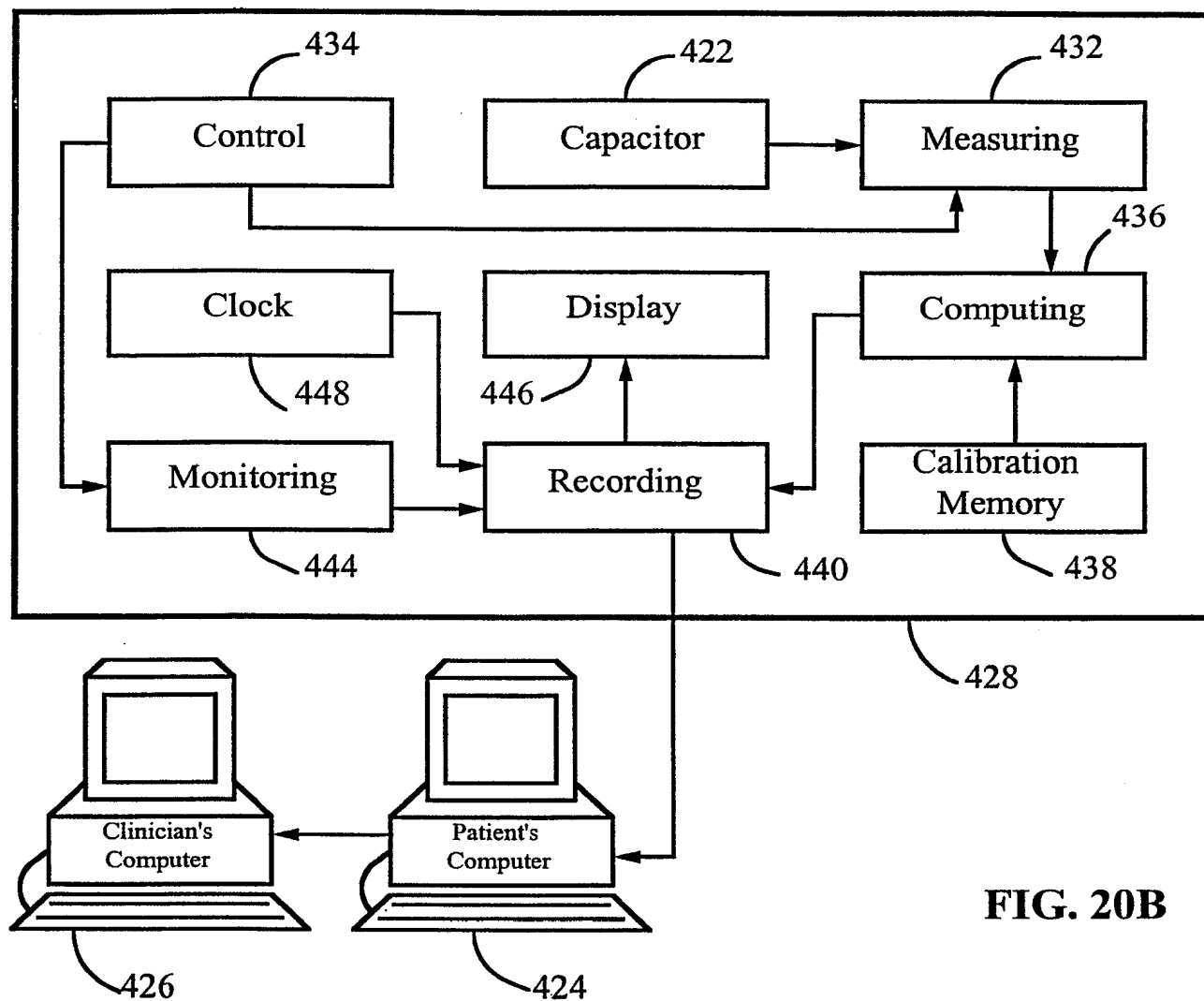
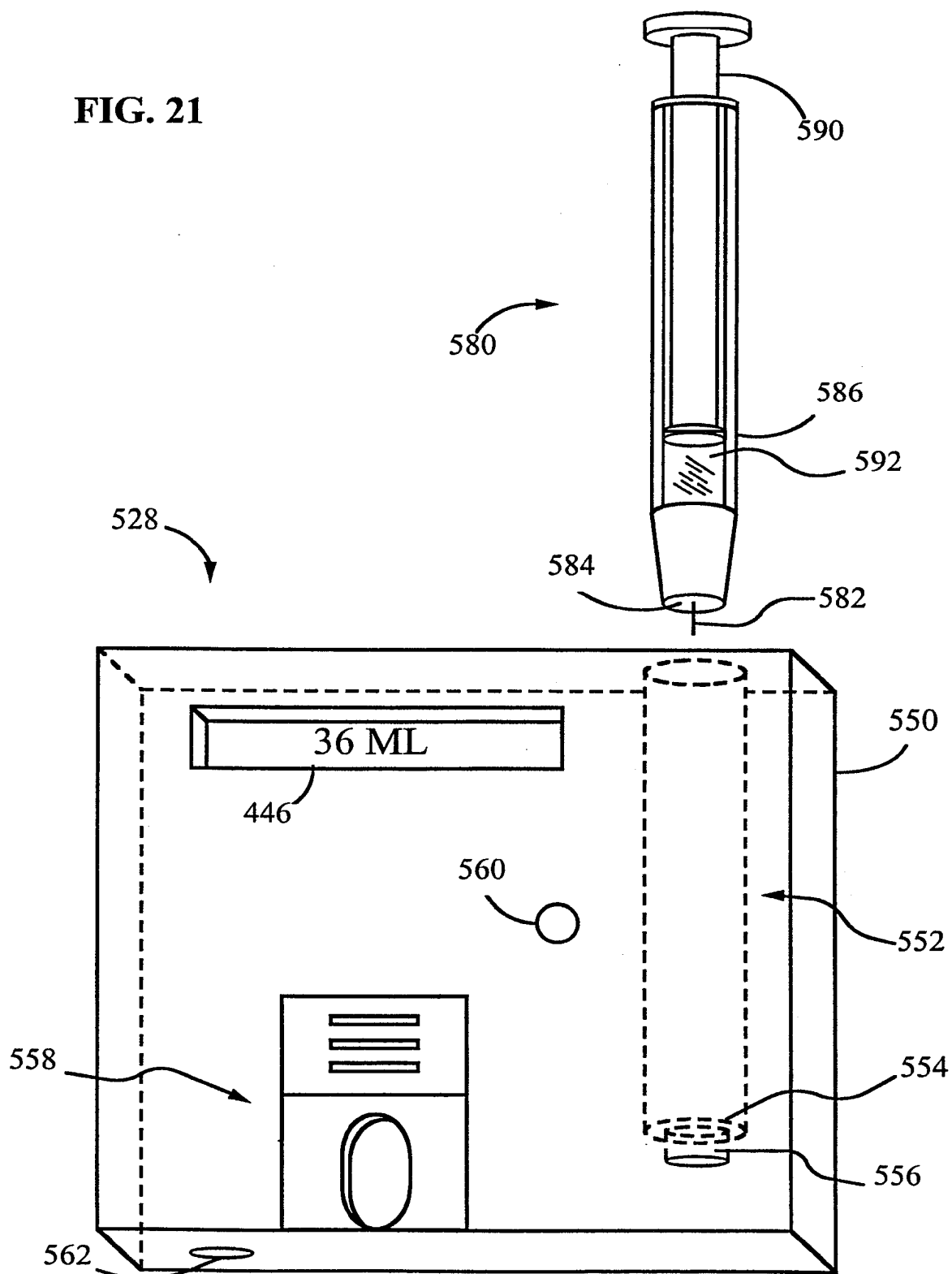


FIG. 20B

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FIG. 21



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FIG. 22A

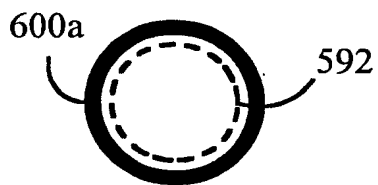
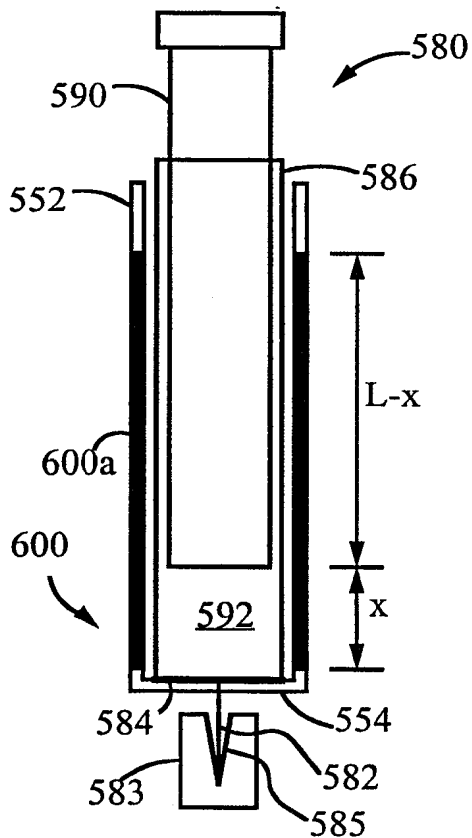


FIG. 22B

FIG. 23A

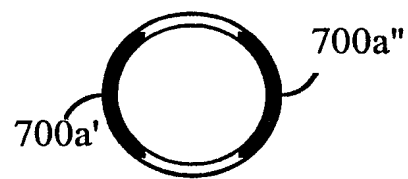
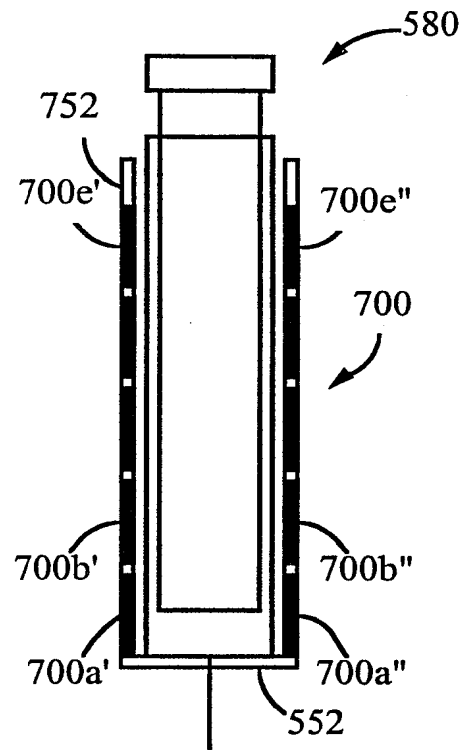


FIG. 23B

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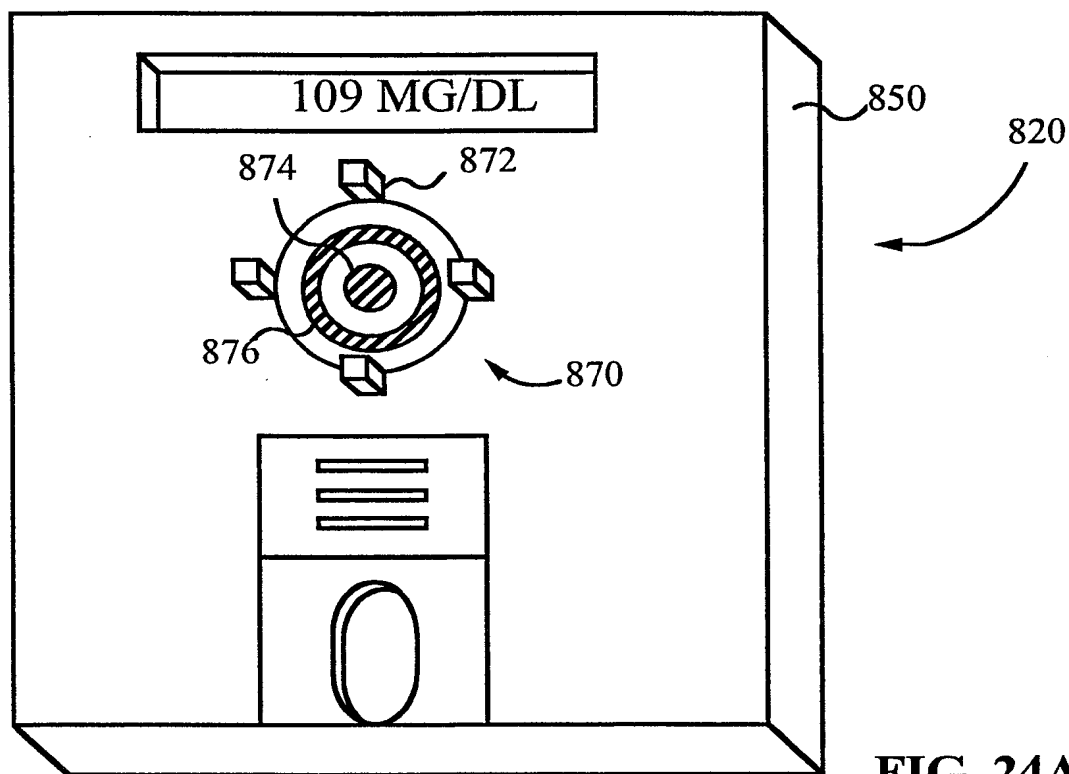


FIG. 24A

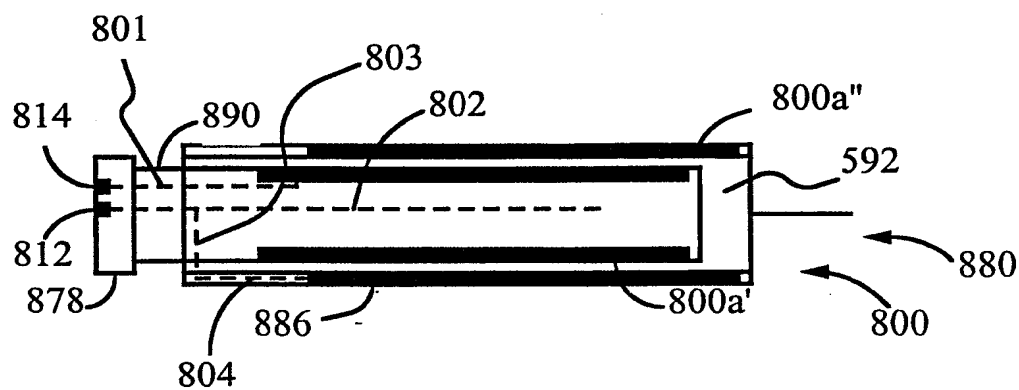


FIG. 24B

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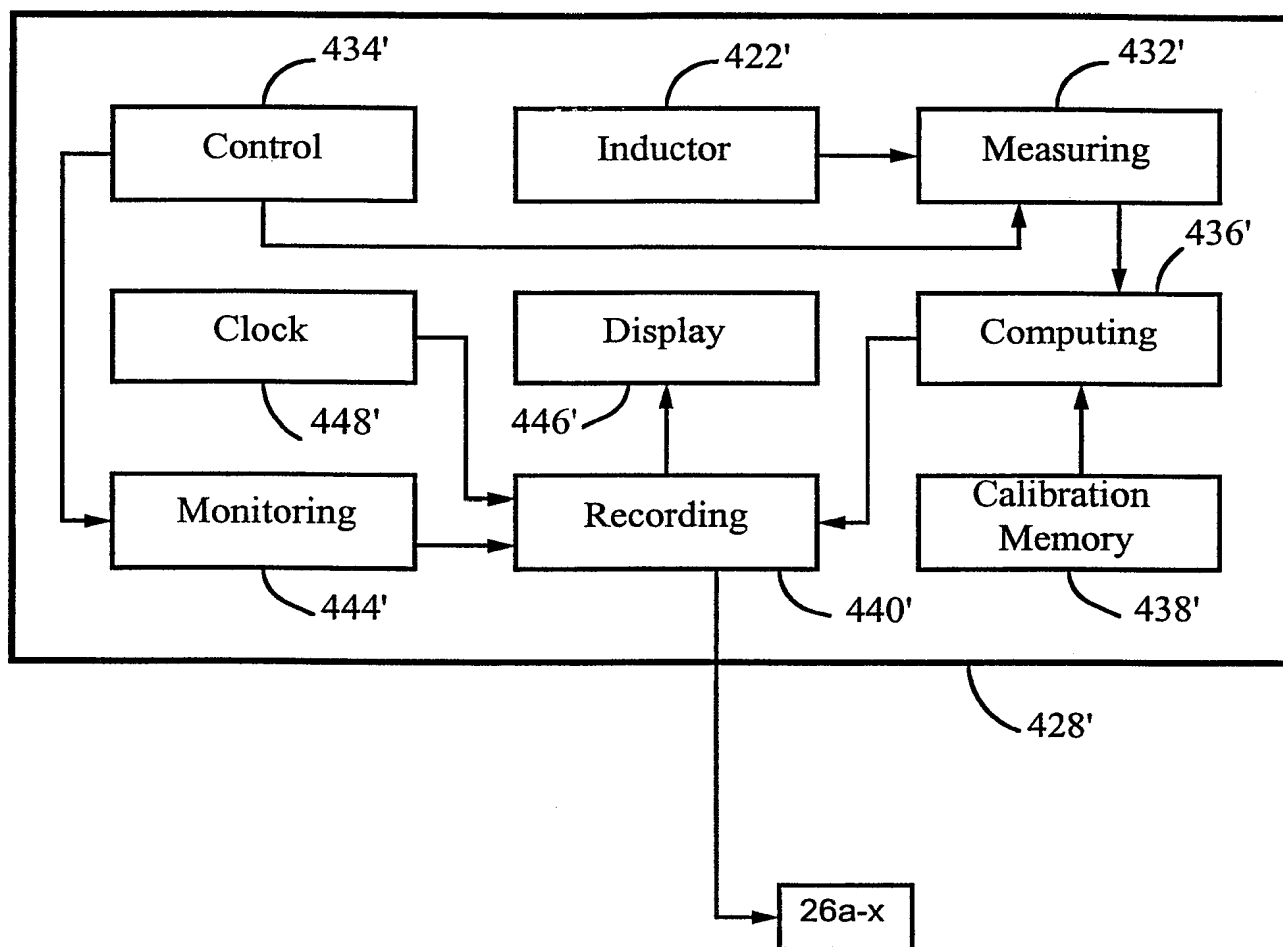
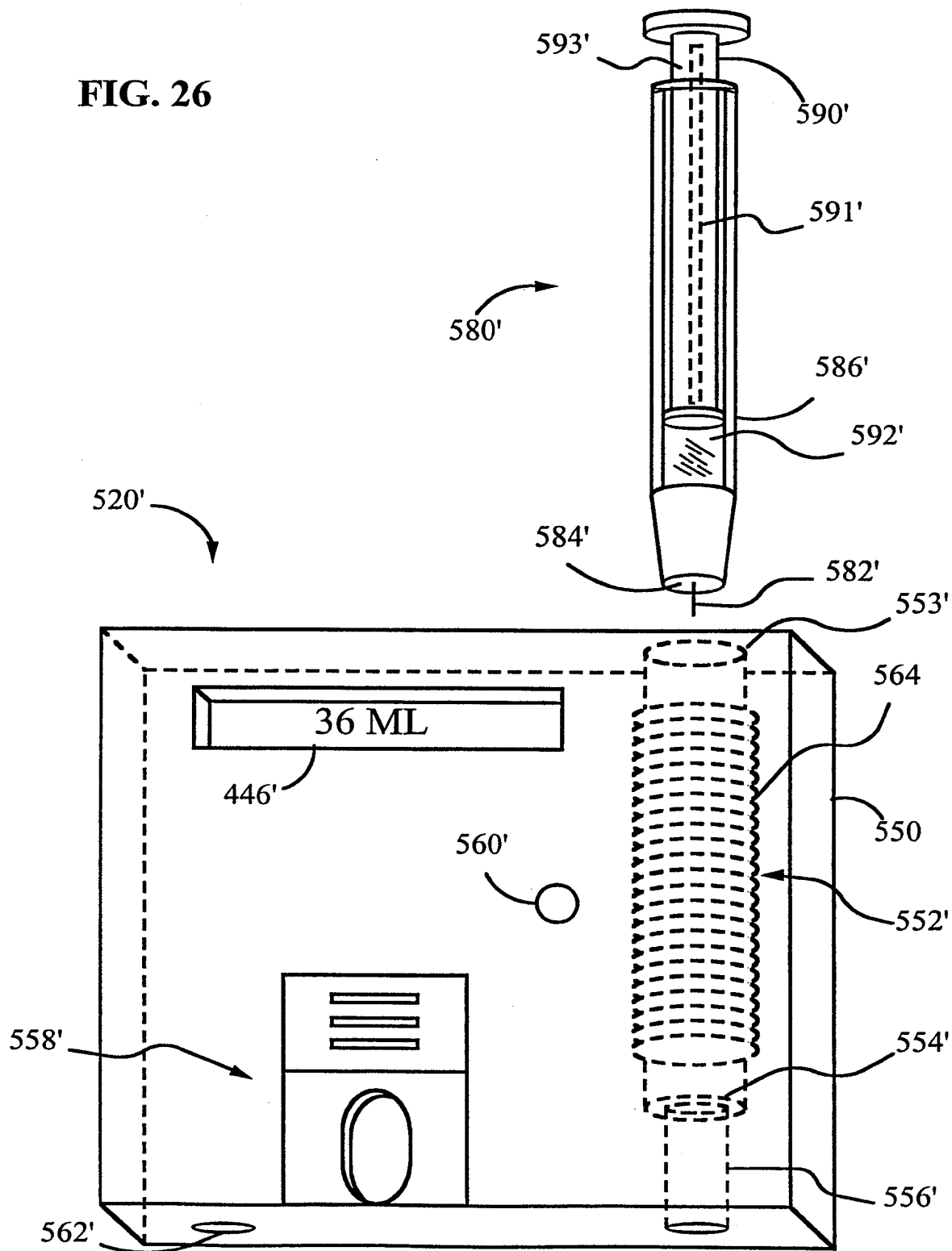


FIG. 25

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FIG. 26



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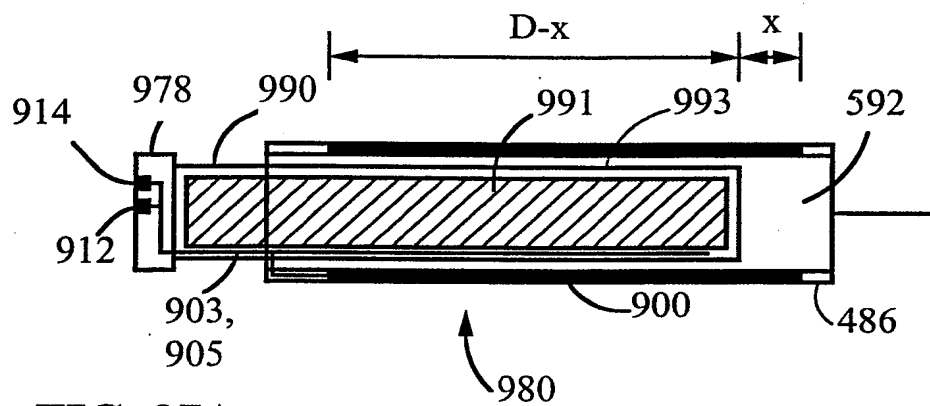


FIG. 27A

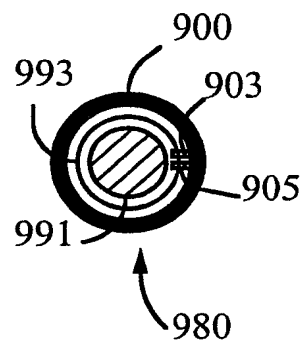
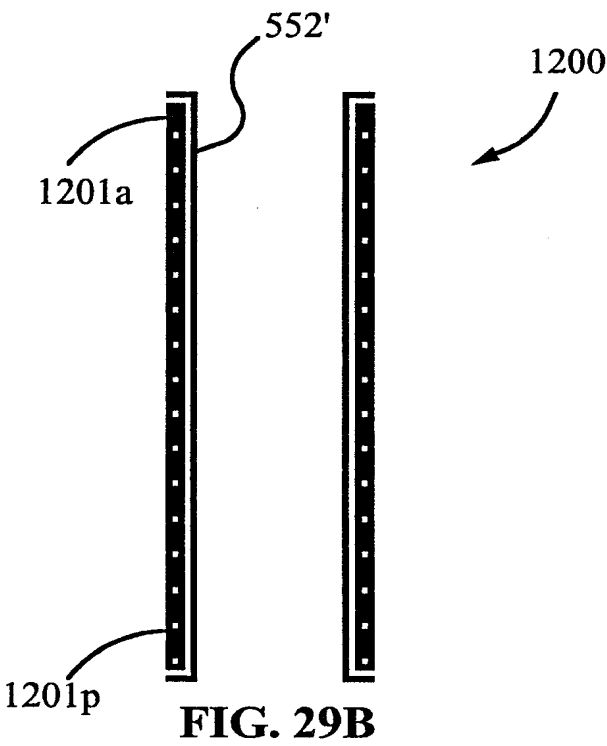
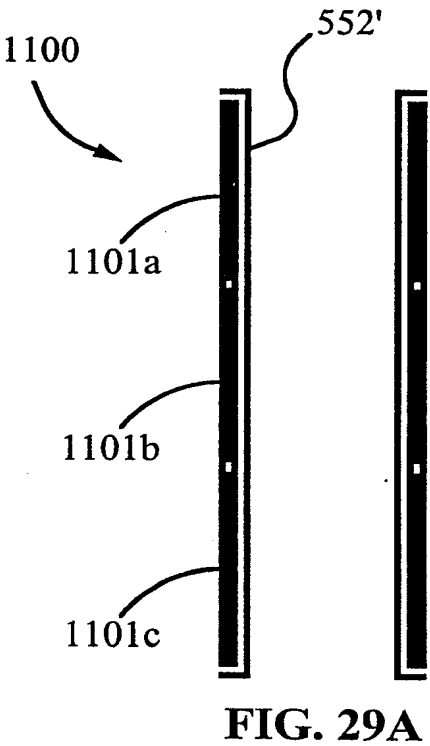
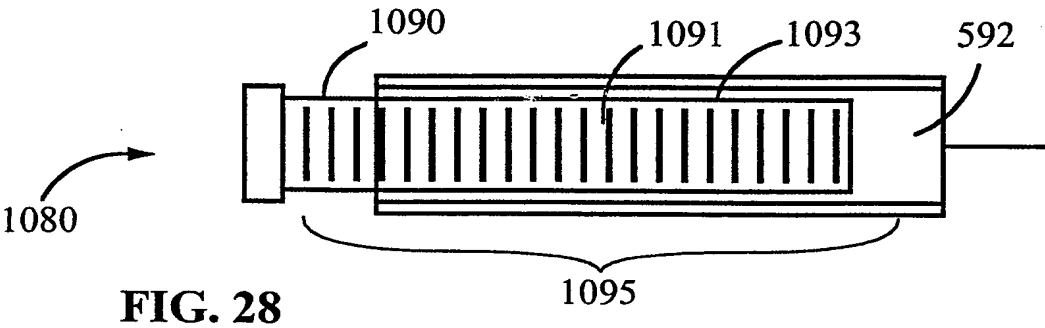
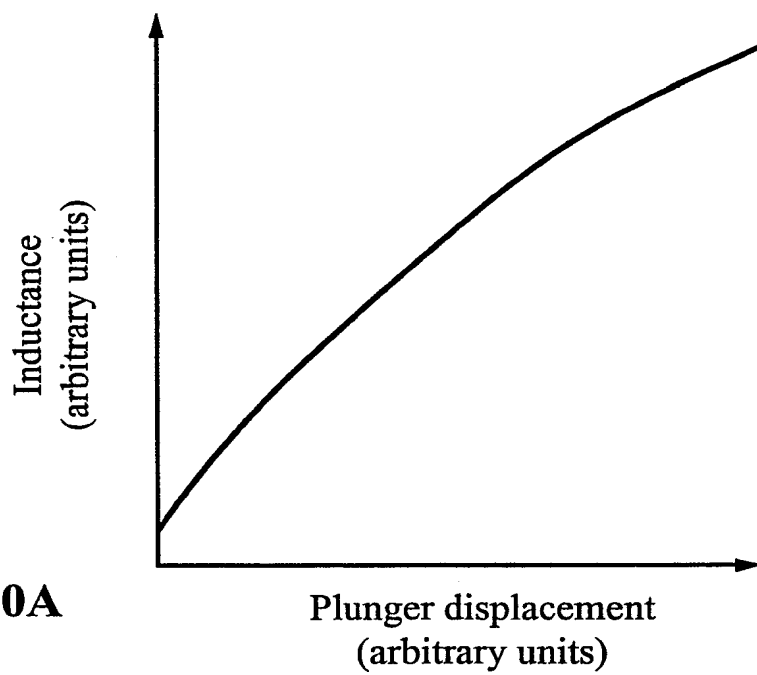
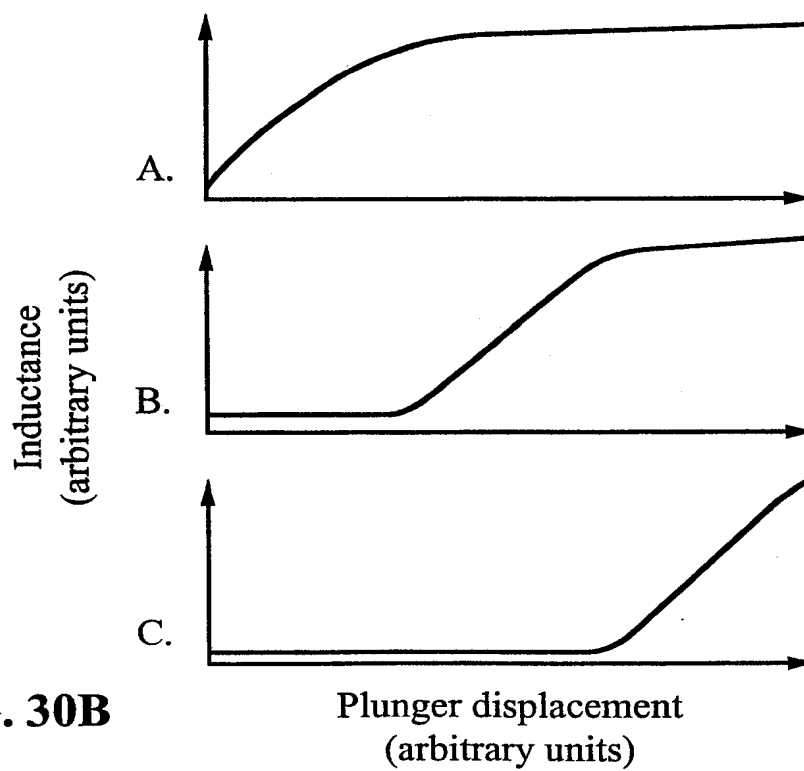
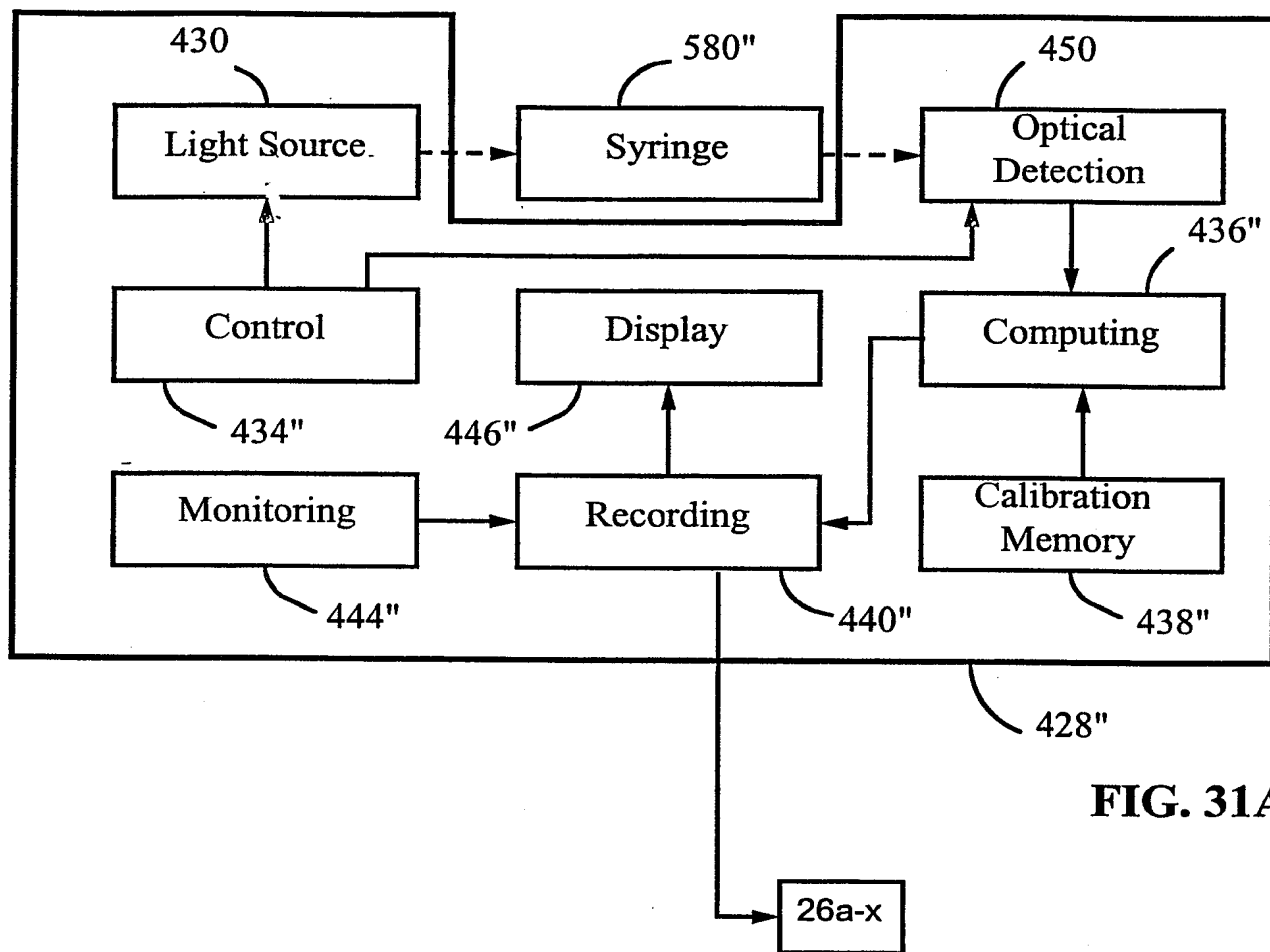
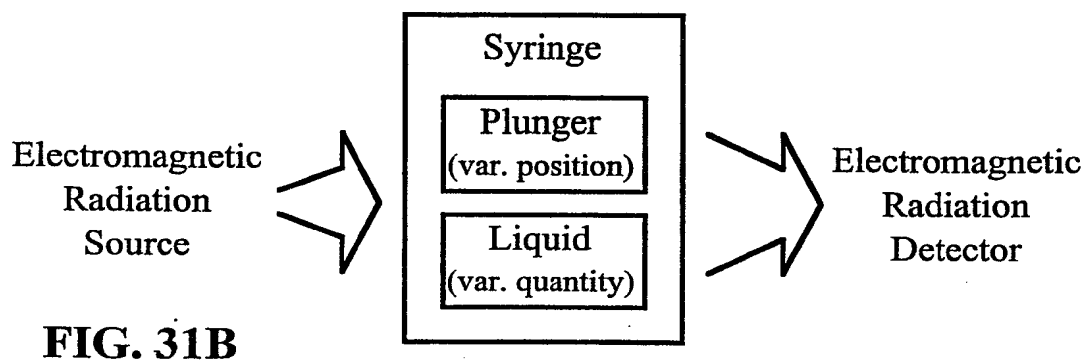


FIG. 27B



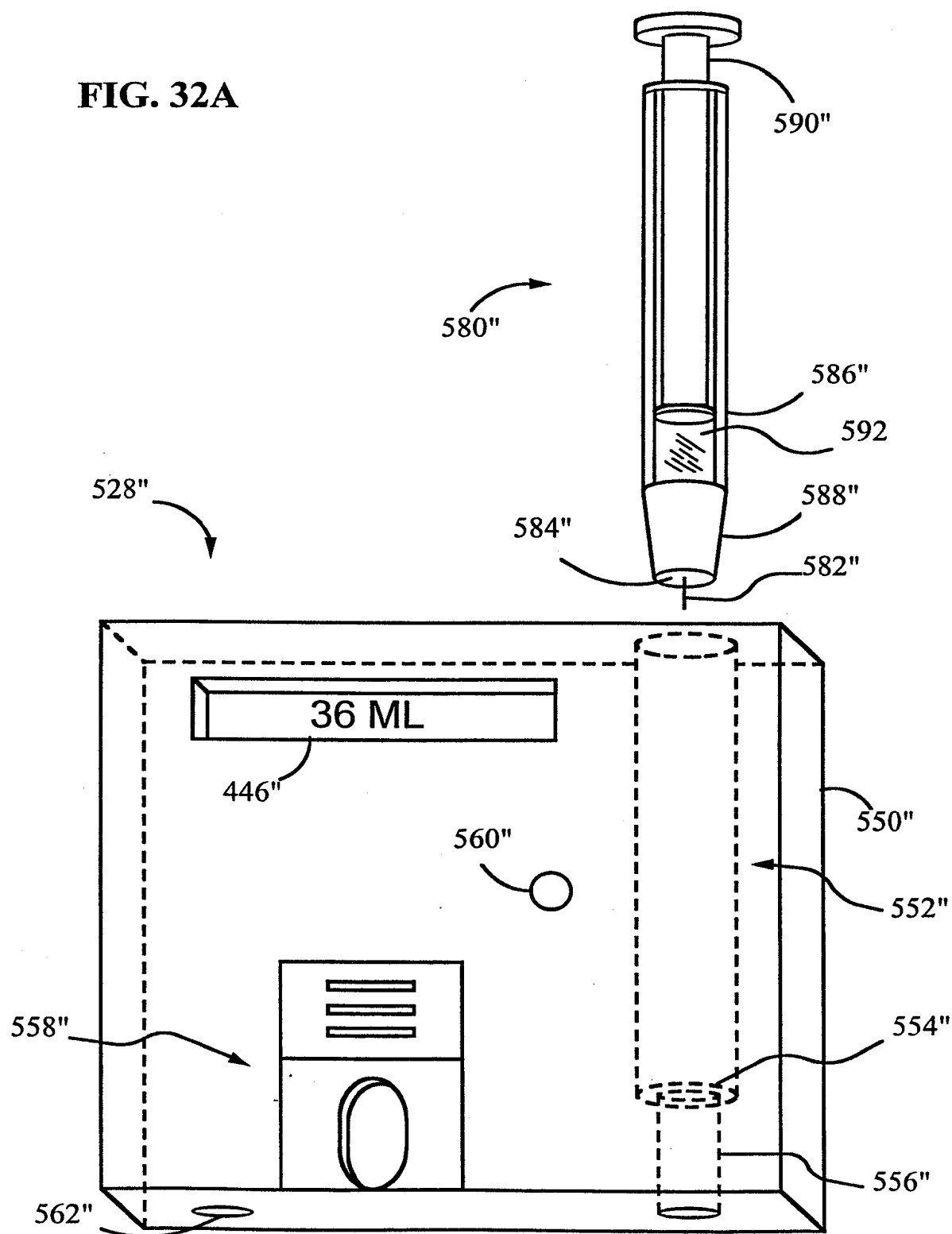
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**FIG. 30A****FIG. 30B**

26/31**FIG. 31A****FIG. 31B**

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FIG. 32A



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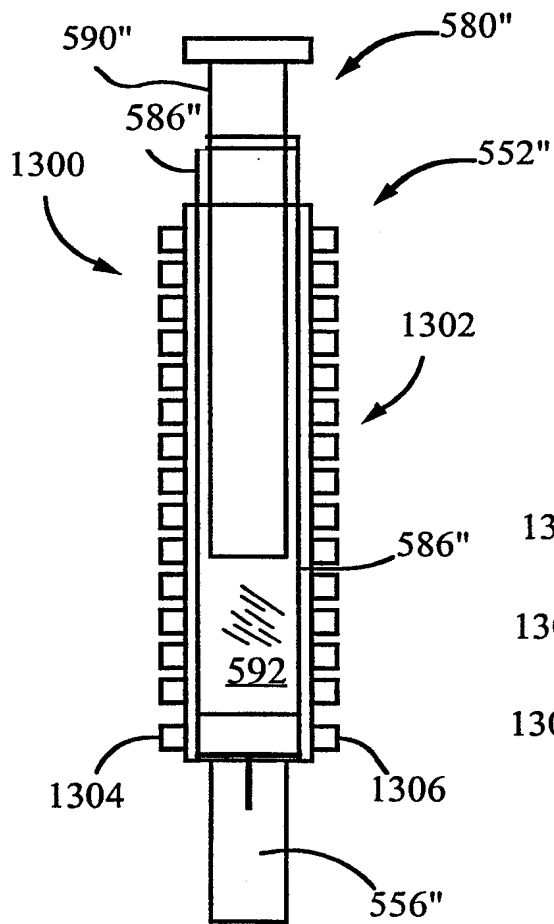


FIG. 32B

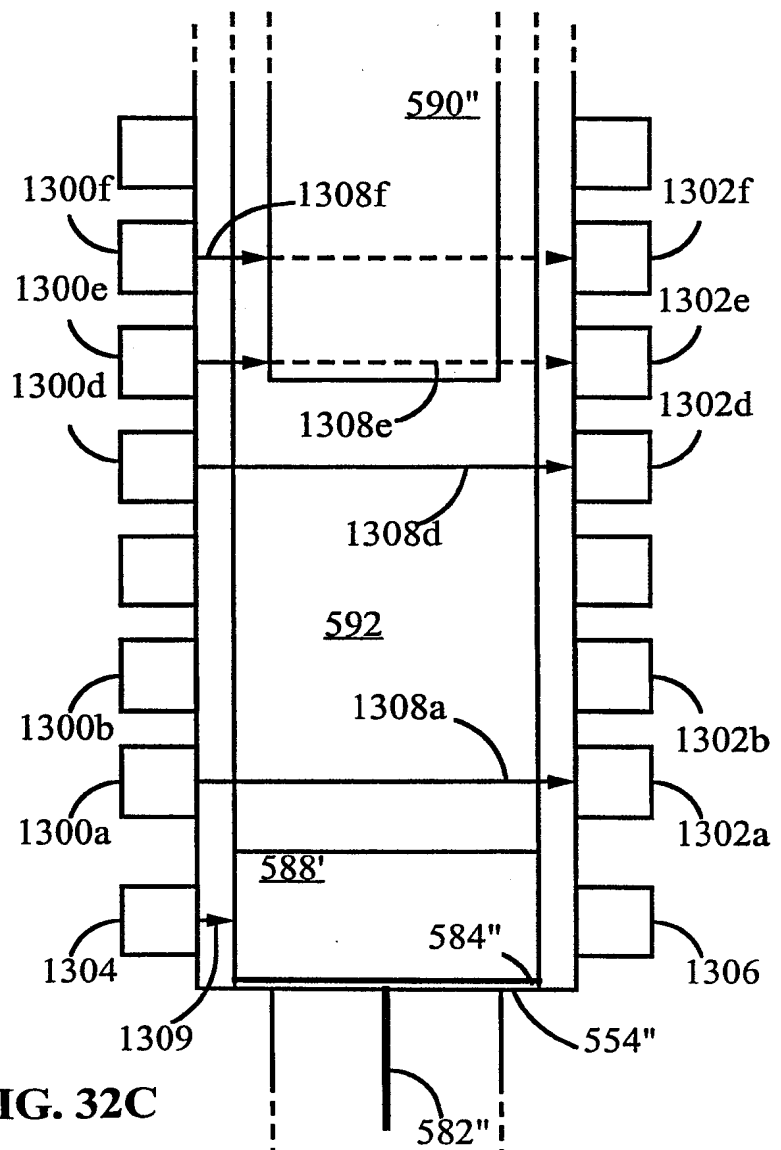
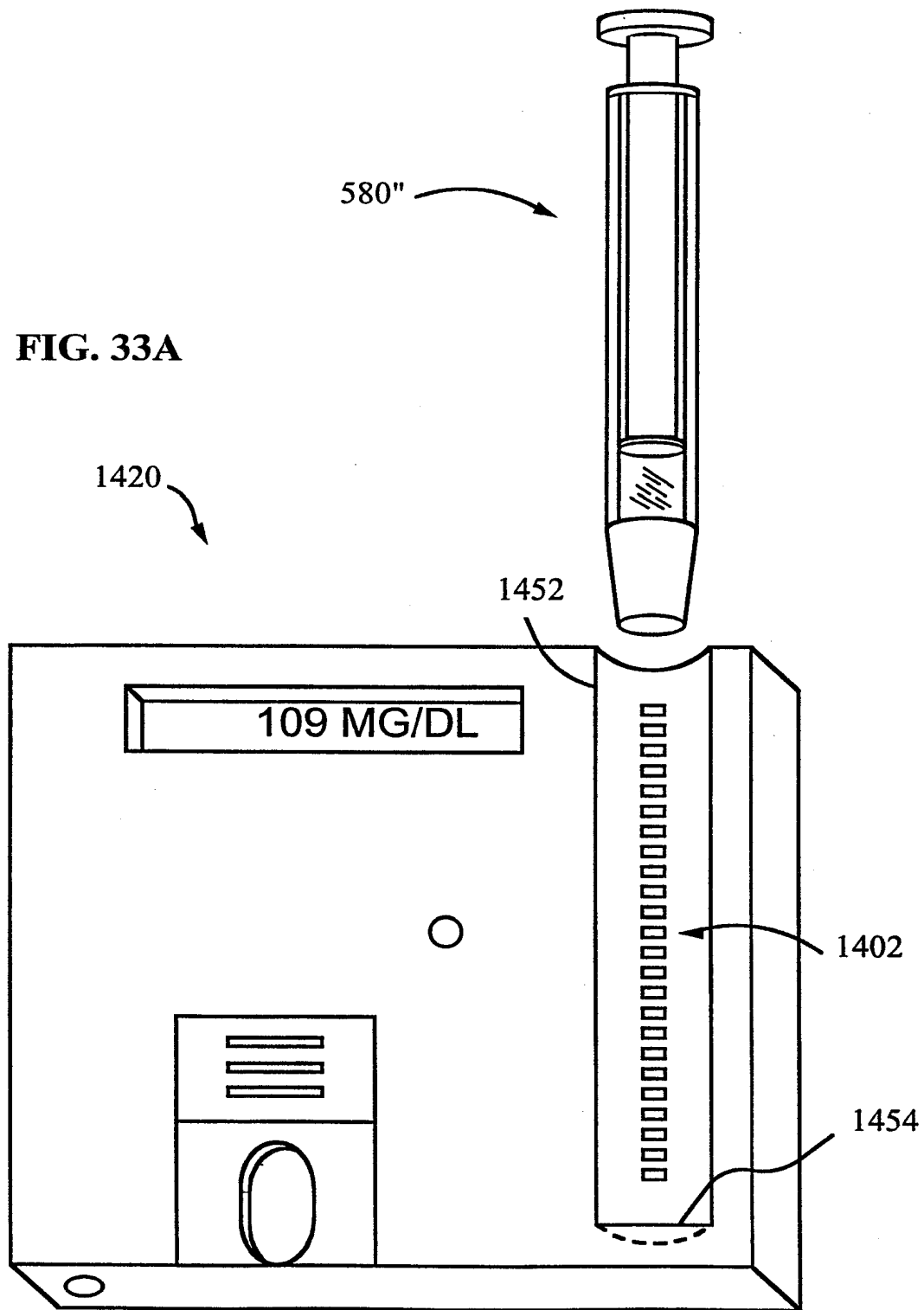


FIG. 32C

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FIG. 33A



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FIG. 32D

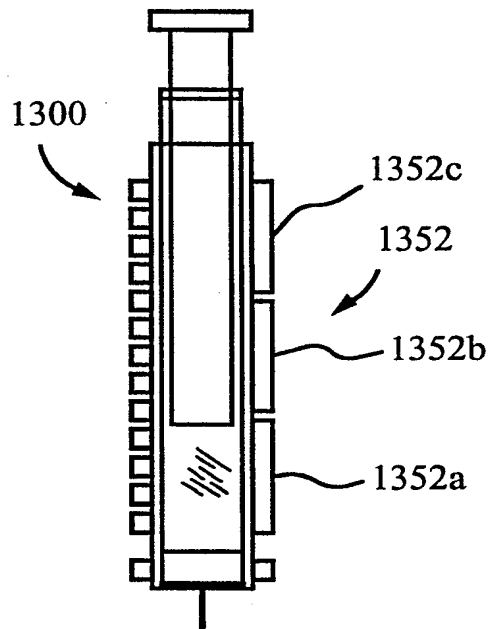


FIG. 32E

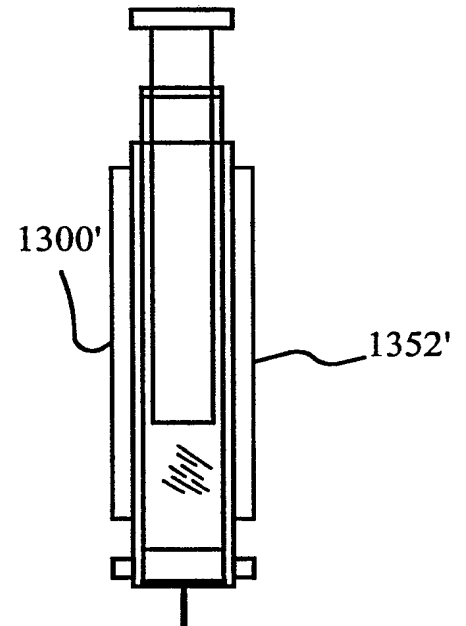
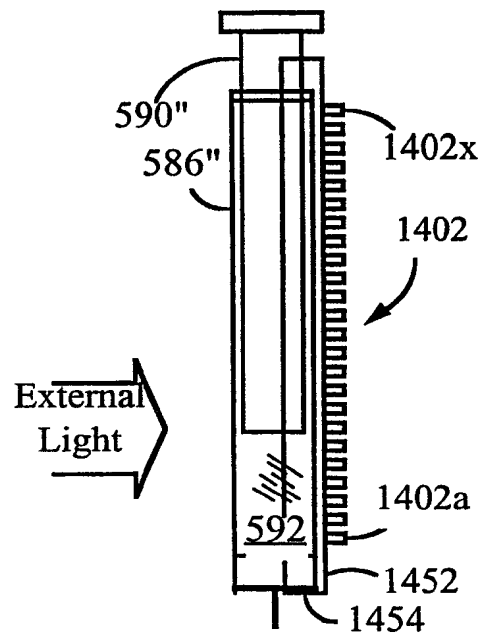
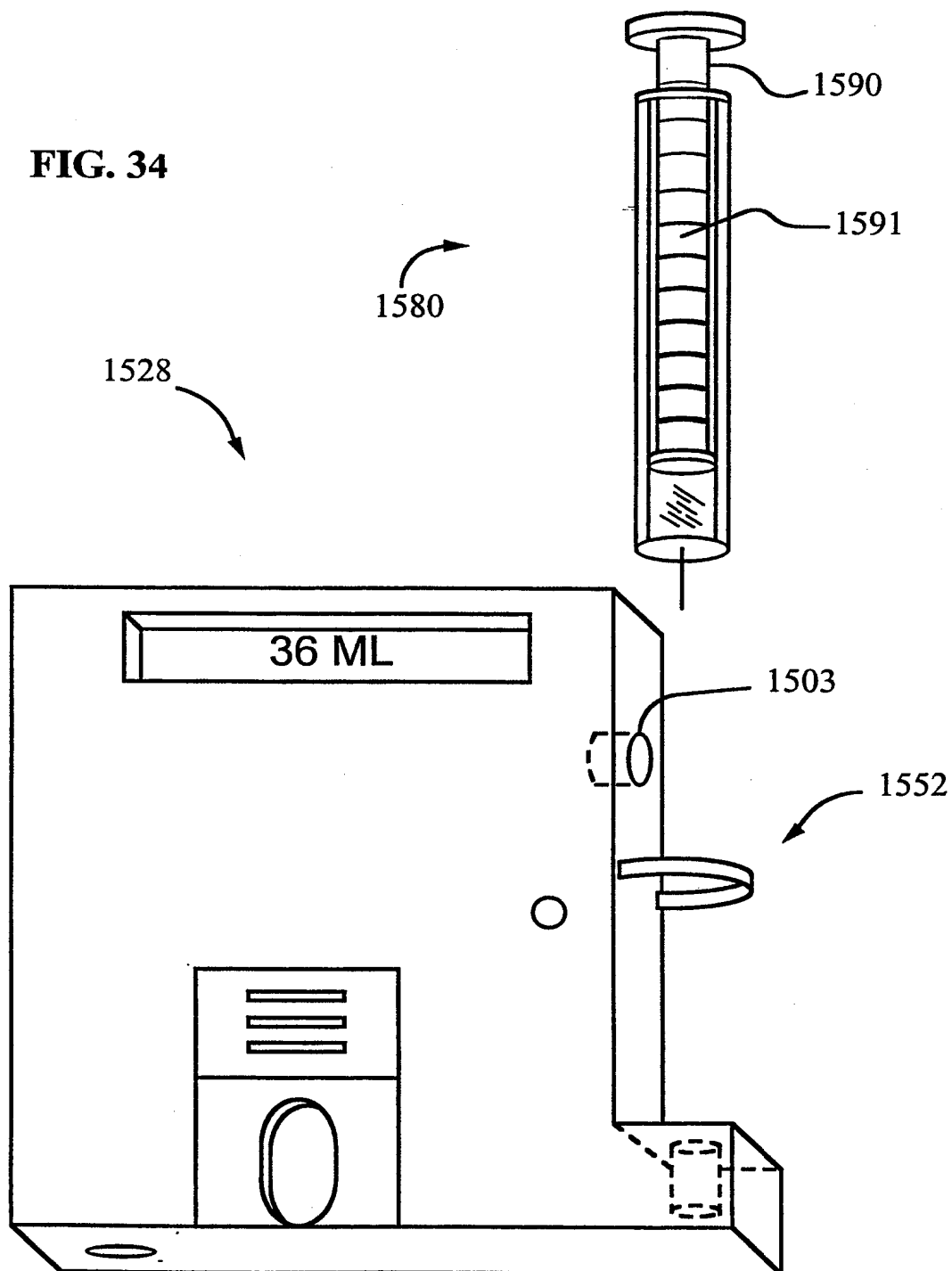


FIG. 33B



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FIG. 34



INTERNATIONAL SEARCH REPORT

International application No.
PCT/US99/28370

A. CLASSIFICATION OF SUBJECT MATTER

IPC(6) :A61B 5/00

US CL :600/300

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 128/903, 904, 920; 600/300, 301, 361, 365

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched
NONE

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)
EAST, and WEST 1.2

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X --- Y	US 5,711,297 A (ILIFF) 27 January 1998, entire document.	37 ----- 1-36, 38-45

☐ Further documents are listed in the continuation of Box C. ☐ See patent family annex.

* Special categories of cited documents:	
"A" document defining the general state of the art which is not considered to be of particular relevance	"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
"E" earlier document published on or after the international filing date	"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
"O" document referring to an oral disclosure, use, exhibition or other means	"&" document member of the same patent family
"P" document published prior to the international filing date but later than the priority date claimed	

Date of the actual completion of the international search

16 FEBRUARY 2000

Date of mailing of the international search report

17 MAR 2000

Name and mailing address of the ISA/US
Commissioner of Patents and Trademarks
Box PCT
Washington, D.C. 20231

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